

European Guidelines on DRLs for Paediatric Imaging

Final complete draft

Contents

12	PREFACE	4
13	EXECUTIVE SUMMARY	4
14	1. Background	9
15	2. Introduction	10
16	3. Purpose and scope	11
17	4. Definitions	12
18	5. Review of existing paediatric DRLs	14
19	5.1 Introduction	14
20	5.2 Methods of review	14
21	5.3 National DRLs for paediatric exams set in the European countries	14
22	5.4 Studies and proposals on paediatric DRLs	17
23	5.5 Strengths and limitations of the available DRLs and systems for their establishment	18
24	5.5.1 Strengths of the available systems	18
25	5.5.2 Shortcomings and limitations	18
26	5.5.3 Accuracy and comparability of DRLs	20
27	6. Need for modality specific paediatric DRLs	22
28	6.1 Radiography and fluoroscopy	22
29	6.2 Computed tomography	23
30	6.3 Interventional radiology (incl. cardiology)	24
31	6.4 Prospective need of DRLs for emerging or increasing new practices	25
32	6.5 Need for further patient dose surveys	26
33	7. Basic approach to paediatric DRLs	27
34	7.1 General	27
35	7.2 Recommended DRL quantities	29

1	7.2.1 Radiography and fluoroscopy	29
2	7.2.2 Computed tomography.....	30
3	7.2.3 Interventional radiology	31
4	7.3 Recommended patient grouping	32
5	8. Practical methods to establish paediatric DRLs.....	34
6	8.1 General.....	34
7	8.2 Patient dose surveys	34
8	8.2.1 DRL quantities and patient grouping	34
9	8.2.2 Technical equipment parameters	34
10	8.2.3 Recommended sample size and composition.....	36
11	8.2.4 Percentile point for DRL.....	36
12	8.3 Setting of DRLs	37
13	8.3.1 Organisations to set the DRLs	37
14	8.3.2 Role of authorities and professional societies.....	38
15	8.4 Automatic dose management	38
16	8.4.1 General review	38
17	8.4.2 Recommendations for the dose management systems to support paediatric DRLs	38
18	9. Methods of using DRLs	40
19	9.1 Use of different types of DRLs	40
20	9.1.1 LDRLs – for optimisation within a healthcare facility or group of healthcare facilities ..	40
21	9.1.2 NDRLs – for both local and nationwide optimisation	40
22	9.1.3 EDRL – for support of national efforts.....	41
23	9.2 Methods of comparison.....	41
24	9.3 Comparison frequency	42
25	9.4 Local reviews and actions when DRLs are exceeded.....	42
26	10. European DRLs (EDRLs)	43
27	10.1 Methods to establish EDRLs.....	43
28	10.2. EDRL values	44
29	10.3 Use of the EDRLs	46
30	ACKNOWLEDGEMENTS	47
31	REFERENCES.....	48
32	ANNEX A. NATIONAL DRL VALUES FOR PAEDIATRIC EXAMINATIONS AND	
33	PROCEDURES IN EUROPEAN COUNTRIES.....	60
34	ANNEX B. DRL VALUES FOR PAEDIATRIC EXAMINATIONS AND PROCEDURES:	
35	SUMMARY OF SELECTED DRL DATA PUBLISHED IN EUROPEAN COUNTRIES.....	70
36	ANNEX C. REVIEW OF EXISTING PAEDIATRIC DRLS	73
37	C.1 Introduction	73
38	C.2 Methods of review.....	73

1	C.2.1 Questionnaire on paediatric DRLs	73
2	C.2.2 Literature review and database	73
3	C.3 National DRLs for paediatric exams set in the European countries.....	74
4	C.3.1 Radiography	76
5	C.3.2 Fluoroscopy	79
6	C.3.3 Computed tomography	80
7	C.3.4 Interventional radiology	83
8	C.4 Studies on paediatric DRLs in European countries.....	83
9	C.4.1 Radiography	84
10	C.4.2 Fluoroscopy	86
11	C.4.3 Computed tomography	86
12	C.4.4 Interventional radiology	89
13	C.5 Other studies on paediatric DRLs	90
14	C.5.1 Radiography	90
15	C.5.2 Fluoroscopy	91
16	C.5.3 Computed tomography	91
17	C.5.4 Interventional radiology	92
18	ANNEX D. NEED FOR PAEDIATRIC DRLs	94
19	D.1 Frequencies of paediatric examinations	94
20	D.2 Population dose from paediatric examinations	98
21	ANNEX E. DEVELOPMENT OF DOSE MANAGEMENT SYSTEMS	100
22	E.1 General development	100
23	E.2 Existing dose management systems	101
24	ANNEX F. DETAILS OF EDRL CALCULATION.....	103
25	ANNEX G. PATIENT DOSES AND DRLS IN PAEDIATRIC CARDIAC AND NON CARDIAC	
26	PROCEDURES.....	105
27	G.1 Paediatric diagnostic or therapeutic interventional cardiac procedures.....	105
28	G.1.1 Introduction	105
29	G.1.2 Recent publications on patient doses and LDRLs.....	105
30	G.1.3 PiDRL survey from two cardiac centres	107
31	G.1.4 Summary	108
32	G.2 Paediatric interventional non-cardiac procedures	110
33	ANNEX H. LIST OF ABBREVIATIONS AND SYMBOLS	116
34		
35		
36		
37		

1 **PREFACE**

2

3 *[To be written by the EC; Approx. no of pages: 1. A proposal on the contents, to account for some*
4 *feedback of the Workshop, is provided separately by the consortium.]*

5

6

7 **EXECUTIVE SUMMARY**

8 The establishment and use of diagnostic reference levels (DRLs) have been recommended by the
9 International Commission on Radiological Protection (ICRP) and required in the European Council
10 Directive 2013/59/Euratom Basic Safety Standards (BSS). DRLs are a useful tool in the quest to
11 optimise patient doses in diagnostic radiology and interventional radiology (IR). Particular attention
12 should be paid to establishing and using DRLs in paediatric radiology because children have a
13 higher risk (for some organs and body areas) compared to adults from the detrimental effects of
14 radiation.

15

16 A comprehensive European and worldwide review of DRLs for paediatric examinations (Section 5
17 and Annex C) has indicated that only a few countries have set DRLs for paediatric examinations
18 and there is a complete lack of national DRLs for many examinations, in particular for all paediatric
19 interventional procedures. Furthermore, the existing DRLs are often adopted from the old European
20 Commission (EC) recommendations or from other countries, and only a few countries have based
21 their DRLs on their own national patient dose surveys. In many countries, the initial DRLs have
22 never been updated. Due to the huge variation of patient sizes among the paediatric population,
23 several age, size or weight groups are needed to establish the DRLs, and there has been little
24 consistency in grouping of the patients. Extensive patient dose surveys are needed to establish
25 DRLs but there has been no detailed guidance on how to carry out and report such surveys in order
26 to ensure consistent methods and comparability of the DRLs, in particular for reliable evaluation of
27 DRLs for use at a European level.

28

29 In these Guidelines, basic recommendations on how to establish and to use DRLs for paediatric x-
30 ray examinations and procedures have been given. DRLs for the paediatric examinations and
31 procedures given in Section 6 should be established and used in accordance with the
32 recommendations given in Sections 7-9.

33

34 The main recommendations of Section 6 are summarized as follows:

35

- 36 • All examinations resulting in high collective doses should have DRLs. This can include both
37 the most common low dose examinations and the less common high dose examinations. It is
38 acknowledged that other common very low dose procedures (e.g. dental) should also be
39 optimised.
- 40 • The application of DRLs should be the responsibility of all providers of X-ray imaging. This
41 means that DRLs should also be applied to imaging performed outside the radiology
42 department, including cardiology, orthopaedic surgery, gastroenterology, intensive care (line
43 placement), neurology, vascular surgery, etc. Specific considerations may also be
44 appropriate for imaging associated with radiation therapy where the purpose and scope of
45 imaging can be different.
- 46 • The list of radiography, fluoroscopy and CT examinations where DRLs are recommended
47 are given in Tables 6.2 and 6.3. DRLs should be defined separately for different indications
48 if these require different image quality.

- For IR procedures, the development of LDRLs should be encouraged and the feasibility of NDRLs and EDRLs should be studied. The main focus should initially be to establish LDRLs for local guidance where the number of variabilities a priori is smaller. LDRLs between centres should then be compared and the reasons for the large differences should be studied, to be able to decide if NDRLs and EDRLs are appropriate. In Section 6.3, a few IR procedures have been specified where DRLs (at least LDRLs) could be established:
- As a note for emerging or increasing new practices, DRLs established for conventional CT should be applied to the CT part of hybrid imaging when the CT is used for diagnostic purposes. There is also a need to develop DRLs for paediatric cone beam CT (CBCT) examinations.

The main recommendations of Section 7-9 are summarized as follows:

- The physical *quantity* used to establish DRLs should be an easily measurable quantity, usually directly obtainable from the x-ray equipment console, obtained either by manual recording or preferably by automatic recording and analysis. Organ doses and effective dose are not considered feasible as a DRL quantity because these cannot be easily determined. The following quantities are recommended (see the list of symbols and abbreviations in Annex H):
 - Radiography: P_{KA} (primary quantity) and $K_{a,e}$ (useful additional quantity)
 - Fluoroscopy: P_{KA} (primary quantity), $K_{a,r}$, fluoroscopy time and number of images (useful additional quantities)
 - Computed tomography: $CTDI_{vol}$ and DLP, determined for a 32 cm phantom (all body CT examinations: chest, abdomen, trunk and spine) and for a 16 cm phantom (head CT examinations); besides $CTDI_{vol}$, when available, SSDE can be used for all body CT examinations
 - IR: P_{KA} (primary quantity), $K_{a,r}$, fluoroscopy time and number of images (useful additional quantities)
- The values used for patient dose monitoring, at the display unit and in the DICOM header should be *regularly calibrated or checked* for all beam qualities used in clinical practice. In particular, such calibrations or checks should be made prior to comparison with NDRLs and also prior to submission of data as part of national dose collection.
- The *parameters to group the patients* should be patient weights for all body examinations and patient ages for all head examinations (this recommendation might not be valid for some examinations where little experience on DRLs exist, e.g. for IR, IC and dental procedures). For body examinations, in the transition period until data from weight-based patient dose surveys becomes available, age can be used as an additional grouping parameter and for the purpose of comparing proposed new weight-based DRLs with earlier age-based DRLs (trend analysis). For the comparison purposes, an approximate equivalence of the average weight and age groups can be deduced from the weight-for-age charts as shown in Table 7.2.
- Grouping of patients should be carried out with *intervals* as follows (Table 7.1):
 - Weight groups for body exams: < 5 kg, 5 - < 15 kg, 15 - < 30 kg, 30 - < 50 kg, 50 - < 80 kg. The recommended first weight group (< 5 kg or neonates) applies to newborn babies but does not apply to those in incubators.
 - Age groups for head exams: 0 - < 3 months, 3 months - < 1 y, 1 - < 6 y, ≥ 6 y
- The DRLs can also be given as a *DRL curve* by expressing the DRL quantity as a continuous function of the grouping parameter (e.g. DLP as a function of patient weight) provided the collected data for setting of the DRLs indicates a clear relationship between patient doses and the grouping parameter. This approach can help to overcome the problem

1 of poor statistics when it is difficult to find adequate patient dose data for each discrete
2 group.

- 3 • The DRLs should be based on sufficient *patient dose data* determined or collected from the
4 records of individual paediatric patients. Using data obtained only from typical protocol data
5 or from measurements in phantoms is not recommended.
- 6 • National DRLs (NDRLs) should be based on national patient dose surveys with a
7 *representative sample* of all radiological institutions and all types of equipment and
8 practices in the country when practical. DRLs based on very limited surveys or on
9 measurements only in phantoms, as well as DRLs adopted from international
10 recommendations, such as these Guidelines (EDRLs) or from other countries, should only
11 be used as preliminary values until data from the relevant patient dose surveys is available.
12 For local DRLs (LDRLs), the sample should include data from all types of equipment used
13 in the hospital or a group of hospitals.
- 14 • For NDRLs, by definition, the 3rd quartile or the 75th *percentile* value of the median (the
15 50th percentile) values of the distributions of patient doses obtained from a representative
16 sample of radiology departments in the country should be determined, for a defined clinical
17 imaging task (i.e., common indication based protocol) surveyed for standardised patient
18 groupings. To provide a better goal of optimisation for those institutions with new
19 technology using advanced dose reduction techniques, the median or 50th percentile from the
20 same distribution of patient doses should be provided as an additional tool for optimisation.
- 21 • For the setting of DRLs, statistically relevant numbers of patient dose data should be
22 collected. From each hospital or radiology department a representative sample of at least 10
23 patients per procedure type and per patient group is recommended for non-complex
24 examinations such as radiography and CT, and at least 20 patients per procedure type and
25 per patient group for complex procedures such as fluoroscopy and fluoroscopically guided
26 procedures.
- 27 • In collecting the patient dose data for the DRLs, likewise in daily imaging practices, there
28 should always be a system in place to judge whether *image quality* is adequate for the
29 diagnosis according to the indication of the examination. This could be based, e.g., on image
30 quality assessment of typical test cases by several radiologists. The image quality
31 requirement should be based on clinical grounds only.
- 32 • Due to the generally large amount of data needed and the large amount of potential errors
33 when these data are to be collected during routine practice, *automatic data collection* is
34 recommended wherever possible.
- 35 • Besides the actual patient dose data according to the recommended patient grouping, *other*
36 *data from the examination characteristics* (e.g. x-ray equipment type, exposure parameters,
37 use of AEC) should be collected for the evaluation and decision making when DRLs are to
38 be established.
- 39 • Patient dose surveys for the basis of setting the NDRLs, should be *conducted* by the
40 authoritative body which sets the DRLs or by another competent institution, with the
41 *collaboration* of national professional/scientific societies or at least having recognized
42 clinical experts as consultants in the process.
- 43 • The complete *history of the patient dose surveys* for the setting of DRLs, including all
44 essential dosimetric and statistical information (e.g. quantities and their collected values,
45 coverage of institutions and practices, sample sizes) should be *documented* and preferably
46 reported.
- 47 • NDRLs should be *set by an authoritative body*, i.e. competent national authorities such as
48 national radiation protection or health authorities, or specific institutions established and
49 authorized by competent national authorities.

- 1 • *Instructions* on how to make use of the NDRLs or LDRLs (the purpose of the DRLs,
2 recommended frequencies for comparison of the local dose levels with DRLs, the sample
3 sizes recommended for comparison etc.) should always be provided with the DRLs.
- 4 • The *comparison* of patient dose levels of a hospital or a group of hospitals with LDRLs or
5 NDRLs should be carried out at the minimum frequency of once per year. A median value
6 of the patient dose distribution should be used to compare against the DRL, determined from
7 a sample of at least 10 patients per patient group from each hospital. In cases where a DRL
8 curve is used, a sample of at least 10 patients per DRL curve is recommended, distributed
9 throughout the range of the patient grouping parameter. Automatic dose
10 management/monitoring systems can enable frequent comparisons.
- 11 • Whenever the DRLs are consistently exceeded, appropriate *investigations* to identify the
12 reasons, and *corrective actions* to improve the clinical practice, if necessary and feasible,
13 should be taken without undue delay.
- 14 • The use of the DRLs, including all findings and subsequent corrective actions should be
15 *documented* and made available for clinical audits (internal or external audits) and for
16 regulatory inspections by competent authorities.
- 17 • DRLs should be *updated regularly*. NDRLs should be reviewed and updated at least every 5
18 years. LDRLs should be reviewed and updated at least every 3 years and when there are
19 changes of equipment or practices which have a potential impact on patient dose levels.
- 20 • The NDRLs should be compared with available EDRLs whenever either of the values have
21 been established or updated and consideration given to the need for further optimisation if
22 the NDRLs are higher than the EDRLs.

23
24 It is strongly recommended that DRLs should be based on patient dose surveys and should
25 sufficiently cover all types of the most common high dose (or where the collective dose to the
26 population is significant) paediatric radiology practices in a healthcare facility or group of
27 healthcare facilities (for LDRLs) or in the country (for NDRLs). As discussed in Section 6, different
28 image quality requirements should be taken care of by using indication based DRLs where
29 appropriate. To facilitate the establishment of DRLs and their frequent updating, the use of
30 automatic dose collection systems is highly recommended whenever possible. The implementation
31 and the results of patient dose surveys, and the subsequent procedures to establish DRLs, should be
32 documented in a way that enables reliable comparison of DRLs. This will allow trends in their
33 development to be followed-up and possibly established as European-wide preliminary levels where
34 national DRLs have not yet been established.

35
36 Based on the critical review of all paediatric national DRLs set by authoritative bodies in European
37 countries, including proposed national values not yet accepted by an authoritative body and also
38 some relevant data from published nationwide patient dose surveys, a few European DRLs have
39 been suggested for radiography, fluoroscopy and CT (Section 10). For fluoroscopy-guided
40 paediatric interventional procedures, it has not been possible to propose EDRLs due to the lack of
41 published NDRLs (paediatric cardiac procedures) or any DRLs (paediatric non-cardiac procedures).
42 However, information on published studies on LDRLs and on the limited patient dose collection in
43 the context of the PiDRL project has been presented in Annex G.

44
45 It is concluded (Section 10) that all the given EDRLs should be considered only as the preliminary
46 choice for the NDRLs, until appropriate national patient dose surveys have been carried out and
47 NDRLs based on these surveys have been established by an authoritative body. In particular, patient
48 dose surveys and further research in coming years is needed for IR procedures, to study the
49 feasibility of NDRLs and EDRLs for interventional procedures and to establish such DRLs when
50 possible.

1. Background

Tremendous growth in the use of computed tomography (CT) and interventional radiology (IR) procedures has taken place over the last 15 years. Radiological imaging of children, some organs of whose are particularly sensitive to radiation, has been shown to be among the fastest growing areas in the last few years. In 1999, the European Commission issued Radiation Protection 109 (RP 109), 'Guidance on diagnostic reference levels (DRLs) for medical exposure'. This document highlights the importance of establishing DRLs for high-dose medical examinations, in particular CT and IR, of patients sensitive to radiation, especially children. The approach most commonly used for adults has been that of average sized adult phantom or standard phantom. The same approach has not been considered appropriate for children in view of the wide variation in body habitus.

Despite a large number of studies available from European countries, European DRLs for paediatric patients are only available for some common radiological examinations. Hence, there was a need to consolidate what is available and to provide guidance on what actions are needed in using DRLs to further enhance radiation protection of children. The European Commission recognised this need and launched the PiDRL project on the establishment of European DRLs for paediatric patients in December 2013.

This 27-month tender project was awarded to a consortium, which is headed by the European Society of Radiology (ESR). Other participating organisations are key European stakeholders and professional groups with relevance to radiation protection of paediatric patients:

- European Society of Paediatric Radiology (ESPR)
- European Federation of Radiographer Societies (EFRS)
- European Federation of Organisations for Medical Physics (EFOMP)
- Finnish Radiation and Nuclear Safety Authority (STUK) with Luxembourg Institute of Science and Technology (LIST) as subcontractor

The PiDRL project aimed at:

- Agreeing on a methodology for establishing and using DRLs for paediatric imaging.
- Updating and extending the European DRLs to cover more procedures and a wider patient age/weight-range based on current knowledge.

The project's work was coordinated with the parallel work of the International Commission on Radiological Protection (ICRP) on DRLs in medical imaging, with an attempt to ensure consistent use of the concepts.

The project's work included three major tasks:

1. Developing European Guidelines on DRLs for paediatric imaging covering plain radiography, fluoroscopy, CT and IR procedures (Work Package 1)
2. Deciding on European DRLs for the main paediatric imaging procedures, involving plain radiography, fluoroscopy, CT, IR and as far as possible, examinations using mobile equipment, e.g. on neonates (Work Package 2)
3. Organising a European workshop to discuss the results of the first two tasks and the need for further action on DRLs and the optimisation of radiation protection of paediatric patients (Work Package 3). This workshop was held at the Lisbon School of Health Technology in Portugal on October 15-17, 2015.

1 **2. Introduction**

2 Diagnostic reference levels (DRLs) have been recommended by the International Commission on
3 Radiological Protection (ICRP) (ICRP, 1991; 1996; 2001; 2007a; 2007b; 2013) as an advisory
4 measure to improve optimisation of patient protection, by identifying high patient dose levels which
5 might not be justified on the basis of image quality requirements. DRLs should be set for common
6 examinations using easily measurable dose quantities. National DRLs are usually set by a
7 collaboration of authorities and professional societies, typically using a percentile point (most
8 commonly 75% or the 3rd quartile) of the observed distribution of patient doses in the country.
9 ICRP has also stated (ICRP 2001) that DRLs specific to clinical indications (clinical protocols) are
10 desirable. Consequently, in several groups of examinations, mainly of the adult population, DRLs
11 have become a valuable tool in the optimisation of the procedures.

12
13 The European Council Directive 2013/59/Euratom Basic Safety Standards (BSS) (EC, 2013;
14 repealing five earlier directives including 97/43/EURATOM, 1997), Article 56, requires that
15 "Member States shall ensure the establishment, regular review and use of DRLs for radiodiagnostic
16 examinations, having regard to the recommended European DRLs where available, and when
17 appropriate, for interventional radiology (IR) procedures, and the availability of guidance for this
18 purpose". In 1999 the Commission issued Radiation Protection 109 (RP 109; EC, 1999), "Guidance
19 on diagnostic reference levels DRLs for medical exposure". RP 109 document highlighted the
20 importance of establishing DRLs for high-dose medical examinations, in particular computed
21 tomography (CT) and IR procedures and for patients groups that are more sensitive to radiation,
22 especially children. However, RP 109 quoted paediatric DRLs only for several plain radiography
23 examinations of standard sized five-year old patients.

24
25 Accumulating evidence from the last decade shows a tremendous growth in the use of CT
26 examinations and IR procedures i.e. fluoroscopy-guided interventional procedures including cardiac
27 procedures. A further significant change has been the transition from conventional film-screen to
28 digital radiology. The importance of the need for DRLs in CT is also highlighted by the fact that
29 exposures from CT examinations contribute a major part of the population dose from all diagnostic
30 uses of radiation (EC, 2014). Radiological imaging of children is among the fastest growing in the
31 last decade (UNSCEAR, 2013). Paediatric examinations and procedures are of special concern
32 because, compared to adults, children have a higher risk from the detrimental effects of radiation.
33 Increased incidence of cancer after CT examinations in childhood has been reported in recent years
34 (Pearce et al, 2012, Matthews et al, 2013, UNSCEAR, 2013, Krill et al., 2015). Because of the
35 limitations of the epidemiological studies so far, there is no indisputable evidence to determine the
36 risk of cancer related to radiation received from diagnostic and interventional procedures (Journy et
37 al. 2014, Harvey et al. 2015, Boice 2015). However, our present knowledge emphasises the
38 significance of justification and dose optimisation in paediatric radiology (see e.g. IAEA, 2012).

39
40 Despite the recommendations and the clear need for DRLs for paediatric examinations, few
41 paediatric DRL data are available and they are only set in a small number of countries within
42 Europe. The reasons for this are many-fold: the number of paediatric examinations is lower than
43 adults; patient dose levels vary considerably as a function of age, size or weight of the patients and
44 therefore, DRLs for several age, size or weight groups need to be defined; due to the lack of
45 standardisation of these groups, the comparison of DRLs or patient dose data with other countries is
46 not straightforward; due to the general paucity of patient dose data for paediatric examinations, it is
47 often difficult to collect sufficient data to establish DRLs, or to compare local values with
48 established DRLs, for each age or weight sub-group. Patient dose surveys are needed to establish
49 DRLs, and there is little guidance on the statistical requirements for such surveys and on how to

1 derive the DRL values. Special challenges may be introduced by different institutions, e.g. the
2 procedures in a specialty cancer centre might require different DRLs compared to those in a more
3 general institution. Further, the rapidly evolving technology may complicate the establishment of
4 DRLs.

5
6 There are continuing efforts to develop DRLs throughout Europe as will be shown in Section 5. For
7 example, DRLs for paediatric CT examinations have been established or studied in several
8 European countries including Germany, France, the UK, Switzerland, Greece, Belgium, Finland,
9 Lithuania, Estonia, Portugal, Ireland, Spain, the Netherlands and Italy. In some countries, patient
10 dose surveys and proposals for national paediatric DRLs have been made but the proposed values
11 have not been confirmed or officially set by an authoritative body. Furthermore, no guidelines are
12 available on how to measure, collect and process the data needed for establishing paediatric DRLs.

13 It is clear that studies designed to establish DRLs should follow a methodology that allows
14 meaningful comparison of DRL values. Unfortunately, this is not the case. For example, some
15 studies on paediatric CT DRLs express results in Computed Tomography Dose Index (CTDI) using
16 the 16 cm standard dosimetry phantom for both head and trunk paediatric examinations and some
17 other studies use the 16 cm dosimetry phantom for head and neck and the 32 cm dosimetry phantom
18 for trunk paediatric examinations. Protocols and patient groupings also differ considerably amongst
19 CT DRL studies. Studies on radiographic and fluoroscopic DRLs have similar issues. All studies
20 designed to establish DRLs should follow a methodology that allows meaningful comparison of
21 DRL values, and of local dose values, to these national DRLs.

22

23 **3. Purpose and scope**

24 The purpose of these Guidelines is trifold:

- 25 • to recommend a methodology for establishing and using DRLs for paediatric
26 radiodiagnostic imaging and IR practices,
- 27 • to update and extend the European DRLs for these examinations where sufficient experience
28 and data are available for a consensus on DRL values,
- 29 • to promote the establishment and use of DRLs in paediatric radiodiagnostic imaging and IR
30 practices so as to advance optimisation of radiation protection of paediatric patients.

31

32 The Guidelines cover all types of examinations and procedures in paediatric radiodiagnostic x-ray
33 imaging: plain radiography, fluoroscopy, CT and IR practices. The focus of the Guidelines is on
34 CT, IR and digital projection imaging.

35

36 The Guidelines do not deal with paediatric imaging in nuclear medicine to avoid duplicating and
37 potentially disrupting the work that has already been extensively undertaken by national and
38 European societies and organisations.

39

1 **4. Definitions**

2 In this document, *patient dose* means the value of the dosimetric quantity indicated by, or
3 determined from the display of the X-ray equipment.

4
5 The concept of DRLs was first introduced by the ICRP (ICRP, 1991), and later on further
6 elaborated in other recommendations by the ICRP (ICRP, 1991; 1996; 2001; 2007a; 2007b).
7 According to the ICRP (ICRP 103), a DRL is a form of investigational level, applied to an easily
8 measured quantity, and intended for use as a simple test for identifying situations where the levels
9 of patient dose are unusually high or low. The objective of DRLs is to help avoid radiation dose to
10 the patient that does not contribute to the clinical purpose of a medical imaging task (ICRP 105).
11 Collection of patient dose data for the purpose of setting DRLs should include an assessment of
12 image quality to ensure relevance of the data; the image quality should be the minimum that meets
13 the need of the clinical question. Image quality that exceeds the clinical requirement leads to
14 unnecessary high patient dose levels.

15
16 In the EU Basic Safety Standard (BSS), DRLs are defined as:
17 “dose levels in medical radiodiagnostic or IR practices, or, in the case of radio-pharmaceuticals,
18 levels of activity, for typical examinations for groups of standard-sized patients or standard
19 phantoms for broadly defined types of equipment”.

20
21 In principle, different generations of given imaging equipment (e.g. CT scanner) may affect the
22 patient dose level significantly and thus, different DRLs for different generations might be
23 suggested. However, this can be too complicated in practice and DRLs usually cover all generations
24 of given equipment (“broadly defined types of equipment”). Due to the possible effect of equipment
25 development on patient doses, it would be important to ensure frequent update of the DRLs.

26
27 For IR, the term “diagnostic reference level” is used in these Guidelines in accordance with the
28 terminology adopted by the ICRP and the EU BSS, even though IR encompasses both diagnostic
29 and therapeutic procedures.

30
31 According to the ICRP recommendations (ICRP 2001, 2007a) a DRL is not to be used to implement
32 constraints on individual patient doses, and it is not for regulatory or commercial purposes.

33
34 DRLs help ensure that the doses delivered to patients are in accordance with the ALARA principle
35 (as low as reasonable achievable). Examination-specific DRLs can provide the stimulus for
36 practices to monitor and promote improvements in patient protection. It can therefore be expected
37 that, within the paediatric radiology community, paediatric DRLs will increase dose awareness and
38 will make paediatric practices more actively manage the required imaging quality that patients need.

39
40 For the purpose of these Guidelines, DRLs are further categorized in three sub-types as follows:

41
42 *Local DRL*

43
44 A local DRL (LDRL) is based on the 3rd quartile (the 75th percentile) value of the
45 distribution of patient doses obtained from radiology departments in a single large
46 healthcare facility or a group of healthcare facilities, for a defined clinical imaging
47 task (i.e., common indication based protocol) surveyed for standardised patient
48 groupings.

1 *Note 1:* If a large group of healthcare facilities are involved, it would be appropriate to
2 use the 75th percentile of the distribution of median values obtained from the facilities,
3 but if just a small group (2-4) of healthcare facilities are involved or one large
4 healthcare facility, then it would be appropriate to use the 75th percentile value of the
5 patient dose distribution (pooled distribution).

6 *Note 2:* The 75th percentile has been chosen to be consistent with the definition of
7 National DRLs.

8 *Note 3:* The 50th percentile value of patient dose distributions obtained from each
9 radiology department should regularly be compared with LDRLs (Section 9.1.1).

10 11 *National DRL*

12
13 A national DRL (NDRL) is based on the 3rd quartile (the 75th percentile) value of the
14 median (the 50th percentile) values of the distributions of patient doses obtained from
15 a representative sample of radiology departments in the country, for a defined clinical
16 imaging task (i.e., common indication based protocol) surveyed for standardised
17 patient groupings.

18 19 *European DRL*

20
21 A European DRL (EDRL) is based on the median (the 50th percentile) value of the
22 distribution of the NDRLs for a defined clinical imaging task (i.e., common indication
23 based protocol) surveyed for standardised patient groupings.

24
25 *Note 1:* The median value of the NDRLs has been chosen to represent the EDRLs as
26 opposed to taking the 75th percentile values because the NDRLs already represent 75th
27 percentile dose values.

28 *Note 2:* This definition for the EDRL has been adopted because of the scarceness of
29 data for EDRL evaluation. It was not possible to establish the EDRLs on single
30 surveys of a representative sample of facilities drawn from European countries.
31 Further, there was no sufficient basis to calculate the EDRLs by weighting national
32 DRL values according to the population of each participating country.

33
34 If the NDRLs exceed the proposed EDRLs, the reasons for the differences should be considered. In
35 particular, if the NDRLs are not based on recent national patient dose surveys, the need for new
36 surveys to update the NDRLs should be considered. This can lead to greater improvements with
37 further reductions in patient doses.

38
39 Further information on the use of these three DRLs is given in Section 9.

1 **5. Review of existing paediatric DRLs**

2 **5.1 Introduction**

3 A review of existing paediatric DRLs has been carried out by a follow-up questionnaire to
4 European countries and by a comprehensive literature review. The information gained has been
5 used to identify the existing status of paediatric DRLs with an emphasis on their application in
6 European countries. Data from this review has also been the basis for the recommendations in
7 Sections 6-10.

8
9 A short summary of the review is presented in this section. Details of the review and the results are
10 presented in Annex C.

11 12 **5.2 Methods of review**

13 National DRLs set by an authoritative body in European countries were reviewed in 2010-11 in the
14 Dose Datamed 2 (DDM2) project (EC, 2014), including DRLs for paediatric examinations. For the
15 present Guidelines, the data on paediatric DRLs stored in the DDM2 database was verified
16 (confirmed and supplemented) by use of a questionnaire, sent to the contact persons of 36 European
17 countries according to the list of contacts established in the DDM2 project and updated for the
18 present purpose.

19
20 Furthermore, a worldwide review of literature on patient doses and DRLs for children of different
21 age groups, or other distributions, and for different examinations was carried out with an emphasis
22 on peer reviewed papers, and reports from authoritative bodies, within Europe. For the output of
23 this review, a database of literature was created, classified in suitable headings, using the Mendeley
24 (www.mendeley.com) platform. The resulting database [consolidated on 25 February 2015]
25 contains 215 articles. For articles reporting on DRLs in European countries, the correspondence of
26 this data with the results of the above questionnaire was checked and the information from the two
27 sources combined.

28 29 **5.3 National DRLs for paediatric exams set in the European countries**

30 The summary of the national DRLs for paediatric exams set by an authoritative body in the
31 European countries is shown in Table 5.1, and the values of these national DRLs are given in
32 Annex A. A more detailed summary, including available information on patient dose surveys and
33 on the setting of the national paediatric DRLs in European countries is compiled in Annex C.

34
35 National paediatric DRLs are provided for some groups of examinations (radiography, fluoroscopy
36 or CT) in 17 countries, i.e. in 47 % of the European countries. In Lithuania and Belgium, the DRLs
37 had been set very recently and were not included in the DDM2 database. In 9 countries (AT, BE,
38 DE, DK, ES, FI, LT, NL and UK) all available national DRLs are based on own patient dose
39 surveys covering several radiology institutions. In 6 countries (CY, LU, PL, RO, CH, IT), the
40 available national DRLs are adopted from published values; in 5 countries (CY, LU, PL, RO, IT)
41 from the EC guidance (EC, 1999) and in Switzerland from published values in another country
42 (DE). In Ireland national DRLs are based on own survey for some CT and radiography
43 examinations, other values are adopted from the UK. In France, the national DRLs are based on
44 collected data, protocol data or adopted from literature. A general observation from the review is
45 that it is difficult to keep the DRLs up-to-date.

46
47 For IR, no national paediatric DRLs have been set for any procedures in any European country.

1 For national DRLs in radiography, fluoroscopy and CT, there seems to be reasonable agreement on
2 the examinations for which DRLs have been needed: skull, chest, abdomen and pelvis in
3 radiography, urinary tract (micturating/voiding cystourethrography, MCU/VCU) in fluoroscopy,
4 and head, chest and abdomen in CT.

5
6 A reasonable agreement prevails also on the quantities used: air kerma-area product or dose-area
7 product and/or entrance-surface air kerma, entrance-surface dose or incident air kerma in
8 radiography, air kerma-area product or dose-area product in fluoroscopy, and dose-length product
9 or air kerma-length product and volume CT air-kerma index in CT. The DRL quantities and their
10 symbols are summarized in Table 5.2. Air kerma at the patient entrance reference point is a possible
11 additional quantity for DRLs in fluoroscopy and IR but has not been applied so far.

12
13

1 Table 5.1. Summary of existing national DRLs in European countries, set or accepted by an
 2 authoritative body, based on the results of the questionnaire and the literature review. Coloured
 3 cells: data accepted for EDRL calculation (c.f. Table 10.1).
 4

Country	Source of DRL values	Radiography		Fluoroscopy	CT		References
		$K_{a,e}$ (ESD, ESAK), $K_{a,i}$ (IAK)	P_{KA} (KAP, DAP)	P_{KA} (KAP, DAP)	DLP (P_{KL})	$CTDI_{vol}$ (C_{vol})	
AT	Own survey		Skull (AP/ PA, LAT) Thorax (AP/PA) Abdomen (AP/PA)	MCU	Brain Chest		Questionnaire (all). Billiger et al. 2010 (radiography)
BE	Own survey		Thorax (PA, PA+LAT) Abdomen		Brain Sinus Thorax Abdomen	Brain Sinus Thorax Abdomen	www.fanc.fgov.be
DE	Own survey		Head (AP, PA, LAT) Thorax (AP, PA, LAT) Abdomen (AP) Pelvis	MCU	Head Facial bones Thorax Abdomen	Head Facial bones Thorax Abdomen	Questionnaire. Bundesamt für Strahlenschutz, 2010.
DK	Own survey	Thorax (AP, PA, LAT) Pelvis (AP) Overview of abdomen		MCU			Questionnaire.
ES	Own survey		Head (AP) Thorax (PA) Abdomen (AP) Pelvis (PA)	MCU	Head Chest Abdomen		Ruiz-Cruces, 2015
FI	Own survey	Sinuses (Waters projection) (discrete values) Thorax (AP, PA, LAT) (DRL-curve)	Sinuses (Waters projection) (discrete values) Thorax (AP, PA, LAT) (DRL-curve)	MCU	Head (discrete values) Thorax, abdomen (abd. + pelvis), WB (chest+abd. +pelvis) (DRL-curve)	Head (discrete values) Thorax, abdomen (abd. + pelvis), WB (chest+abd. +pelvis) (DRL-curve)	Questionnaire. Kiljunen et al., 2007. Järvinen et al. 2015.
LT	Own survey	Chest (PA) Skull (AP/PA, LAT) Abdomen	Chest (PA) Skull (AP/PA, LAT) Abdomen		Head		Questionnaire.
NL	Own survey		Thorax (AP, PA) Abdomen (AP)	MCU	Head	Head	Questionnaire.
UK	Own survey			MCU Barium meal Barium swallow	Head Chest	Head Chest	Hart et al. 2012 (F). Shrimpton et al., 2006, 2014 (CT).
IE	Own survey for some radiography and CT examinations. Other values adopted from other countries.	Skull (AP, LAT) Chest (AP/PA) Abdomen (AP) Pelvis (AP)		MCU Barium meal Barium swallow	Brain Abdomen/Pelvis		Questionnaire. Medical council, 2004. HSE Medical Exposures Radiation Unit, 2013.
FR	Own survey for radiography, CT data based on protocol data or literature	Thorax (AP, LAT) Pelvis	Thorax (AP, PA, LAT) Abdomen (AP) Pelvis		Brain Facial Bone Petrous Bone Chest Abdomen+Pelvis	Brain Facial Bone Petrous Bone Chest Abdomen+Pelvis	Questionnaire. Roch et al., 2012.
CY	Adopted (EC)	Head (AP, PA, LAT) Thorax (AP, PA, LAT) Abdomen Pelvis (AP)					Questionnaire.
IT	Adopted (EC)	"					Questionnaire
LU	Adopted (EC)	"					Questionnaire.
PL	Adopted (EC)	"					Questionnaire.
RO	Adopted (EC)	"					Questionnaire.
CH	Adopted (DE)				Brain Face, nasal cavity Thorax Abdomen Lumbar spine	Brain Face, nasal cavity	Questionnaire.. Galanski and Nagel, 2005

5
6

1 Table 5.2. Quantities used for DRLs and their symbols. The symbols used in these guidelines (the
 2 second column) are in accordance with the latest publications of the ICRP (2016) and the ICRU
 3 (2012). See also ICRU (2006) and IAEA (2007).
 4

Quantity	Symbol used in these guidelines	Other symbols used in literature	Closely similar quantity*
Incident air kerma	$K_{a,i}$	IAK	
Entrance-surface air kerma	$K_{a,e}$	ESAK	Entrance-surface dose (ESD)
Air kerma at the patient entrance reference point**	$K_{a,r}$	CAK	
Air kerma-area product	P_{KA}	KAP	Dose-area product (DAP)
Volume computed tomography dose index	$CTDI_{vol}$	C_{vol}	
Dose-length product	DLP	-	Air kerma-length product (P_{KL})

5 *Because “air kerma” and “dose in air” are numerically equal in diagnostic radiology energy range.

6 **Also names “cumulative dose”, “reference air kerma” and “reference point air kerma” have been used in the literature

7
 8 Most of the current national DRLs are based on the 3rd quartile method. In one case for CT, a 50 %
 9 level is given as supplementary information (FI) and in another case, a metric referred to as
 10 “achievable dose levels” was also given (NL). For patient grouping, a set of age groups up to 15
 11 years of age (0, 1, 5, 10, 15 y) is the most common practice. In one country (FI), a DRL curve with
 12 patient thickness (radiography) or weight (CT) as the parameter is used to overcome the problems
 13 of poor statistics with discrete groups. Most of the current national DRLs have been set by national
 14 authorities, based on patient dose data which is from 2 years to more than 10 years old. In one case
 15 (NL), the DRLs have been set by a national committee, which consists of members of several
 16 professional organisations. There is a large variation between countries on the number of
 17 institutions and patients included in the patient dose surveys. For user guidelines, typically, patient
 18 dose data is required from a minimum of 10 patients for each patient grouping with a comparison
 19 frequency between 1-5 years.
 20

21 It is evident that a rough consensus on the examinations for the DRLs and the DRL parameters
 22 (quantities, percentile of dose distribution, patient grouping) already exists or is closely achievable.
 23 However, better standardisation and guidelines would be of benefit, in particular for the patient dose
 24 surveys as the basis of setting DRLs.
 25

26 5.4 Studies and proposals on paediatric DRLs

27 Besides the NDRLs set by authoritative bodies for paediatric examinations and procedures, several
 28 studies have been published to propose NDRLs or to develop LDRLs for paediatric examinations,
 29 or to compare patient dose distributions between several countries. These studies are summarized in
 30 Annex C. The actual values of the proposed NDRLs, or of *selected* other DRLs, are presented in
 31 Annex B.
 32

33 For radiography and fluoroscopy, except for the few studies for NDRLs, the other published studies
 34 on paediatric DRLs are either dated or limited to a few centres so that they do not provide high
 35 quality input to the setting of European paediatric DRLs. Also the few studies outside European

1 countries had major limitations and could not be considered as the basis for European paediatric
2 DRL determination.

3
4 For CT, a small number of European publications have collected paediatric CT data, mostly to
5 propose NDRL values, using a range of different methodologies. In particular, studies varied
6 according to whether patient or phantom/protocol data was collected and how patients were
7 categorized into specific age ranges. The majority of studies outside European countries reported
8 local paediatric DRLs for a small number of centres and not national values. Age was the most
9 commonly used method to categorise paediatric patients but there was little consistency in terms of
10 the age categories used.

11
12 For paediatric interventional cardiology procedures, data concerning patient doses and DRLs are
13 still very scarce in Europe, and even scarcer outside Europe. Neither national nor regional DRLs are
14 available, only LDRLs are provided. The studies greatly differ in their methodology and
15 information provided, making comparisons very difficult.

16
17 For paediatric non-cardiologic interventional procedures, no studies are available on DRLs from
18 European countries. Data published outside Europe are extremely scarce and limited to common
19 vascular and enteric procedures. No data are available for embolization or sclerotherapy of vascular
20 malformations, neuroradiology procedures, arteriography, CT guided biopsies, and biliary IR.
21 Although relatively rare, these procedures can cause very high doses.

22 23 **5.5 Strengths and limitations of the available DRLs and systems for their establishment**

24 **5.5.1 Strengths of the available systems**

25 Review of the existing systems of paediatric DRLs (both NDRLs set by authoritative bodies and
26 published other proposals of NDRLs or LDRLs) has shown some strengths and benefits of their
27 establishment and use. There has been consistent understanding on what DRLs are needed: mainly
28 skull, thorax, abdomen and pelvis exams of radiography, MCU in fluoroscopy, and brain, chest and
29 abdomen in CT. The use of DRLs has helped to identify non-optimised practices and thus improve
30 optimisation. The observed reductions on DRLs over time (Shrimpton et al., 2014) may partly be
31 due to improved techniques. On the other hand, there are also cases where successive DRLs have
32 shown an increasing trend due to changes of technology and practices (Shrimpton et al., 2014), thus
33 indicating their capability to detect negative influences of technology changes on patient dose
34 optimisation and to trigger further studies and efforts for improved optimisation. As for the
35 technical details of DRLs, there has been relatively good consensus on the DRL quantities used, and
36 their values have been easily available from the equipment consoles.

37 38 **5.5.2 Shortcomings and limitations**

39 While there are clear benefits of establishing and using DRLs in paediatric radiology, these have not
40 been implemented in an optimal way, and there have been several shortcomings and limitations
41 justifying additional considerations and guidance to be given.

42
43 In general, despite the comprehensive review (questionnaire and literature search) the retrievable
44 data has not been sufficient e.g. for detailed analysis of the representativeness of the collected
45 patient dose data and consequently, for their reliability. While the physical quantity and the patient
46 grouping (mainly by age) selected for the DRL settings have usually been reported exactly, the
47 background information on the patient dose collection is often only briefly reported or not described
48 at all. Few reports provide exact information on the practical methods of data collection, and the

1 coverage of the imaging institutions (types, percentage of total) and the imaging practices have been
2 reported in only a few countries. Most probably, data was collected manually, occasionally not well
3 controlled, and possibly hampered by human errors. Few notes are available on the application of
4 automatic data management systems for data collection or how the use of the DRLs has been
5 specified. Published information is rarely available on the experiences of using paediatric DRLs and
6 on their feasibility in practice.

7
8 Despite the recognized importance and need for DRLs, less than half of the EU countries have set
9 DRLs for paediatric examinations, and there is a complete lack of paediatric DRLs in many
10 countries (it is noted that the new BSS (2013) which should be implemented by February 2018
11 requires Member States to ensure that DRLs are established). Only in about one fifth of the
12 countries are the existing DRLs based on own national patient dose surveys (less than half of the
13 countries with established DRLs). Furthermore, there has been a very slow updating of the existing
14 DRLs, in comparison with the rapid development of imaging technology. In most countries, the
15 established DRLs are the first ones ever implemented, and only in a few countries does information
16 exist on the trends with several successive DRLs. For the high dose procedures in IR, including
17 cardiac procedures, there is a complete lack of NDRLs; only some local efforts have been
18 published.

19
20 The patient dose surveys required for setting DRLs are resource demanding and time consuming, in
21 particular because the main methods of data collection still rely on manual or semi-manual due to
22 the lack, or non-compatibility, of automatic data management systems. Data analysis is also
23 difficult because there is often a lack of standardisation in the specification of a given examination.
24 This makes comparisons of DRLs difficult and sometimes not relevant. In some countries, the
25 infrastructure is not capable of estimating the frequencies of examinations or the proportion of
26 paediatric examinations from all (including adult) examinations, which would be useful
27 supplementary information when planning to establish paediatric DRLs. Patient dose surveys may
28 suffer from a low response rate unless good cooperation between authorities and professional
29 societies exists to promote the participation of healthcare institutions.

30
31 As discussed above, the review of current systems of DRLs has shown that there is an insufficient
32 recording of the procedures used to establish the DRLs, and the available information also reveals
33 large differences in approaches. There is a lack of consistency in patient groupings (age, weight or
34 other groups with a variety of options) and lack of clear recommendations on the dose quantities to
35 be used. Detailed guidelines are needed on how to organise patient dose surveys and how to
36 establish DRLs, e.g.:

- 37
- 38 • What sort of institutions should be included in the data collection/survey (public, private,
39 general or devoted paediatric)?
- 40 • What information is needed besides the actual patient dose data?
- 41 • What dosimetric quantities are to be used (e.g. should one use P_{KA} vs $K_{a,e}$ in radiography,
42 should one use effective dose, what is the role of Size Specific Dose Estimate (SSDE))?
- 43 • Should patients be grouped together by age, size or weight?
- 44 • What should be the granularity of such grouping?
- 45 • How are DRLs to be derived from the patient dose distribution (percentile point) etc.?
- 46 • How are DRLs used to review and improve clinical practice?
- 47

48 In more advanced setting of DRLs other questions arise such as how to deal with different
49 equipment generations and technologies and the different levels of implementation of automatic
50 dose saving systems.

1
2 The problem associated with the much lower frequency of paediatric examinations, compared with
3 adult examinations, and the subsequent problems of poor statistics because of the need to collect
4 data for several patient age, size or weight groups can be addressed by introducing the “DRL curve”
5 (Kiljunen et al., 2007; Järvinen et al. 2015). This approach can be particularly useful for small
6 institutions with a very low number of paediatric patients.
7

8 An easy and effective follow-up of patient doses and their comparison with DRLs still suffers from
9 the slow development or non-compatibility of automatic data management systems. The availability
10 of more compatible systems regardless of the type of x-ray equipment and the development of
11 institutions’ overall data management systems in the future could provide valuable support for the
12 implementation of DRLs, not only for occasional comparisons but for continuous patient dose
13 monitoring and comparisons, with appropriate practices to alert staff on any unusually high or low
14 dose levels.
15

16 **5.5.3 Accuracy and comparability of DRLs**

17 For the comparability of NDRLs between countries, in particular when trying to establish joint
18 DRLs for several countries (e.g., for European wide DRLs), the following points need to be
19 considered:
20

- 21 (1) *The accuracy of the dose values.* For the comparison and follow-up of patient dose levels as
22 a quality control measure, whatever patient dose quantity is selected, the equipment used has
23 to display appropriate values of this quantity to a known (calibrated) accuracy. For example,
24 experience has shown (e.g., Vano et al., 2008) that P_{KA} displays can easily have more than
25 50% error.
- 26 (2) *The representativeness of the collected patient dose data.* It is important that the samples of
27 data collected include data from various levels of institutions; small and big, public and
28 private, so that the established DRL is representative of all radiology practices in the
29 country. However, attention should be paid to exceptionally high differences of data from
30 some centres compared with the average data, in order to avoid the inclusion of biased data
31 from very old equipment or suboptimal practice.
- 32 (3) *The adequacy of collected patient dose data.* It is important that a sufficiently representative
33 number of institutions (compared with the total number) and reasonable samples of patients
34 per age/weight group from each institution are collected.
- 35 (4) *The data collection period.* The DRLs should be updated at regular intervals, based on new
36 patient dose surveys (see Section 8.2), because both the development of technology and the
37 imaging practices can change rapidly and have a large impact on the patient dose levels.
38 There is also both an expectation and practical evidence (e.g. Shrimpton et al., 2014) that
39 DRLs will tend to decrease over time during the course of their application, even though the
40 changes in technology or practices can sometimes have an opposite effect. Therefore, it
41 would not be appropriate to include in the evaluation, patient dose studies and DRLs which
42 are more than 5-10 years old.
43

44 Further, significant differences in the level of technology in the country, e.g. due to the differences
45 in the national income and available economic resources, may affect the patient dose level.
46 However, such differences are difficult to assess and cannot usually be taken into account.
47

1 The uncertainties caused by item (1) may be a relatively small factor in the overall comparability of
2 the DRLs, in particular because such errors can compensate each other in the nationwide evaluation
3 of data from several centres.
4

5 If the above conditions (1)-(3) can be ensured and (4) considered homogenous enough for the
6 evaluation of the median value of the national DRLs, e.g. to determine the European DRL (see
7 Section 4), the interquartile value (i.e., the ratio of 3rd and 1st quartiles) of the DRLs gives an
8 indication of their variability. High interquartile values indicates significant variation of the
9 practices which may be associated with different levels of optimisation. A high interquartile value
10 can also be used as a measure of the possible weakness in adopting the European DRL instead of a
11 DRL based on own national patient dose survey (see Annex F). The distributions of the NDRLs in
12 European countries and their impact on the feasibility of the European DRL are discussed in further
13 detail in Annex F.

1 **6. Need for modality specific paediatric DRLs**

2 In this section, the paediatric examinations and procedures with the greatest need for DRLs will be
3 presented separately for each imaging modality (radiography and fluoroscopy, CT and IR). The
4 information is derived from the data on existing DRLs (Section 5 and Annexes A-C), from the
5 results of specific questionnaires sent to selected paediatric institutions in European countries
6 (Annex D) and from literature on examination frequencies. The need for further studies to establish
7 DRLs is highlighted, based on the identified lack of patient dose surveys, together with the need for
8 DRLs on important present or emerging new imaging practices.
9

10 The need for a DRL is judged on the basis of collective dose to the paediatric population: all
11 examinations resulting in high collective doses should have DRLs. This can include both the most
12 common low dose examinations and the less common high dose examinations. Due to the observed
13 difficulties in setting paediatric DRLs, this has been used as the main criterion, but it is
14 acknowledged that other common very low dose procedures (e.g. dental) should also be optimised.
15

16 The lists of procedures given in this section are neither exhaustive nor prescriptive – countries or
17 local healthcare facilities may choose to establish DRLs for their practices that may be important
18 contributors to patient dose in their jurisdiction. Further, it should be stressed that the application of
19 DRLs should be the responsibility of all providers of X-ray imaging. This means that DRLs should
20 also be applied to imaging performed outside the radiology department, including cardiology,
21 orthopaedic surgery, gastroenterology, intensive care (line placement), neurology, vascular surgery,
22 etc. Specific considerations may also be appropriate for imaging associated with radiation therapy
23 where the purpose and scope of imaging can be different.
24

25 **6.1 Radiography and fluoroscopy**

26 Table 6.1 provides the list of radiography and fluoroscopy examinations where DRLs are
27 recommended. Only examinations that have an important contribution to the collective effective
28 dose have been included. Conventional chest examination is included, even though it is a relatively
29 low dose examination, because it is by far the most frequent paediatric radiography examination in
30 all countries and produces a significant contribution to the collective effective dose. No
31 examinations of extremities, even though these are the most frequent of all radiography
32 examinations, are included in Table 6.1 because of their very low dose and low contribution to the
33 collective effective dose.
34

35 There has been no attempt to define paediatric DRLs according to detailed indications, or the
36 complexity of the procedure.
37

1 Table 6.1 Radiography and fluoroscopic examinations where DRLs should be set (AP/PA means
 2 that the same DRL applies to both AP and PA projections).
 3

Anatomical region	Projection(s) or procedure
Radiography	
Head (skull)	AP/PA
	LAT
Thorax (chest)	AP/PA
Abdomen	Abdomen-pelvis AP
Pelvis	Pelvis/hip AP
Cervical spine	AP/PA
	LAT
Thoracic spine	AP/PA
	LAT
Lumbar spine	AP/PA
	LAT
Whole spine/Scoliosis	AP/PA
	LAT
Fluoroscopy	
Urinary tract	Micturating/Voiding cystourethrography (MCU/VCU)
Gastro-intestinal tract	Upper GE-examinations
	Contrast enema

4
 5
 6

6.2 Computed tomography

7 Table 6.2 gives the list of CT examinations for which DRLs are recommended. CT provides the
 8 highest contribution (typically up to 60 %) of the total collective effective dose from all paediatric
 9 medical imaging, and all the CT examinations of Table 6.2. are potentially high dose examinations.
 10 CT examinations of extremities are excluded from Table 6.2, because of their relatively low dose
 11 and low contribution to the collective effective dose.

12
 13 The CT examinations in Table 6.2 correspond to complete routine CT examinations. Multi-phase
 14 scanning is only used for special purposes, and a need for a DRL for such purposes should be
 15 considered separately. Pre-contrast scans are not needed in paediatrics (except bolus-tracking).

16
 17 Different image quality requirements should use indication based DRLs, e.g. defining the DRL for
 18 CT Head, indication: ventricular size.

19
 20 There is no attempt to define DRLs according to the complexity of the CT procedure.
 21
 22

1 Table 6.2. CT examinations where the DRLs should be set
2

Anatomical region	Procedure
Head	Routine
	Paranasal sinuses
	Inner ear/internal auditory meatus
	Ventricular size (shunt)
Neck	Neck
Chest	Chest
	Cardiovascular CT angiography
Abdomen	Abdomen (upper abdomen)
	Abdomen+pelvis
Trunk	Whole body CT in trauma
Spine	Cervical spine
	Thoracic spine
	Lumbar spine

3
4

5 **6.3 Interventional radiology (incl. cardiology)**

6 Interventional radiology (IR) covers a wide range of procedures – from several types of cardiac
7 interventions and procedures to non-cardiac procedures (fluoroscopy and CT guided) to vascular
8 access, treatment of thrombosed dialysis shunts, and embolization of tumours (e.g. central nervous
9 system) without any other treatment option. The questionnaire reported in Annex D did not address
10 paediatric IR, cardiac and non-cardiac, image guided procedures, and there are no similar statistics
11 available. However, there has been a significant increase in IR procedures during the last decade,
12 and although these procedures are less common in the paediatric population, they deliver high
13 radiation doses (see also Annex G). Radiation protection issues in interventional cardiology has
14 recently been addressed by the ICRP (ICRP, 2013), including the need for DRLs.

15
16 As shown in Section 5, no NDRLs exist for paediatric IR procedures, and LDRLs have been
17 published only for paediatric interventional cardiology (IC) procedures. The development of
18 LDRLs for these procedures should be encouraged and the feasibility of NDRLs and EDRLs should
19 be studied. For IR procedures, patient dose depends on several factors, including the maturity of the
20 patient (preterm, baby, child), the complexity of the specific situation, and the experience of the
21 medical staff. There will always be case based decisions and in these situations the use of DRLs is
22 not appropriate. DRLs may therefore only be feasible for a few standard procedures like diagnostic
23 cardiac catheterization (morphology, pressure measurements, oximetry, biplane guided cardiac
24 function assessment), interventional closure of cardiac septal defects or stent placements (e.g.
25 coarctation), and peripheral insertion of central catheters (PICC) or nephrostomy from non-cardiac
26 procedures. In Annex G, some information is presented on patient doses and published LDRLs for
27 IC procedures, and on the results of a limited survey within the PiDRL project for non-cardiac
28 procedures.

29
30 For IC procedures, the experiences presented in Annex G suggest that the establishment of a generic
31 DRL for all diagnostic procedures or for all therapeutic procedures might not be appropriate. In
32 particular, for therapeutic procedures, the observed variation of patient doses between different
33 types of procedures suggests the need for procedure-specific DRLs. This is further complicated by

1 the fact that several techniques may have been developed for the same procedure and there would
2 be a need to establish a DRL for each technique.

3
4 For non-cardiac IR, catheter placement and diagnostic procedures are usually completed with just a
5 single procedure with defined steps. For most of the other non-cardiac procedures, such as
6 embolization and sclerotherapy, it may be necessary to perform two, three or more procedures
7 within a few weeks, the steps of the procedure are not clearly defined, and the duration of a single
8 procedure can be very different according to the severity of the condition requiring the procedure.
9 Ultrasonic guidance in paediatrics is more often combined with fluoroscopy than in adults, and the
10 relative contribution of the two techniques widely varies with the clinical task and the experience of
11 the interventionalist. Consequently, setting DRLs for non-cardiac IR procedures might only be
12 possible for catheter placement and diagnostic procedures.

13
14 Due to the observed high variation of dose levels between various centres (see Annex G), the
15 feasibility of NDRLs (or EDRLs) is questionable. The main focus should therefore initially be to
16 establish LDRLs for local guidance where the number of variabilities a priori is smaller. LDRLs
17 between centres should then be compared and the reasons for the large differences should be
18 studied, to be able to decide if NDRLs and EDRLs are appropriate.

19
20 Based on the limited information available from the few published articles and the small-scale extra
21 surveys carried out within the PiDRL project, a few IR procedures have been specified where DRLs
22 (at least LDRLs) could be established:

- 23 • Cardiac procedures
 - 24 ○ Patent Ductus Arteriosus (PDA) occlusion
 - 25 ○ Atrial Septal Defect (ASD) occlusion
 - 26 ○ Pulmonary valve dilatation
 - 27 ○ Diagnostic cardiac catheterization
- 28 • Non-cardiac procedures
 - 29 ○ Peripherally inserted central catheter (PICC)

30
31 For the following non-cardiac procedures, further studies should be carried out to confirm the
32 feasibility of LDRLs:

- 33 • Embolization (arterio-venous malformation, trauma, iatrogenic, portal); there is probably a
34 need for anatomical separation (all excluding head+neck+spine); the DRL should include
35 the whole treatment in case of multiple sessions
- 36 • Embolization (arterio-venous malformation, trauma, iatrogenic) head/brain+neck+spine
- 37 • Sclerotherapy (vascular malformations, cysts); the DRL should include the whole treatment
38 in case of multiple sessions
- 39 • Arteriography (anatomical separation needed: head/neck, trunk, extremities)

40
41 The present very low or partially non-existing experience on DRLs in IR procedures does not allow
42 the determination of specific complexity levels of the procedures (to establish DRLs). However,
43 this aspect should be taken into consideration when patient dose surveys are conducted to study the
44 feasibility of establishing DRLs for specific complexity levels in IR procedures.

45 46 **6.4 Prospective need of DRLs for emerging or increasing new practices**

47 Emerging new or increasing practices for which the establishment of DRLs should be considered
48 include hybrid imaging (currently PET-CT and SPECT-CT) as well as cone beam CT (CBCT).
49 Besides these examples of practices, a challenge for the future development of DRLs could be to

1 distinguish and establish DRLs, within a given examination for a given anatomical region, for
2 different indications if these require considerably different image qualities.

3
4 Concerning the use of CT in hybrid imaging, limited effort has been taken to establish DRLs and
5 there is currently only one guideline available (Segall et al., 2010). It should be emphasized that the
6 DRLs established for conventional CT should be applied to the CT part of hybrid imaging when the
7 CT is used for diagnostic purposes (this is not relevant if CT is only used for the determination of
8 attenuation correction). This is important because the users in some nuclear medicine departments
9 might not be adequately aware of CT doses and their optimisation, and the use of DRLs could thus
10 improve their awareness and the overall optimisation of hybrid imaging.

11
12 *Cone Beam CT (CBCT)* represents an imaging modality introduced in recent years, and is used
13 especially in paediatric dental procedures (Ludlow and Walker, 2013, Noffke et al., 2011, Prins et
14 al., 2011, Schulze, 2013, Vassileva et al., 2013, EC, 2012). An effective dose of 0.05 mSv to
15 paediatric patients has been reported (Vassileva and Stoyanov, 2010), and doses in paediatric
16 procedures can be 36% higher than those for adults, mainly due to the higher relative position of the
17 thyroid gland (Ludlow and Walker, 2013). EC publication RP172 (SEDENTEX-CT report; EC,
18 2012) contains a strong recommendation on the need to establish DRLs for CBCT. Establishing
19 DRLs is also supported by the recent ICRP publication on CBCT (ICRP, 2015). These observations
20 suggest a need to develop DRLs for paediatric CBCT examinations.

21 22 **6.5 Need for further patient dose surveys**

23 To decide the need for further paediatric patient dose surveys to provide paediatric DRLs, the
24 following questions should be addressed:

- 25 • Which examinations or procedures (examination or procedure protocols) should have
26 DRLs?
- 27 • Which examinations or procedures have DRLs that are no longer relevant and need
28 updating?
- 29 • Which emerging new practices might need DRLs in the future?

30
31 The first question is discussed in Sections 6.1 -6.3 and the second question partly in Section 5 and
32 Annexes A-D. As evident from Section 5, most European countries have never established
33 paediatric DRLs or the DRLs have been established only for a few paediatric examinations. Patient
34 dose surveys are therefore needed to provide data for many examinations. Further, there is an
35 evident need for new patient dose surveys to update many of the existing NDRLs. The last question
36 is discussed in Section 6.4.

1 **7. Basic approach to paediatric DRLs**

2 The dose quantities and the grouping of patients recommended in this section are based on the
3 analysis of the present status and experiences on paediatric DRLs (Section 5), the identified need
4 for the DRLs (Section 6) and the discussions and consultations during the PiDRL project. The
5 general principles are presented followed by separate considerations for each modality (radiography
6 and fluoroscopy, CT, IR).
7

8 The recommended statistics and methods for the setting of the DRLs, i.e. the minimum data and the
9 selection of institutions for patient dose surveys, representativeness of samples, methods of data
10 collection and the percentile point selected at patient dose distribution, are discussed in Section 8.
11 The recommended methods of using DRLs, i.e. the minimum number of patient dose data for
12 comparison with DRLs, frequency of comparisons etc., are discussed in Section 9.
13

14 **7.1 General**

15 *The DRL quantity* should be an easily measurable quantity (ICRP 1996, 2007b), usually directly
16 obtainable from the x-ray equipment console, obtained either by manual recording or preferably by
17 automatic recording and analysis (Section 8.4). The quantity should reflect the changes in the
18 patient dose level with different selections of the imaging parameters and imaging practices, thus
19 enabling follow-up of the patient dose level when using similar equipment, and also enabling
20 comparisons with other equipment, rooms or institutions for the same examination or procedure. It
21 is however well known that different beam qualities or acquisition geometries in radiography and
22 fluoroscopy can result in very different organ doses even when the P_{KA} values are the same. The
23 same applies for CT if tube voltage or bow tie filter is adjusted. It would be advantageous if the
24 quantity is closely related to the real patient dose: organ doses or whole body doses approximated
25 by effective dose. However, organ doses and effective dose are not considered feasible as a DRL
26 quantity because these are not measurable and their use also introduces extraneous factors that are
27 not needed or pertinent for the purpose of DRLs.
28

29 The DRLs should be based on sufficient patient dose data determined or collected from the records
30 of individual paediatric patients (for more details of the recommended patient dose surveys, see
31 Section 8). Using data obtained from typical protocol data or from phantom measurements to
32 determine DRLs are not recommended because the data should take into account the technical
33 settings and characteristics of the equipment, *and* the clinical practice (data based on individual
34 patient characteristics, imaging area, scan length, differences in the use and effect of the automatic
35 exposure control and other dose saving systems etc.). Simple geometrical phantoms, such as
36 polymethyl methacrylate (PMMA) plates can however be used to verify doses under various
37 conditions. They should be an integral part of the acceptability and quality control tests by the
38 medical physicist / medical physics expert. Also, anthropomorphic phantoms can be used to predict
39 or explain low or high patient dose settings. Phantoms can therefore provide complementary
40 information to patient dose surveys and valuable inputs for optimisation studies.
41

42 Particular consideration is needed in the grouping of patients for paediatric DRLs because the size
43 of children, and hence the dose levels, significantly varies not only by age but also at a given age.
44 Adults usually vary in size by a factor of 4 (40 – 160 kg bodyweight), whereas paediatric patients
45 vary in size from premature babies (e.g., 300-400 g) to obese adolescents (> 80 kg body weight)
46 representing a factor of more than 200. Classification of DRLs should also take into account the
47 steep growth pattern of a baby: within the first six months of life a baby's body weight doubles and
48 during the first year its weight trebles.
49

1 More radiation is needed for bigger patients to obtain the same image quality compared to smaller
2 patients. Due to the large variation of patient size (e.g. patient trunk thickness or effective diameter)
3 at a given age, the *weight* or *size* (e.g. girth or patient diameter) is generally a more relevant
4 parameter for patient grouping for DRLs in body examinations (see e.g. Järvinen et al., 2015,
5 Watson and Coakley, 2010). Patient weight is recommended because it is currently more easily
6 available than the size parameters. Accordingly, patients' weights should be used, at least for
7 prospective collection of data, for all body examinations. If age has been used for previous DRLs
8 and the aim is to make comparisons and trend analysis, it could continue be used as an additional
9 parameter (in association with weight or size) during the transition phase to weight groupings. The
10 recommended grouping parameters might not be valid for some examinations where little
11 experience on DRLs exist, e.g. for IR, IC and dental procedures.

12
13 Except for the first two years of life, the size of a patient's head does not show the same high
14 variation as that of a patient's trunk; therefore, age should be used as a grouping parameter for all
15 head examinations (see Section 7.3).

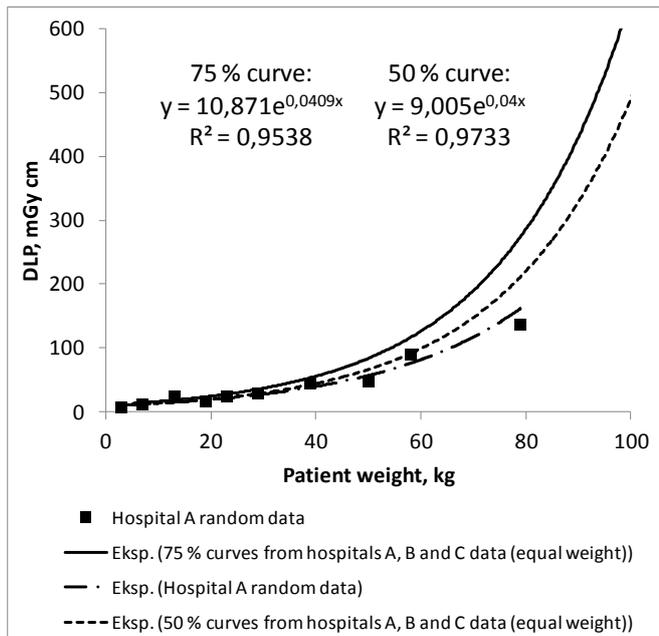
16
17 Some X-ray systems can now acquire data on the X-ray attenuation of the patient. This data would
18 be a more valuable patient dose metric than patient trunk thickness or effective diameter. Digital
19 imaging and communication in medicine (DICOM) working groups are proposing to incorporate
20 the 'patient equivalent thickness', as obtained from pre-exposure or exposure, into the extended
21 radiation dose structured report (RDSR) of the patient (IEC 2007; 2010). Once the "patient
22 equivalent thickness" becomes generally available in dose management systems, it could also be
23 used as a grouping parameter for NDRLs.

24
25 The groupings for *DRLs* (*weight, size or age*) should be defined unambiguously using intervals; e.g.
26 weight intervals < 5 kg, 5 - <15 kg, etc. The number of groups should be restricted because of the
27 practical difficulty in collecting a sufficient number of patient dose data in each group (both for
28 setting of the DRLs and for the use of the DRLs).

29
30 To overcome the problem caused by the need for several patient groups and the general paucity of
31 patient dose data in paediatric imaging, instead of using discrete patient groups, the dosimetric
32 quantity can be presented as a function of the parameter used for patient grouping, i.e. to define a
33 *DRL-curve*; an example is shown in Fig. 7.1. For the comparison of local patient dose data with the
34 DRL-curve, the user can obtain data e.g. for ten consecutive patients, regardless of their
35 age/size/weight, and insert these data points in the graph with the DRL-curve. If the majority of the
36 points are below the curve, or if a similar curve fitted to the points (provided these cover a sufficient
37 range of the patient grouping parameters) runs mostly below the DRL-curve, then the DRL has not
38 been exceeded, and vice versa. For comparison of the DRL curve with the DRLs given for discrete
39 patient groups, average data from the DRL curve can be derived for each discrete weight or size
40 group (interval).

41
42 The DRL-curve approach can be applied when the data from the patient dose surveys indicates a
43 clear relationship between the dosimetric quantity and the patient grouping parameter. For
44 appropriate comparison of local patient doses with the DRL-curve, data points should cover the
45 range of parameter values as completely as possible. The DRL-curve method provides an easy and
46 comprehensive visual indication of the local dose level compared with the DRL in cases where no
47 other analysis is possible due to the scarceness of data. It is recognised that this comparison might
48 not give an assurance with the same confidence as would be possible if the sample of patients had
49 been much higher.

50



1
2
3 Fig. 7.1. An example of DRL-curves for DLP in chest CT.
4 The DLP values relate to the 32 cm diameter CT dosimetry phantom.
5 The lowest dotted curve shows an example of using the DRL curve.
6 (Järvinen et al. 2015)

7
8 Instead of using patient size or age groups with defined intervals (e.g. 1-2 y, 2-5 y,...), another
9 approach is to specify certain standard sizes (patient widths, with a correlation to age) and to define
10 a method to convert the dosimetric parameter for a patient of any width to that for the closest
11 standard patient width (Hart et al., 2000). The conversion factor can be based on the average change
12 of absorption as a function of width for different patient widths compared to the standard patient
13 width. While this method is more exact for grouping data, the conversion might not be appropriate
14 for each patient if additional conversions from age to width are required, and it may be difficult to
15 obtain sufficient patient dose data for each standard size.

16 17 7.2 Recommended DRL quantities

18 7.2.1 Radiography and fluoroscopy

19 Air kerma-area product (P_{KA}) is the recommended primary DRL quantity for radiography and
20 fluoroscopy. It is commonly available in radiography and fluoroscopy equipment of the present
21 technology and takes into account the full radiation exposure of the patient. This quantity can be
22 easily recorded in daily practice and there are possibilities for automatic recording and comparison
23 with the DRLs (See section 8.4).

24
25 For radiography, entrance-surface air kerma ($K_{a,e}$) is recommended as an additional DRL quantity.
26 The $K_{a,e}$ provides added value for the follow up of patient dose, and enables comparisons and trend
27 analysis with earlier DRLs because the majority of the present DRLs have been given in terms of
28 $K_{a,e}$.

29
30 For fluoroscopy, air kerma at patient entrance reference point ($K_{a,r}$), fluoroscopy time and number
31 of images are recommended as useful additional DRL quantities (a multiple DRL). For example, the

1 3rd quartile or median value of the fluoroscopy time distribution for a sample of patients in standard
2 procedures can provide an indication of the achieved optimisation/ quality of the practice.

3
4 The P_{KA} is determined either by built-in or removable P_{KA} meters, or by computational systems in
5 x-ray units that calculate the P_{KA} value from the imaging parameters. The $K_{a,r}$ is determined by
6 computational systems in x-ray units and is indicated at the equipment console. In all cases, it is
7 important to ensure accurate values of the dosimetric quantity by regular calibration, or checks, that
8 are typically performed by the medical physicist during the acceptance and quality control tests. In
9 particular, such checks should be made prior to comparison with NDRLs and also prior to
10 submission as part of a national dose collection. The dose values shown at the display unit and in
11 the DICOM header should be verified for all beam qualities used in clinical practice (IAEA, 2007;
12 2013).

13
14 The $K_{a,e}$ can be calculated by dividing the P_{KA} by the entrance surface area measured at the patient
15 skin (delineated by the light beam), and multiplying by the appropriate backscatter factor (IAEA,
16 2006; 2013). When the P_{KA} is not available, $K_{a,e}$ can be calculated from the measured beam output
17 (air kerma/current time product; mGy/mAs) and the associated backscatter factor, or from the
18 detailed acquisition parameter by using indirect calculation (IAEA, 2015).

19 20 **7.2.2 Computed tomography**

21 *7.2.2.1 Present recommendations*

22
23 Both volume computed tomography dose index ($CTDI_{vol}$) and dose length product (DLP) are
24 recommended quantities for setting DRLs. The former is relevant for the patient dose burden per
25 slice while the latter is relevant for the patient dose burden for the complete CT procedure. Both
26 quantities together enable analysis of the scan length e.g. for studying the reasons for exceeding a
27 DRL. In modern CT scanners, both $CTDI_{vol}$ and DLP are available from the console and can also be
28 automatically retrieved from the radiation dose structured reports for automatic dose management
29 (see Section 8.4). Besides $CTDI_{vol}$, a Size-Specific Dose Estimate (SSDE; see Section 7.2.2.2),
30 when available, can be used as a DRL metric for body CT examinations.

31
32 An important consideration for the determination of $CTDI_{vol}$ and DLP, as well as for the setting of
33 DRLs in terms of these quantities, is the calibration of the CT console readings. The calibration uses
34 standard cylindrical CT phantoms, with either 16 cm or 32 cm diameters (“head” and “body”
35 phantoms; IEC, 2002, IAEA, 2013). In some scanners the calibration phantom size used is different
36 in paediatric body CT protocols. In recording and reporting patient dose values, it is therefore
37 essential to state the phantom size (diameter either 16 or 32 cm) used in the calibration of the
38 console value. Consequently, the $CTDI_{vol}$ and DLP values should also always be specified together
39 with the size of the calibration phantom. It is recommended that $CTDI_{vol}$ and DLP are determined
40 for a 32 cm phantom for all paediatric body CT examinations (chest, abdomen, trunk and spine) and
41 for a 16 cm phantom for paediatric head CT examinations.

42
43 It is important to ensure that correct $CTDI_{vol}$ and DLP values are obtained from CT consoles by
44 regular re-calibration, or check of the calibration, using the above standard CT phantoms (IAEA,
45 2006; 2013). This test is included in the acceptance and quality control tests performed by the
46 medical physicist, and in particular, should be made prior to comparison with NDRLs and also prior
47 to submission as part of national dose collection. It is recommended that verification of the dose
48 displays is performed for all parameters with possible influences from: large and small phantom,
49 tube voltage, collimation, bowtie filter and tube current modulation activated.

1 7.2.2.2 *Future developments: SSDE*

2
3 The data from a number of investigators have shown that for the same CT technique factors, the
4 average absorbed dose is higher for smaller patients (ICRU, 2013). A Size-Specific Dose Estimate
5 (SSDE) is a quantity recently introduced by the AAPM (AAPM, 2011; 2014) and the ICRU (ICRU,
6 2013) aimed at taking into consideration the size of the patient so that the dose metrics would better
7 correspond to the actual dose to the patient.
8

9 The SSDE can be calculated from $CTDI_{vol}$ by using published conversion factors as a function of
10 effective diameter (d_{eff}) or water-equivalent patient diameter (d_w). The latter quantity is more
11 appropriate for CT images of the chest region where an appreciable amount of internal air is
12 contained within the body dimensions. The calculation is straightforward when the tube current
13 modulation (TCM) is not utilized and when the patient diameter is relatively uniform over the scan
14 length. However, TCM is being widely applied in clinical practice and therefore, tube current and
15 hence the absorbed dose in the patient can vary appreciably along the z axis of the patient. The
16 exact calculation of the SSDE would then require the use of CT-image-by-image data instead of
17 using the above “global” correction factors (ICRU, 2013). In practice, such calculation requires
18 automated software which is not available in the current stage of technology.
19

20 Due to its closer relationship to the actual patient dose for varying sizes of paediatric patients,
21 SSDE is, in principle, a more suitable parameter than $CTDI_{vol}$ as a DRL quantity. However, when
22 the global conversion factor is used for its calculation from $CTDI_{vol}$, it has the same weakness as
23 $CTDI_{vol}$. For the same water-equivalent diameter, there will be variation from patient to patient due
24 to the TCM operation and varying anatomies of the patients. Furthermore, SSDE is not yet in such
25 general use as $CTDI_{vol}$, and its value cannot be used to calculate DLP which remains another
26 important DRL quantity. When the scanner technology develops to provide automatic calculation of
27 the more advanced SSDE, it will be a valuable addition to overall dose management.
28

29 **7.2.3 Interventional radiology**

30 7.2.3.1 *Present recommendations*

31
32 Air kerma-area product (P_{KA}) is the recommended primary DRL quantity for IR procedures. Air
33 kerma at patient entrance reference point ($K_{a,r}$), fluoroscopy time and number of images are
34 recommended as useful secondary DRL quantities (a multiple DRL) (Stecker et al. 2009). All these
35 quantities are usually available in IR x-ray equipment of the present technology. They can be easily
36 recorded in daily practice and there are possibilities for automatic recording and comparison with
37 the DRLs (See section 8.4).
38

39 For the determination of the DRL quantities and the requirements of calibration, see Section 7.2.1.
40

41 7.2.3.2 *Future developments*

42
43 For cardiac interventional procedures, a practical alternative, P_{KA} normalized to body weight
44 (P_{KA}/BW) has been proposed as a DRL quantity (Onnasch et al., 2007; Chida et al. 2010; see Annex
45 G). This was based on the observation that P_{KA}/BW remains reasonably constant making it
46 unnecessary to specify any patient grouping. Another new parameter has also been proposed:
47 product of fluoroscopy time and weight (Chida et al., 2010). These parameters can become useful
48 options in the future if more experience is gained about their general applicability.
49

1 **7.3 Recommended patient grouping**

2 For all body examinations, and for DRLs based on prospective patient dose surveys, weight should
3 be used as the parameter for patient grouping in accordance with the general recommendations in
4 Section 7.1. The recommended weight groups (intervals) are shown in Table 7.1. For head
5 examinations, age is recommended as the grouping parameter. The recommended age groups
6 (intervals) are shown in Table 7.1. When the DRL-curve approach is adopted as described above,
7 patient (trunk) thickness can also be used as the grouping parameter for radiography (Kiljunen et
8 al., 2007).

9
10 The recommended first weight group (< 5 kg) applies to newborn babies but does not apply to those
11 in incubators. The optimisation of the dose for babies in incubators is important but it might not be
12 appropriate to establish DRLs for these very specific and varying cases, where, e.g., different types
13 of incubators affect dose differently.

14
15 The basic definition of the DRLs refers to “standard-sized patients” (Section 4). It is important,
16 therefore, to realize that very obese or severely underweight patients should be excluded from the
17 sample of patients used in patient dose surveys to establish DRLs, or to compare the local median
18 patient dose value with the LDRLs or NDRLs. The effect of including very obese or severely
19 underweight patients can be significant in very small samples and becomes less important or
20 insignificant in very large samples. Published tables of weight-for-age charts (Centers for Disease,
21 2015) can be used to judge the acceptability of the weight of a patient of a given age for inclusion in
22 the survey, e.g. by excluding patients below the 5th percentile and above 95th percentile of weight;
23 see also Table 7.2.

24
25 Because most of the current NDRLs have been given in terms of patient age, it is acknowledged
26 that age will still be used in a transition period until data from the recommended weight based
27 patient dose surveys become available. In the transition period, age can be used as an additional
28 parameter for patient grouping and for the purpose of comparison of proposed new, weight-based
29 DRLs with earlier values (trend analysis).

30
31 There is a rough correlation between the average weight and age groups, as can be deduced from
32 the published weight-for-age charts (Centers for Disease, 2015). Using the 25th to 75th percentiles of
33 weight, i.e. by excluding the relatively low or high weights for a given age, an approximate
34 equivalence shown in Table 7.2 can be obtained. There are also some published studies on
35 empirical equivalencies (AAPM, 2011; Seidenbusch and Schneider, 2008).

36
37 The weights to age range equivalence shown in Table 7.2 should only be used as a rough
38 approximation when comparing the weight-based DRLs with previous age-based DRLs. It should
39 also be noted that several differing sets of age groups have been used for the NDRLs (or
40 equivalent); the most common grouping found is approximated in the last column of Table 7.2.
41 When calculating the EDRLs (Section 10), the age groupings in the last two columns of Table 7.2
42 have been used to roughly derive the EDRLs based on weight.

43
44 Every effort should be taken to group patients according to the above recommendations. However,
45 less groupings can be considered if it can be justified nationally by clear reasoning, e.g., if the range
46 of patient weights for a given examination in a country is narrower than those described in Table
47 7.1.

48

1 Table 7.1. Recommended grouping of patients for paediatric DRLs

2

Recommended weight groups (intervals) for <i>body</i> examinations	Recommended age groups (intervals) for <i>head</i> examinations
< 5 kg	0 - < 3 months
5 - < 15 kg	3 months - < 1 y
15 - < 30 kg	1 - < 6 y
30 - < 50 kg	≥ 6 y
50 - < 80 kg	

3

4

5 Table 7.2. Approximate equivalence of weight and age groups for the purpose of comparing weight-

6 based DRLs with age-based DRLs.

7

Description	Weight group	Age group based on weight-for-age charts	Most common age groups used for the NDRLs (or equivalent)
Neonate	< 5 kg	< 1 m	0 y
Infant, toddler and early childhood	5 - < 15 kg	1 m - < 4 y	1 y
Middle childhood	15 - < 30 kg	4 - < 10 y	5 y
Early adolescence	30 - < 50 kg	10 - < 14 y	10 y
Late adolescence	50 - < 80 kg	14 - < 18 y	15 y

8

9

10

1 **8. Practical methods to establish paediatric DRLs**

2 **8.1 General**

3 DRLs should be established primarily for paediatric examinations that significantly contribute to the
4 collective effective dose of the paediatric patient population (as discussed and introduced in Section
5 6). This can include both the most common examinations and less common high dose examinations.

6
7 DRLs should be based on appropriate patient dose surveys. These surveys should have sufficient
8 coverage of all institutions for which the DRLs are intended (i.e., the geographical area concerned),
9 whenever possible. In particular, DRLs should be based on national patient dose surveys with a
10 representative sample of all radiological institutions in the country when available. DRLs based on
11 very limited surveys or on measurements only in phantoms, as well as DRLs adopted from
12 international recommendations or from other countries, should only be used as preliminary values
13 until data from the relevant national patient dose surveys are available.

14
15 Patient dose data can be collected manually or by making use of automatic data recording and
16 collection systems (see Section 8.4). Due to the generally large amount of data needed and the large
17 amount of potential errors when these data are to be collected during routine practice, automatic
18 data collection is recommended wherever possible. However, a manual approach is needed until
19 automatic systems become generally available, validated for accuracy of collected data and are
20 sufficiently harmonised.

21
22 There is a need to update the DRLs at regular intervals, based on new patient dose surveys. National
23 DRLs should be reviewed and updated at a minimum frequency (maximum interval) of 5 years.
24 Once automatic dose management systems become more generally available, the frequency could
25 be 3 years or even lower. Local DRLs should be reviewed and updated at least every 3 years and
26 when there are changes of the equipment or practices which have a potential impact on patient dose
27 levels.

28 29 **8.2 Patient dose surveys**

30 To carry out patient dose surveys, the following parameters should be carefully determined:

- 31 • procedures for which DRLs are needed
- 32 • dose and other quantities (DRL quantities)
- 33 • patient grouping (according to weight, age, body size)
- 34 • technical equipment parameters
- 35 • number and distribution of X-ray departments participating in the survey
- 36 • percentile point for the DRL selection

37 38 **8.2.1 DRL quantities and patient grouping**

39 Patient dose data should be collected consistently with the DRL quantities and patient grouping
40 (discrete groups or continuous DRL curve) recommended for DRLs in Section 7.

41 42 **8.2.2 Technical equipment parameters**

43 Besides the actual patient dose data according to the recommended patient grouping, there are other
44 data (Table 8.1) which are useful for the evaluation and decision making when DRLs are to be
45 established.

46

1 Table 8.1. Supplementary data to support the patient dose surveys for establishing DRLs.
2

Radiography	Fluoroscopy	CT	IR
Equipment data: manufacturer and type	Equipment data: manufacturer and type	Equipment data: manufacturer and type	Equipment data: manufacturer and type
Detector system (screen/film, including speed class (S/F); computed radiography, including phosphor used (CR); digital radiography; type of detector (DR)	Type of detector (DR)	Detector configuration (number of detector rows)	Type of detector (DR)
Source detector distance (SDD)	Source detector distance (SDD)		Source detector distance (SDD)
Added filtration	Added filtration		Added filtration
Grid (used/not used/not removable)	Grid (used/not used/not removable)		Grid (used/not used/not removable)
Exposure parameters: kV, mA, mAs	Exposure parameters: kV, mA, mAs	Exposure parameters: kV, mA, mAs	Exposure parameters: kV, mA, mAs
		Automatic tube voltage selection tool used/ not used	
		Rotation time, mode (sequential/helical), pitch (helical) or table increment (sequential), Field of View (FOV), collimation thickness, beam shaping filters, scanning length	Field of View (FOV)
Automatic exposure control (AEC) (activated/ deactivated)	AEC mode	Tube-current modulation	AEC mode
		Image quality level: Quality Reference mAs/noise index/reference image	
		Standard deviation of CT numbers or equivalent	
		Image handling: reconstruction slice thickness, iterative reconstruction	
		Number of phases and scan sequences	
		Size of the calibration phantom	

1 **8.2.3 Recommended sample size and composition**

2 Patient dose data should be collected from a representative sample of various types of equipment
3 and practices in the geographical area concerned. For LDRLs, data should be collected from all
4 rooms and all types of x-ray equipment used. For NDRLs, the institutions providing patient dose
5 data should include dedicated paediatric healthcare facilities and departments (i.e. children
6 hospitals or departments/units specialising in paediatric imaging), and general healthcare facilities
7 and departments where paediatric practices are part of the overall radiology services. Among the
8 healthcare facilities and departments, big, medium size and small units as well as private and
9 public units should be selected.

10
11 Statistically relevant numbers of patient dose data should be collected. In general, the number of
12 subjects used to estimate DRLs, the confidence level, the confidence interval and the variability
13 observed in patient doses for the same type of x-ray examination are interrelated variables.
14 Confidence intervals from small sample sizes may produce unacceptably imprecise results. It is
15 common practice to consider a 95% level of confidence. For a given confidence level, the larger
16 the sample size the smaller the confidence interval. To obtain a 10% confidence interval at a 95%
17 level of confidence requires a sample size of about 100 patients and a 20% confidence interval
18 requires a sample size of about 25 patients. Therefore, for a given confidence level, the larger the
19 variability in patient doses for the same type of examination the larger the sample size needed to
20 obtain a given confidence interval.

21
22 In IR procedures, a very wide distribution of doses for the same type of procedures has been
23 observed. This variability may be attributed to many factors including technique variations
24 between interventionalists and complications arising during the interventional procedure.
25 Investigators should balance the benefits of increased sample size and increased precision against
26 the cost of increased time of data collection.

27
28 It is recommended that from each institution a representative sample of at least 10 patients per
29 procedure type and per patient group is needed for non-complex examinations such as radiography
30 and CT and at least 20 patients per procedure type and per patient group for complex procedures
31 such as fluoroscopy and fluoroscopically guided procedures. If the DRL- curve approach can be
32 used, a total of 10 (non-complex examinations) and 20 (complex procedures) patients per DRL
33 curve are required and consequently, much less patients are needed per procedure type. For cardiac
34 catheterization and interventional cardiology in paediatric patients, even more patients may be
35 needed because of large differences in complexity and duration of the procedures; however, to
36 recommend the minimum number for these procedures, further studies are needed.

37 38 **8.2.4 Percentile point for DRL**

39 For setting the values of NDRLs and LDRLs, according to the definition, the 3rd quartile (the
40 75th percentile) should be used. This will ensure effective recognition of the “outliers”, i.e., the
41 institutions and practices which have unusually high patient dose levels compared with most of the
42 other institutions, possibly because of old x-ray units or the lack of adequate optimisation.
43 However, the full dose distribution should be exploited for optimisation in addition to DRLs: the
44 median (2nd quartile (the 50th percentile)) value should also be determined and retained for the
45 purpose of follow up of optimisation, trend analysis and comparisons in the future updates of the
46 DRLs. The comparison of the relative changes in the 75% and 50% levels can provide useful
47 information on the development of the optimisation.

48

1 When the DRLs are being updated, in particular if the dose distribution is less peaked and the
2 variation between the median values collected from institutions is less prominent than during the
3 first introduction of the DRLs, the 50th percentile of the dose distribution could be used as a
4 supplementary metric to the DRL (the 75th percentile). This provides a better goal for optimisation
5 in those institutions with advanced level of technology and optimisation of practices.
6

7 In consideration of the patient dose needed, the overriding criterion is an acceptable image quality:
8 the image quality should be adequate for the diagnosis according to the indication of the
9 examination. In the patient dose surveys for setting DRLs, likewise in daily imaging practices, there
10 should always be a system in place to judge whether the image quality is adequate. Patient doses
11 associated with rejected images should not be included in the sample for setting DRLs. The image
12 quality requirement should be based on clinical grounds only. Therefore no limit or warning level
13 for low image quality based solely on the dose level is recommended. If specific actions are taken to
14 reduce a LDRL, it is advisable to establish a dose management team, consisting of a radiologist,
15 radiographer and a medical physicist.
16

17 **8.3 Setting of DRLs**

18 **8.3.1 Organisations to set the DRLs**

19 The organisation which should set the DRLs depends on whether the DRL is local, national, or
20 European (see the definitions in Section 4).
21

22 *LDRLs* are set by a given hospital or group of hospitals within a defined district for their own use,
23 as an aid to improve optimisation of imaging practices in all rooms and with all radiology
24 equipment used in the radiology departments of the hospital or group of hospitals. These can be set
25 to correspond to the level of technology and local achievements of optimisation, to ensure
26 continuous vigilance on the optimum procedures and to provide an alert when any unjustified
27 changes in the local patient dose levels occur.
28

29 *NDRLs* are set by an authoritative body, i.e. competent national authorities such as national
30 radiation protection or health authorities (e.g. ministry of health; e.g., in AT, FI, DE), or specific
31 institutions established and authorized by competent national authorities (e.g. in FR) (see Tables
32 C.2 and C.4 in Annex C). The purpose of the NDRLs is to provide a tool for each hospital or
33 radiology department in the country to check their local median patient dose levels or LDRLs
34 against the national 75th percentile levels for standard radiological practices and to undertake
35 appropriate actions when the NDRLs are exceeded (see also section 9.1.2).
36

37 The organisation conducting the patient dose surveys, for the basis of setting the NDRLs, can be
38 either the same authoritative body, which sets the NDRLs, or another institution capable of
39 coordinating such an effort. Good practice is to undertake these surveys and to analyse the results
40 with the collaboration of national professional/scientific societies or at least having recognized
41 clinical experts as consultants in the process.
42

43 *EDRLs* are given by European Commission (this publication). EDRLs are recommendations, and
44 can be adopted by the countries as NDRLs only as long as NDRLs based on national patient dose
45 surveys are not available (see Section 10.3).
46

1 **8.3.2 Role of authorities and professional societies**

2 The competent national authorities should be responsible for guaranteeing the establishment,
3 implementation and use of DRLs. The authorities should take the lead in bringing together the
4 professional societies representing medical doctors, radiographers and medical physicists to
5 implement patient dose surveys and to establish NDRLs according to the methodology defined in
6 these guidelines. The strong involvement of all professional societies in the establishment of
7 NDRLs is the best vehicle to promote the effective use of the DRL concept.
8

9 In practice, the professional societies and their clinical experts should advise on the examinations
10 and procedures where DRLs should be set, advise on organising or coordinate the patient dose
11 surveys (institutions included, practical methods), and advise on the analysis and conclusions on the
12 results to establish the NDRLs.
13

14 **8.4 Automatic dose management**

15 **8.4.1 General review**

16 Dose management solutions can play an important role in the establishment and use of NDRLs or
17 LDRLs. These systems facilitate data collection for patient dose surveys, enable the comparison of
18 patient dose data with DRLs and harvest electronic dose data.
19

20 The general development for automatic dose management systems is reviewed in Annex E. A list of
21 currently available dose management systems is also presented in Annex E. Besides the commercial
22 systems shown in Annex E, the dose management system with the largest CT database in the world
23 is the ACR Dose Index Registry (Bhargavan-Chatfield and Morin, 2013). Currently it has captured
24 data from over 800 facilities and 16 million examinations and is available to facilities both within
25 the US and outside of the US.
26

27 Most products on the market already support the control and review of paediatric DRLs. The most
28 important parameters are collected and export functions exist in most products, so the systems are
29 becoming very useful tools to establish LDRLs and NDRLs and to make comparisons of local
30 patient dose data with these DRLs. Specific paediatric models currently in development will further
31 facilitate these tasks.
32

33 It is important that the desired features (Section 8.4.2) and the local needs should be considered
34 from the beginning and discussed in collaboration with the chosen system manufacturer. For
35 example, in CT imaging, the most critical point in the systems currently is the availability of
36 weight, effective diameter and/or SSDE values. The efficient implementation and use of the
37 systems in daily practice should be ensured by appropriate personnel resources, including training
38 on their use and how to interpret the results and when to undertake further investigations and
39 remedial actions.
40

41 **8.4.2 Recommendations for the dose management systems to support paediatric DRLs**

42 To establish and use paediatric DRLs for the different imaging modalities, the dose management
43 system should be able to provide the following features:
44
45

- 1 General features:
- 2 • Access patient age
 - 3 • Access patient weight
 - 4 • Access to required patient dose quantities (see below)
 - 5 • Access to technical equipment parameters (exposure parameters, image handling
 - 6 algorithms etc.; see the list in Section 8.2.2)
 - 7 • Export of a filtered set of data for further analysis e.g. examination type, patient grouping
 - 8 with age or weight, etc.)

9

10 Radiography

- 11 • P_{KA}
- 12 • $K_{a,e}$

13

14 CT

- 15 • CTDIvol (calibration phantom size indicated)
- 16 • DLP
- 17 • Patient width or water equivalent diameter
- 18 • SSDE (AAPM, 2011)

19

20 Interventional procedures

- 21 • P_{KA}
- 22 • $K_{a,r}$
- 23 • Fluoroscopy time
- 24 • Number of cine, digital, and frontal versus lateral images

25

26 It is desirable that these features are easily accessible in any selected product. To allow non-

27 standard evaluations of the collected data, a flexible export feature should be available to export a

28 selected dataset for further analysis.

29

1 **9. Methods of using DRLs**

2 **9.1 Use of different types of DRLs**

3 The use of different DRLs should be in accordance with their definitions (Section 4) and therefore,
4 three different levels are distinguished in the following:

- 5
- 6 (1) DRLs available at the level of the healthcare facility or group of healthcare facilities
7 (LDRL)
- 8 (2) DRLs available at national level (NDRL)
- 9 (3) DRLs available at European level (EDRL)

10

11 The comparison of patient doses with DRLs should always be based on data from a sample of
12 patients, as described below, and should not be used on an individual patient basis.

13

14 **9.1.1 LDRLs – for optimisation within a healthcare facility or group of healthcare facilities**

15 The median (the 50th percentile) values of patient dose distributions from a wide representative
16 sample of examinations, obtained from within the healthcare facility or group of healthcare
17 facilities, should regularly be compared with any existing LDRLs. The objectives of these
18 comparisons is to identify and improve shortcomings in the optimisation of the patient doses within
19 the healthcare facility or group of healthcare facilities, to follow up the patient dose levels and to
20 find out if there are any unexpected changes in the levels, e.g. due to equipment malfunction,
21 unauthorized change of the imaging practice or lack of sufficient training of new users. The LDRLs
22 will enable more systematic studies of patient dose levels and the achievement of optimisation
23 within the healthcare facility or group of healthcare facilities, e.g., comparisons between radiology
24 departments, effect of selected local parameters such as week-end versus working days, day time
25 versus night shift, dedicated paediatric versus general radiology staff, or performance of selected
26 teams of radiographers.

27

28 **9.1.2 NDRLs – for both local and nationwide optimisation**

29 NDRLs should be set by an authoritative body, based on national patient dose surveys and
30 according to the other principles laid down in Section 8. The NDRLs, when not adopted from the
31 EDRLs, should be compared with the EDRLs (see Section 10.3).

32

33 Institutions that have their own LDRLs must carry out regular comparison of the LDRLs with
34 NDRLs to ensure they are not higher. Where it is found that an LDRL is higher than a newer
35 reported NDRL, increased attention must be paid to optimisation and new patient dose surveys
36 should be conducted to check whether updating the LDRL is needed. If the LDRL or its update
37 remains higher than the relevant NDRL, it should be replaced by the NDRL.

38

39 Where no LDRLs have been set, the median (the 50th percentile) values of patient dose distributions
40 from representative samples of examinations, obtained from the healthcare facility or group of
41 healthcare facilities, should regularly be compared with the NDRLs for all types of examinations
42 where NDRLs have been set. The objectives of these comparisons are to identify and improve
43 shortcomings of local practices in the optimisation of the patient doses, to follow up the patient dose
44 levels in various hospitals and to find out if there have been any changes in the levels, e.g. due to
45 change of imaging technology or imaging practices, or lack of sufficient training of users. Cases
46 should be investigated where the median values of the local patient dose distributions are above the
47 NDRLs and reduced through appropriate changes in practice in order to improve patient protection.

1
2 The authoritative body issuing the NDRLs should complement them with detailed guidance on how
3 to compare the values with local patient dose levels. The implementation of such comparisons
4 should be a component in the regulatory inspection program and it is highly recommended that the
5 correct implementation and the results of comparisons are among the key topics of regular clinical
6 auditing (EC, 2009). Results of the comparisons should also be collected and summarized from time
7 to time, to enable trend analysis and to check the need for updating the NDRLs, and to focus
8 training efforts on practices and areas where the need is most evident.
9

10 **9.1.3 EDRL – for support of national efforts**

11 How individual countries can use EDRLs is discussed in Section 10.3.

12
13 The use of EDRLs provides an interim solution for countries with no national patient dose surveys,
14 until such surveys are made. The established EDRLs, together with the recommendations of Section
15 6, will indicate the examinations where the establishment of NDRLs is feasible and recommended.
16 The analysis and development of EDRLs also indicates the examinations where harmonisation of
17 DRLs could be achievable, as well as the types of examinations where DRLs would be needed but
18 are not currently available, and consequently, where patient dose surveys and research on DRLs
19 should be directed.
20

21 Regular updates of EDRLs will provide data for trend analysis and development of the optimisation
22 of paediatric patient doses in Europe. The patient dose surveys used for the basis of paediatric
23 DRLs can also be exploited in studies on the collective doses to the paediatric population from
24 medical imaging.
25

26 **9.2 Methods of comparison**

27 When comparing the local patient dose data with DRLs, it is clear that the same quantities and
28 patient groupings have to be applied as those used for the DRLs. In the cases where the same
29 patient groupings are not available, conversions (e.g. from age to weight) can be applied but this
30 will add uncertainty to the comparison.
31

32 The median value of a patient dose distribution, for a minimum of 10 patients for each patient group
33 (weight, age), should be calculated and compared with the DRL. If the DRL curve method is used, a
34 minimum of 10 (non-complex examinations) or 20 (complex procedures) patients is sufficient for
35 the whole comparison provided these cover reasonably well the whole range of patient weight or
36 size parameter.
37

38 As the main purpose of using DRLs is to find where patient doses are significantly higher than
39 those generally achievable, a simple observation that the local median dose level exceeds the DRL,
40 or a visual observation that the local dose data points or the curve fitted through them exceeds the
41 DRL-curve generally suffice. However, the significance of the difference can be more exactly
42 studied and confirmed by statistical means e.g. the Student's t-test can be applied.
43

44 The development of automatic dose management systems with integrated dose monitoring
45 programs will enable frequent or even on-line comparisons of the median (the 50th percentile)
46 values of patient dose distributions with the DRL (LDRL or NDRL), and can include an automatic
47 indication when the DRL is exceeded. Such automatic systems can provide continuous follow-up of
48 patient dose levels and ensure a rapid communication between the radiographers (operators) and the
49 medical physicist / medical physics expert to identify the reasons for the unusual dose levels.
50

1 **9.3 Comparison frequency**

2 The local patient dose levels should be compared with LDRLs or NDRLs at least once per year.
3 LDRLs should be compared with NDRLs and NDRLs with EDRLs whenever any DRLs have been
4 established or updated.
5

6 **9.4 Local reviews and actions when DRLs are exceeded**

7 All radiological departments should apply the available NDRLs, unless lower (more strict) LDRLs
8 have been defined. Whenever the DRLs applied are consistently exceeded, appropriate
9 investigations to identify the reasons, and corrective actions to improve the clinical practice, if
10 necessary and feasible, should be undertaken without undue delay (EC, 2014). The investigation
11 should include review of equipment performance, the settings used, and the examination protocols
12 (Martin, 2011). The factors most likely to be involved are dose survey methodology, equipment
13 performance, procedure protocol and operator skill. A typical reason maybe related to a failure to
14 adapt the imaging protocol to account for paediatric diseases and paediatric patient sizes.
15

16 Findings of deficiencies in equipment performance might require a critical review of QA and
17 maintenance programmes or initiate the replacement of equipment, Other corrective actions may
18 include for example adjustment of the AEC, review and adjustment of standard operating
19 procedures and protocols, and setting of equipment controls,
20

21 The responsibility for investigations and corrective actions must be given to appropriate staff who
22 have the necessary expertise. The groups of staff involved will depend on arrangements in each
23 country or region, and may be medical physicists, radiographers, medical physics technologists, or
24 paediatric radiologists, who may be employed by the healthcare provider or under contract to the
25 provider (Martin et al., 2013).
26

27 The use of the DRLs, including all findings and subsequent corrective actions should be
28 documented and made available for clinical audits (internal or external audits) and for regulatory
29 inspections by competent authorities. Several international recommendations (EC, 2009; ICRP,
30 2007; IAEA, 1996) point out that the patient dose should be addressed in clinical audits in
31 comparison with the given DRLs. As a minimum, assessing the local practice of comparisons of
32 patient doses with the DRLs should be part of the clinical audit procedure.
33

34 As highlighted in the introduction (Section 2), optimization of paediatric x-ray examinations and
35 procedures is of particular importance due to the children's higher radiation risk. The application of
36 DRLs is an important part of this but not sufficient, by itself, for optimisation of protection.
37 Optimisation is generally concerned with maintaining the quality of the diagnostic information
38 commensurate with the medical purpose while, at the same time, seeking to reduce patient
39 exposures to radiation to a level as low as reasonably achievable. Methods to achieve optimisation
40 that encompass both DRLs and image quality evaluation should therefore be implemented.
41
42
43

1 **10. European DRLs (EDRLs)**

2 **10.1 Methods to establish EDRLs**

3 For these guidelines there has been no possibility to establish new large scale patient dose surveys,
4 either nationally or European wide. Therefore, the proposed European DRLs (EDRLs) had to be
5 based on national DRLs (NDRLs) existing in European countries. EDRLs have been derived as the
6 median values of the relevant NDRLs, in accordance with the definitions adopted in Section 4.
7 However, due to the scarceness of official NDRLs, i.e. NDRLs set by an authoritative body, a few
8 recent publications presenting proposed NDRLs or relevant results (the 75th percentiles) of
9 nationwide patient dose surveys, have also been taken into consideration. The DRL data (the
10 official and proposed NDRLs and the published 75th percentile values) were accepted for the
11 calculation if these met the following criteria (see also Section 5.5.3):

- 12 • Data had to be based on own national patient dose surveys i.e. no phantom or protocol
13 based evaluations, no DRLs adopted from other countries or from the out-of-date European
14 recommendations.
- 15 • Patient dose surveys had to cover a representative sample of national practices (number
16 and types of institutions).
- 17 • DRL quantities must be in accordance with the recommendations (Section 7 and Executive
18 summary).
- 19 • Patient groupings for DRLs must be adaptable to the recommended groupings (Section 7
20 and Executive summary), i.e. if different groups have been used, their equivalence with the
21 recommended groups has to be specified.
- 22 • The percentile point for the DRL selection had to be 75%.
- 23 • Patient dose surveys must not be more than 6 years older than the most recent survey for
24 the DRL quantity in question.
- 25 • DRLs from at least 3 countries must be available for the calculation.
- 26 • DRLs for CT must refer to a complete routine CT examination (one scan series).

27
28 With the above criteria, EDRLs could only be derived for a few examinations in radiography,
29 fluoroscopy and CT.

30
31 For IR, no EDRL can be proposed because neither official nor proposed NDRLs exist. As shown in
32 Section 5, for paediatric cardiac procedures, only LDRLs have been published, and for paediatric
33 non-cardiac procedures, no DRL data is available. In the context of the PiDRL project, a limited
34 number of patient dose data for both cardiac and non-cardiac procedures was collected from a few
35 paediatric centres. In Annex G, a summary of the most recent publications on patient doses and
36 LDRLs for cardiac procedures, including some notes of the limited PiDRL survey, has been
37 presented, as well as a brief summary of the PiDRL patient data collection for paediatric non-
38 cardiac procedures. The need for DRLs for paediatric IC and other IR procedures was stated in
39 Section 6.3 and is further highlighted in the summaries of Annex G. It is concluded that further
40 research and data collection from several cardiac centres has to be conducted to assess the
41 feasibility of paediatric NDRLs or EDRLs and to obtain a sufficient and reliable basis for
42 suggesting these DRLs when feasible.

43
44 The DRL data or publications used for the evaluation of the EDRLs for radiography, fluoroscopy
45 and CT are shown in Table 10.1. More details of the selection of the data are given in Annex F.

46
47

1 Table 10.1. Data on DRLs accepted for consideration of the European DRLs.

2

	Radiography	Fluoroscopy	Computed tomography	Interventional radiology
NDRLs set by an authoritative body (Annex 1)	AT- Billiger et al., 2010 BE DE DK ES- Ruiz-Cruces, 2015 FI- Kiljunen et al., 2007 FR- Roch et al., 2012 LT NL	AT DE DK ES- Ruiz-Cruces, 2015 FI NL UK- Hart et al. 2012	AT BE DE ES- Ruiz-Cruces, 2015 FI- Järvinen et al. 2014 IE- HSE Medical Exposures Radiation Unit , 2013 LT NL UK- Shrimpton et al. 2006, Shrimpton et al. 2014	No NDRLs exist
Other published/available data			PT- Santos et al. 2013 IT- Granata et. al. 2015	No acceptable data.

3

4 **10.2. EDRL values**

5 The resulting EDRLs are presented in Table 10.2 a, b. In these tables, the recommended age groups
6 for head examinations and weight groups for body examinations have been used (see Table 7.1).

7

8 In Annex F, the mean values and the interquartile values of the DRL-data used in the calculations
9 are also given. These data can give some understanding of the possible uncertainties when adopting
10 an EDRL as an NDRL (see also Section 10.3).

11

1 Table 10.2a. European DRLs for radiography and fluoroscopy

2

Radiography and fluoroscopy			
Examination	Age or weight group	EDRL	
		$K_{a,e}$, mGy	P_{KA} , mGy cm ²
Head AP/PA	3 months-<1 y		215
	1-<6 y		295
	≥6 y		350
Head LAT	3 months-<1 y		200
	1-<6 y		250
Thorax AP/PA**	<5 kg		15
	5-<15 kg	0,06	22
	15-<30 kg	0,08	50
	30-<50 kg	0,11	70
	50-<80 kg		87
Abdomen AP	<5 kg		45
	5-<15 kg		150
	15-<30 kg	0,40	250
	30-<50 kg	0,75	475
	50-<80 kg		700
Pelvis AP	15-<30 kg		180
	30-<50 kg		310
MCU	<5 kg		300
	5-<15 kg		700
	15-<30 kg		800
	30-<50 kg		750*

*Based on 4 NDRLs, range 400-2000 mGy cm²; **AP/PA: DRL applies to both AP and PA projections

3

4

5 Table 10.2b. European DRLs for computed tomography. EDRLs for head CT refer to 16 cm
6 phantom and EDRLs for thorax and abdomen for 32 cm phantom. DRLs refer to a complete routine
7 CT examination (one scan series).

8

Computed tomography			
Exam	Age or weight group	EDRL	
		CTDI _{vol} , mGy	DLP, mGy cm
Head	0-<3 months	24	300
	3 months-<1 y	28	385
	1-<6 y	40	505
	≥6 y	50	650
Thorax	<5 kg	1,4	35
	5-<15 kg	1,8	50
	15-<30 kg	2,7	70
	30-<50 kg	3,7	115
	50-<80 kg	5,4	200
Abdomen	<5 kg		45
	5-<15 kg	3,5	120
	15-<30 kg	5,4	150
	30-<50 kg	7,3	210
	50-<80 kg	13	480

9

1 **10.3 Use of the EDRLs**

2 It is strongly recommended that NDRLs, based on adequate national patient dose surveys, are
3 established in each country instead of adopting the above EDRLs. Therefore, all the EDRLs
4 presented in these Guidelines (Tables 10.2a,b) should be considered only as the preliminary choice
5 for the NDRLs until appropriate national patient dose surveys have been carried out and NDRLs
6 based on these surveys have been established by an authoritative body.

7
8 If the NDRLs exceed the EDRLs, the reasons for these differences should be considered. In
9 particular, if the NDRLs are not based on recent national patient dose surveys, the need for new
10 surveys to update the NDRLs should be considered.

11

1 **ACKNOWLEDGEMENTS**

2

Scientific Coordinator

John Damilakis, ESR

Guidelines Leader

Hannu Järvinen, STUK

Project Management

Monika Hierath, ESR

Ulrike Mayerhofer-Sebera, ESR

Project Officer

Georgi Simeonov

Contributors to the Project

Hilde Bosmans, EFOMP

John Damilakis, ESR

Hubert Ducou le Pointe, ESPR

Stephen Evans, EFOMP

Shane Foley, EFRS

Claudio Granata, ESPR

Andreas Jahnén, LIST

Hannu Järvinen, STUK

Mika Kortnesniemi, STUK

Catherine Owens, ESPR

Graciano Paulo, EFRS

Dean Pekarovic, EFRS

Raija Seuri, STUK

Erich Sorantin, ESPR

Virginia Tsapaki, EFOMP

Peter Vock, ESR

Expert Advisory Panel

*Cardiovascular and Interventional
Radiological Society of Europe (CIRSE):*

Erich Sorantin

*International Atomic Energy Agency
(IAEA):* Jenia Vassileva

*International Commission on Radiological
Protection (ICRP):* Eliseo Vano-Carruana

*National Council on Radiation Protection
and Measurements (NCRP):* James A. Brink

Public Health England (PHE): Sue Edyvean

World Health Organisation (WHO): Maria
Perez

**Feedback on the guidelines document
has been received from**

*Association for European Paediatric and
Congenital Cardiology (AEPC):* Eero
Jokinen, Ornella Milanese

*Cardiovascular and Interventional
Radiological Society of Europe (CIRSE):*
Anna-Maria Belli, Werner Jaschke

European Commission (EC): Georgi
Simeonov

*European Federation of Organisations
for Medical Physics (EFOMP):* Carmel
Caruana, Koos Geleijns, Alberto Torresin

*European Federation of Radiographer
Societies (EFRS):* Csaba Vandulek

*European Society of Paediatric
Radiology (ESPR):* ESPR board, Claudio
Granata

European Society of Radiology (ESR):
Guy Frija, Wolfram Stiller

*Heads of the European Radiological
Protection Competent Authorities
(HERCA):* Jürgen Griebel

Image Gently Alliance: Kimberly
Applegate, Priscilla Butler, Donald P.
Frush, Marta Schulman, Keith Strauss

*International Atomic Energy Agency
(IAEA):* Ahmed Meghzifene, Harry Delis

*Working Party on Medical Exposures of
the Group of Experts referred to in Art.
31 of the EURATOM Treaty:* Vasiliki
Kamenopoulou, Reinhard Loose,
Geraldine O'Reilly, Eliseo Vano-
Carruana

It is also acknowledged that constructive
feedback was received from a wide range
of stakeholders during the PiDRL
Workshop held in Lisbon, Portugal, on
October 15-17, 2015.

3

1 **REFERENCES**

2 AAPM (2011). American Association of Physicists in Medicine. Size-Specific Dose Estimates
3 (SSDE) in Paediatric and Adult Body CT Examinations, AAPM Report No. 204 (American
4 Association of Physicists in Medicine, College Park, MD).
5
6 AAPM (2014). American Association of Physicists in Medicine. Use of Water Equivalent Diameter
7 for Calculating Patient Size and Size-Specific Dose Estimates (SSDE) in CT, AAPM Report No.
8 220 (American Association of Physicists in Medicine, College Park, MD).
9
10 ACR-AAPM (2013). ACR-AAPM Practice parameter for diagnostic reference levels and
11 achievable doses in medical x-ray imaging, Revised 2013.
12 http://www.acr.org/~media/ACR/Documents/PGTS/guidelines/Reference_Levels.pdf
13
14 ACR (1998): CRCPD Publication E-04-5. Nationwide evaluation of x-ray trends (NEXT).
15 Tabulation and graphical summary of the 1998 pediatric chest survey, September 2014.
16 http://crcpd.org/Pubs/NEXT_docs/NEXT98PediatricChest.pdf
17
18 Alzen, G. and Benz-Bohm, G. Radiation Protection in Paediatric Radiology. *Dtsch Arztebl Int*
19 (2011), 108: 407-14.
20
21 Bacher, K., Bogaert, E., Lapere, R., De Wolf, D., and Thierens, H. (2005a). Patient-specific dose
22 and radiation risk estimation in paediatric cardiac catheterization. *Circulation*, 111(1), 83–9.
23 doi:10.1161/01.CIR.0000151098.52656.3A
24
25 Bacher, K., Bogaert, E., Lapere, R., De Wolf, D., and Thierens, H. (2005b). Patient-specific dose
26 and radiation risk estimation in paediatric cardiac catheterization. *Circulation*, 111(1), 83–9.
27 Retrieved from <http://www.ncbi.nlm.nih.gov/pubmed/15611374>
28
29 Barnaoui, S., Rehel, J. L., Baysson, H., Boudjemline, Y., Girodon, B., Bernier, M. O., Bonnet D.
30 and Aubert, B. (2014). Local Reference Levels and Organ Doses From Paediatric Cardiac
31 Interventional Procedures. *Paediatric Cardiology. Pediatr Cardiol.* 2014 Aug;35(6):1037-45. doi:
32 10.1007/s00246-014-0895-5. Epub 2014 Mar 21.
33
34 Bhargavan-Chatfield M. and Morin R.L. The ACR Computed Tomography Dose Index
35 Registry: The 5 Million Examination Update. *JACR* 2013;10(12):980-983.
36
37 Billiger, J., Nowotny R. and Homolka P. Diagnostic reference levels in paediatric radiology in
38 Austria. *Eur. Radiol.* (2010), 20: 1572-1579.
39
40 Born, M., Spiller, L., Bachour, H., Heydweiller, A. and Franke, I. (2013). Dose area product of
41 paediatric VCUG with regard to the strongly lowered German diagnostic reference levels. *RöFo :*
42 *Fortschritte Auf Dem Gebiete Der Röntgenstrahlen Und Der Nuklearmedizin*, 185(3), 262–7.
43 Retrieved from <http://www.ncbi.nlm.nih.gov/pubmed/23154862>
44
45 Boice, J.D. Jr. Radiation epidemiology and recent paediatric computed tomography studies. *Ann*
46 *ICRP.* 2015 Mar 24. pii: 0146645315575877. [Epub ahead of print].
47

- 1 Brady Z., Ramanauskas F., Cain T.M. and Johnston P.N. Assessment of paediatric CT dose
2 indicators for the purpose of optimisation. *Br J Radiol.* 2012;85(1019):1488-1498.
3 doi:10.1259/bjr/28015185.
4
- 5 Brindhavan, A., and Eze, C. U. (2006). Estimation of radiation dose during diagnostic X-ray
6 examinations of newborn babies and 1-year-old infants. *Medical Principles and Practice:*
7 *International Journal of the Kuwait University, Health Science Centre*, 15(4), 260–5.
8 doi:10.1159/000092987
9
- 10 Brisse, H. J. and Aubert, B. (2009). CT exposure from paediatric MDCT: results from the 2007-
11 2008 SFIPP/ISRN survey. *Journal de Radiologie*, 90(2), 207–15. Retrieved from
12 <http://www.ncbi.nlm.nih.gov/pubmed/19308005>.
13
- 14 Buls, N., Bosmans, H. and Mommaert, C. (2010). CT paediatric doses in Belgium: a multi-centre
15 study, (February 2010). Retrieved from <http://www.afcn.be/GED/00000000/2400/2449.pdf>
16
- 17 Bundesamt für Strahlenschutz: Bekanntmachung der aktualisierten diagnostischen Referenzwerte
18 für diagnostische und interventionelle Röntgenuntersuchungen, Vom 22. Juni 2010. Retrieved from:
19 [https://www.bfs.de/DE/themen/ion/anwendung-
21 medizin/diagnostik/referenzwerte/referenzwerte.html](https://www.bfs.de/DE/themen/ion/anwendung-
20 medizin/diagnostik/referenzwerte/referenzwerte.html)
22
- 22 Centers for Disease (CDC) (2015). Data Tables for Weight-for-age Charts, Retrieved from:
23 http://www.cdc.gov/growthcharts/html_charts/wtageinf.htm
24
- 25 Chida, K., Ohno, T., Kakizaki, S., Takegawa, M., Yuuki, H., Nakada, M., Takahashi, S. and
26 Zuguchi, M. (2010). Radiation dose to the paediatric cardiac catheterization and intervention
27 patient. *AJR. American Journal of Roentgenology*, 195(5), 1175–1179. doi:10.2214/AJR.10.4466
28
- 29 Corredoira E, Vañó E, Ubeda C and Gutiérrez-Larraya F. Patient doses in paediatric interventional
30 cardiology: impact of 3D rotational angiography. *J Radiol Prot.* 2015 Mar;35(1):179-95.
31
- 32 CRCPD (2012). Spelic D.C. Nationwide Evaluation of X-Ray Trends. *Journal of the American*
33 *College of Radiology, J Am Coll Radiol.* 2008 Feb;5(2):146-8. doi: 10.1016/j.jacr.2007.11.003
34
- 35 Dabin J., Struelens L. and Vanhavere F. Radiation dose to premature new-borns in the Belgian
36 neonatal intensive care units. *Radiation Protection Dosimetry* (2014), Vol. 158, No. 1, pp. 28–35.
37
- 38 DICOM (2005). Digital Imaging and Communications in Medicine (DICOM). Supplement 94:
39 Diagnostic X-Ray radiation Dose Reporting (Dose SR) (2005).
40
- 41 Dragusin, O., Gewillig, M., Desmet, W., Smans, K., Struelens, L. and Bosmans, H. (2008).
42 Radiation dose survey in a paediatric cardiac catheterisation laboratory equipped with flat-panel
43 detectors. *Radiation Protection Dosimetry*, 129(1-3), 91–95. doi:10.1093/rpd/ncn035
44
- 45 El Sayed, M. H., Roushdy, A. M., El Farghaly, H. and El Sherbini, A. (2012). Radiation exposure
46 in children during the current era of paediatric cardiac intervention. *Paediatric Cardiology*, 33(1),
47 27–35. Retrieved from <http://www.ncbi.nlm.nih.gov/pubmed/21811814>
48
- 49 Emigh, B., Gordon, C. L., Connolly, B. L., Falkiner M. and Thomas K. E. Effective dose estimation
50 for paediatric upper gastrointestinal examinations using an anthropomorphic phantom set and metal

1 oxide semiconductor field-effect transistor (MOSFET) technology. *Pediatr Radiol* 43:1108-1116,
2 2013

3

4 European Commission (EC), 1996. European guidelines on quality criteria for diagnostic
5 radiographic images in paediatrics, Report EUR 16261EN.

6

7 European Commission (EC), 1999. Guidance on Diagnostic Reference Levels (DRLs) for medical
8 exposures, Radiation Protection 109.

9

10 European Commission (EC), 2009. European commission guidelines on clinical audit for medical
11 radiological practices (diagnostic radiology, nuclear medicine and radiotherapy), Radiation
12 Protection 159.

13

14 European Commission (EC), 2012. Cone beam CT for dental and maxillofacial radiology
15 (Evidence-based guidelines), Radiation Protection No 172.

16

17 European Commission (EC), 2013. European Council Directive 2013/59/Euratom Basic Safety
18 Standards (BSS).

19

20 European Commission (EC), 2014. Dose Datamed 2 (DDM2) Project Report Part 2: Diagnostic
21 Reference Levels (DRLs) in Europe.

22

23 Foley, S. J., McEntee, M. F. and Rainford, L. A. (2012). Establishment of CT diagnostic reference
24 levels in Ireland. *The British Journal of Radiology*, 85(1018), 1390–7. doi:10.1259/bjr/15839549

25

26 Fukushima, Y., Tsushima, Y., Takei, H., Taketomi-Takahashi, A., Otake, H. and Endo, K. (2012).
27 Diagnostic reference level of computed tomography (CT) in Japan. *Radiation Protection Dosimetry*,
28 151(1), 51–7. doi:10.1093/rpd/ncr441

29

30 Galanski, M., Nagel, H.-D., & Stamm, G., "Pädiatrische CT-Expositionspraxis in der
31 Bundesrepublik Deutschland", UFO-Vorhaben StSch 4470, 2006. Available at: [https://www.mh-
32 hannover.de/fileadmin/kliniken/diagnostische_radiologie/download/Report_Paed-CT-
33 Umfrage_2005_06.pdf](https://www.mh-hannover.de/fileadmin/kliniken/diagnostische_radiologie/download/Report_Paed-CT-Umfrage_2005_06.pdf).

34

35 Goske, M., Strauss, K. J., Coombs, L. P., Mandel, K. E., Towbin, A. J., Larson, D. B., Callahan M.
36 J., Darge K., Podberesky D. J., Frush D. P., Westra S. J. and Prince, J. S. (2013). Diagnostic
37 Reference Ranges for pediatric abdominal CT. *Radiology*. 2013 Jul;268(1):208-18. doi:
38 10.1148/radiol.13120730. Epub 2013 Mar 19

39

40 Govia K., Connolly B. L., Thomas, K. E., and Gordon, C. L. Estimates of effective dose to
41 paediatric patients undergoing enteric and venous access procedures. *J Vasc Interv Radiol* 23:443-
42 450. 2012

43

44 Granata C., Origgi D., Palorini F., Matranga D. and Salerno S. Radiation dose from multidetector
45 CT studies in children: results from the first Italian nationwide survey. *Pediatr Radiol*. 2015 May;
46 45(5):695-705.

47

48 Harbron R. W., Pearce M. S., Salotti J. A., McHugh K., McLaren C., Abernethy L., Reed S.,
49 O’Sullivan J. and Chapple C.-L. Radiation doses from fluoroscopically guided cardiac

1 catheterization procedures in children and young adults in the United Kingdom: a multicentre study,
2 Br. J. Radiol. 88 (2014).
3
4 Hart D., Hillier M.C. and Shrimpton P.C. Doses to patients from Radiographic and Fluoroscopic X-
5 ray Imaging Procedures in the UK – 2010 Review. Health Protection Agency (UK) ReportHPA-
6 CRCE-034 (2012).
7
8 Hart D., Hillier M.C. and Wall B.F. Doses to patients from medical X-ray examinations in the UK –
9 2000 review. NRPB-W14 (2002).
10
11 Hart D. and Wall B.F. Development of diagnostic reference levels in paediatric radiology, IAEA-
12 CN-85-56. Retrieved from:
13 http://www.iaea.org/inis/collection/NCLCollectionStore/_Public/32/039/32039917.pdf
14
15 Hart D., Wall B. F., Shrimpton P. C., Bungay D. R. and Dance D. R. (2000). Reference doses and
16 patient size in paediatric radiology. Report NRPB-R318. www.hpa.org.uk.
17
18 Harvey H. B., Brink J. A. and Frush D. P. Informed consent for radiation risk from CT is unjustified
19 based on the current scientific evidence, *Radiology* 275 (2015) 2, 321-325.
20
21 Hayton, A., Wallace, A., Marks, P., Edmonds, K., Tingey, D. and Johnston, P. (2013). Australian
22 diagnostic reference levels for multi detector computed tomography. *Australasian Physical &
23 Engineering Sciences in Medicine / Supported by the Australasian College of Physical Scientists in
24 Medicine and the Australasian Association of Physical Sciences in Medicine*, 36(1), 19–26.
25 doi:10.1007/s13246-013-0180-6
26
27 Hioms, M. P., Saini, A. and Marden, P. J. A review of current local dose-area product levels for
28 paediatric fluoroscopy in a tertiary referral centre compared with national standards. Why are they
29 so different? *Br J Radiol* 79:326-330, 2006
30
31 HSE Medical Exposures Radiation Unit (2013). Radiation Protection Manual. Section 7: Diagnostic
32 Reference Levels, page 6. Available at:
33 [http://www.hse.ie/eng/about/Who/qualityandpatientsafety/safepatientcare/medexpradiationunit/RP%](http://www.hse.ie/eng/about/Who/qualityandpatientsafety/safepatientcare/medexpradiationunit/RP%20Manual%202013.pdf)
34 [20Manual%202013.pdf](http://www.hse.ie/eng/about/Who/qualityandpatientsafety/safepatientcare/medexpradiationunit/RP%20Manual%202013.pdf)
35
36 Hsi, R. S., Dearn, J., Dean, M., Zamora, D. A., Kanal, K. M., Harper, J. D. and Merguerian, P. A.
37 (2013). Effective and organ specific radiation doses from videourodynamics in children.
38 *The Journal of Urology*, 190(4), 1364–9. Retrieved from
39 <http://www.ncbi.nlm.nih.gov/pubmed/23707437>
40
41
42 Integrating the Healthcare Enterprise (IHE) (2014a). www.ihe.net (retrieved July 2014).
43
44 Integrating the Healthcare Enterprise (IHE) (2014b).
45 http://wiki.ihe.net/index.php?title=Radiation_Exposure_Monitoring (retrieved July 2014).
46
47 International Atomic Energy Agency (IAEA), International Basic Safety Standards for Protection
48 against Ionizing Radiation and for the Safety of Radiation Sources, Safety Series No. 115, Rep. No.
49 115, IAEA, Vienna (1996).
50

1
2 International Atomic Energy Agency (IAEA), Dosimetry in Diagnostic Radiology: An International
3 Code of Practice, Technical Reports Series No. 457, IAEA, Vienna (2007)
4
5 International Atomic Energy Agency (IAEA), Radiation protection in Paediatric Radiology, Safety
6 reports series no. 71, IAEA, Vienna (2012).
7
8 International Atomic Energy Agency (IAEA). Dosimetry in Diagnostic Radiology for Paediatric
9 Patients, 2013. IAEA Human Health Series No 24.
10
11 International Atomic Energy Agency (IAEA). Diagnostic Radiology Physics, A handbook for
12 Teachers and Students, 2014. Technical editors: Dance, D. R., Christofides, S., Maidment A. D. A.,
13 McLean, I. D. and Ng, K. H.
14
15 International Commission on Radiation Units and Measurements (ICRU), Patient Dosimetry for X
16 Rays Used in Medical Imaging, ICRU Rep. 74, ICRU, Bethesda, MD (2006).
17
18 International Commission on Radiation Units and Measurements (ICRU). Radiation dose and
19 image-quality assessment in computed tomography, ICRU Report 87, Journal of the ICRU Volume
20 12 No 1 2012.
21
22 International Commission on Radiological Protection (ICRP) (1991). 1990 Recommendations of
23 International Commission on Radiological Protection. ICRP Publication 60. Ann. ICRP 21 (1-3).
24
25 International Commission on Radiological Protection (ICRP) (1996). Radiological protection in
26 medicine. ICRP Publication 73. Ann. ICRP 26 (2).
27
28 International Commission on Radiological Protection (ICRP) (2001). Radiation and your patient: A
29 guide for medical practitioners. ICRP Supporting Guidance 2. Ann. ICRP 31 (4).
30
31 International Commission on Radiological Protection (ICRP) (2007a). The 2007 Recommendations
32 of International Commission on Radiological Protection. Ann. ICRP 37 (2-4).
33
34 International Commission on Radiological Protection (ICRP) (2007b). Radiological protection in
35 medicine. ICRP Publication 105. Ann. ICRP 37 (5).
36
37 International Commission on Radiological Protection (ICRP) (2013). Radiological Protection in
38 paediatric diagnostic and interventional radiology, ICRP-121.
39
40 International Commission on Radiological Protection (ICRP) (2013). Radiological protection in
41 cardiology. ICRP Publication 120. Ann. ICRP 42 (1).
42 International Commission on Radiological Protection (ICRP) (2015). Radiological Protection in
43 Cone Beam Computed Tomography (CBCT). ICRP Publication 129, Annals of the ICRP 44(1),
44 2015.
45
46 International Electrotechnical Commission (IEC) (2002). IEC 60601-2-44. Medical electrical
47 equipment – Part 2-44: Particular requirements for the safety of X-ray equipment for computed
48 tomography.
49

- 1 International Electrotechnical Commission (IEC) (2007). IEC/PAS 61910-1. Medical electrical
2 equipment – Radiation dose documentation – Part 1: Equipment for radiography and radioscopy.
3
- 4 International Electrotechnical Commission (IEC) (2010). IEC 60601-2-43. Medical electrical
5 equipment – Part 2-43: Particular requirements for the basic safety and essential performance of X-
6 ray equipment for interventional procedures.
7
- 8 Institute of Physics and Engineering in Medicine (IPEM) (2004). Guidance on the Establishment
9 and Use of Diagnostic Reference Levels for Medical X-Ray Examinations. IPEM Report 88. York,
10 UK.
11
- 12 Journy N., Rehe J.-L., Ducou Le Pointe H., Lee C., Brisse H., Chateil J.-F., Caer-Lorho S., Laurier
13 D. and Bernier M.-O. Are the studies on cancer risk from CT scans biased by indication? Elements
14 of answer from a large-scale cohort study in France. *Br. J. Cancer* 112 (2015), 185-193.
15
- 16 Järvinen, H., Merimaa, K., Seuri, R., Tyrväinen, E., Perhomaa, M., Savikurki-Heikkilä, P.,
17 Svedström, E., Ziliukas, J., Lintrop, M. (2011). Patient doses in paediatric CT: feasibility of setting
18 diagnostic reference levels. *Radiation Protection Dosimetry*, 147(1-2), 142–6.
19 doi:10.1093/rpd/ncr293
20
- 21 Järvinen H., Seuri R., Kortnesniemi M., Lajunen A., Hallinen E., Savikurki-Heikkilä P., Laarne P.,
22 Perhomaa M., and Tyrväinen E. Indication based national diagnostic reference levels (DRL) for
23 paediatricCT: a new approach with proposed values, Paper to be published in RPD, 2015.
24
- 25 Kharita, M. H. and Khazzam, S. (2010). Survey of patient dose in computed tomography in Syria
26 2009. *Radiation Protection Dosimetry*, 141(2), 149–61. doi:10.1093/rpd/ncq155
27
- 28 Kiljunen T., Järvinen H. and Savolainen S. Diagnostic reference levels for thorax X-ray
29 examinations of paediatric patients. *Br J Radiol.* 2007;80(954):452-9. doi:10.1259/bjr/60918774.
30
- 31 Kim, B. H., Do, K.-H., Goo, H. W., Yang, D. H., Oh, S. Y., Kim, H. J., Lee, K. Y. and Lee, J. E.
32 (2012). National survey of radiation doses of paediatric chest radiography in Korea: analysis of the
33 factors affecting radiation doses. *Korean Journal of Radiology: Official Journal of the Korean*
34 *Radiological Society*, 13(5), 610–7. doi:10.3348/kjr.2012.13.5.610
35
- 36 Krille, L., Dreger, S., Schindel, R., Albrecht, T., Asmussen, M., Barkhausen, J., Berthold, J. D.,
37 Chavan, A., Claussen, C., Forsting, M., Gianicolo, E. A. L., Jablonka, K., Jahnen, A., Langer, M.,
38 Laniado, M., Lotz, J., Mentzel, H. J., Queißer-Wahrendorf, A., Rompel, O., Schlick, I., Schneider,
39 K., Schumacher, M., Seidenbusch, M., Spix, C., Spors, B., Staatz, G., Vogl, T., Wagner, J.,
40 Weisser, G., Zeeb, H. and Blettner, M. Risk of cancer incidence before the age of 15 years after
41 exposure to ionising radiation from computed tomography: results from a German cohort study
42 *Radiat Environ Biophys* (2015) 54:1-12.
43
- 44 Kritsaneepai boon, S., Trinavarat, P. and Visrutaratna, P. (2012). Survey of paediatric MDCT
45 radiation dose from university hospitals in Thailand: a preliminary for national dose survey. *Acta*
46 *Radiologica* (Stockholm, Sweden : 1987), 53(7), 820–6. doi:10.1258/ar.2012.110641
47
- 48 Lassmann, M. and Treves, S. T. (2014). Paediatric radiopharmaceutical administration:
49 harmonization of the 2007 EANM paediatric dosage card (version 1.5.2008) and the 2010 North

- 1 American consensus guidelines. *European Journal of Nuclear Medicine and Molecular Imaging*,
2 41(5), 1036–41. doi:10.1007/s00259-014-2731-9
3
- 4 Lee R, Thomas, K. E., Connolly, B. L., Falkiner M. and Gordon, C. L. Effective dose estimation for
5 cystourethrography using an anthropomorphic phantom set and metal oxide semiconductor field-
6 effect transistor (MOSFET) technology. *Pediatr Radiol* 39:608-615, 2009.
7
- 8 Ludlow, J. B. and Walker, C. (2013). Assessment of phantom dosimetry and image quality of i-
9 CAT FLX cone-beam computed tomography. *American Journal of Orthodontics and Dentofacial*
10 *Orthopedics : Official Publication of the American Association of Orthodontists, Its Constituent*
11 *Societies, and the American Board of Orthodontics*, 144(6), 802–17.
12 doi:10.1016/j.ajodo.2013.07.013
13
- 14 Goske, M. J., Applegate, K. E., Bell, C., Boylan, J., Bulas, D., Butler, P., Callahan, M. J., Coley, B.
15 D., Farley, S., Frush, D. P., McElveny, C., Hernanz-Schulman, M., Johnson, N. D., Kaste, S. C.,
16 Morrison, G. and Strauss, K. J. Image Gently: providing practical educational tools and advocacy to
17 accelerate radiation protection for children worldwide. *Semin Ultrasound CT MR*. 2010
18 Feb;31(1):57-63. doi: 10.1053/j.sult.2009.09.007.
19 Available at: <http://linkinghub.elsevier.com/retrieve/pii/S0887217109000870?showall=true>.
20
- 21 Martin, C.J., 2011. Management of patient dose in radiology in the UK. *Radiat. Prot. Dosim.*147,
22 355–372.
23
- 24 Martin, C.J., Le Heron, J., Borrás, C., Sookpeng, S., Ramirez, G., 2013. Approaches to aspects of
25 optimisation of protection in diagnostic radiology in six continents. *J. Radiol. Prot.* 33, 711–734.
26
- 27 Martinez, L. C., Vano, E., Gutierrez, F., Rodriguez, C., Gilarranz, R. and Manzananas, M. J. (2007).
28 Patient doses from fluoroscopically guided cardiac procedures in paediatrics. *Physics in Medicine*
29 *and Biology*, 52(16), 4749–4759. doi:10.1088/0031-9155/52/16/003
30
- 31 McCollough, C., Branham, T., Herlihy, V., Bhargavan, M., Robbins, L., Bush, K., McNitt-Gray,
32 M., Payne, J. T., Ruckdeschel, T., Pfeiffer, D., Cody, D. and Zeman, R. (2011). Diagnostic
33 reference levels from the ACR CT Accreditation Program. *Journal of the American College of*
34 *Radiology : JACR*, 8(11), 795–803. doi:10.1016/j.jacr.2011.03.014
35
- 36 McFadden, S., Hughes, C., D’Helft, C. I., McGee, A., Rainford, L., Brennan, P. C., McCrum-
37 Gardner E. and Winder, R. J. (2013). The establishment of local diagnostic reference levels for
38 paediatric interventional cardiology. *Radiography* 19 (2013), 295-301.
39 doi:10.1016/j.radi.2013.04.006
40
- 41 McFadden, S. L., Hughes, C. M., Mooney, R. B. and Winder, R. J. (2013). An analysis of radiation
42 dose reduction in paediatric interventional cardiology by altering frame rate and use of the anti-
43 scatter grid. *Journal of Radiological Protection : Official Journal of the Society for Radiological*
44 *Protection*, 33(2), 433–443. doi:10.1088/0952-4746/33/2/433
45
- 46 McFadden, S. L., Hughes, C. M. and Winder, R. J. (2013a). Variation in radiographic protocols in
47 paediatric interventional cardiology. *Journal of Radiological Protection : Official Journal of the*
48 *Society for Radiological Protection*, 33(2), 313–319. doi:10.1088/0952-4746/33/2/313
49
- 50 Medical Council (Ireland), 3 September 2004. Diagnostic Reference Levels, Position paper.

1
2 Miller, D. L. (2013). Efforts to optimize radiation protection in interventional fluoroscopy. *Health*
3 *Physics*, 105(5), 435–44. Retrieved from <http://www.ncbi.nlm.nih.gov/pubmed/24077043>
4
5 Mattheews JD, Forsythe AV, Brady Z, Butler MW, Goergen SK, Byrnes GB, Giles GG, Wallace
6 AB, Anderson PR, Guiver TA, McGale P, Cain TM, Dowty JG, Bickerstaffe AC, Darby SC. *BMJ*
7 2013 21;346:f2360
8
9 Mohiy, H. Al, Sim, J., Seeram, E., Annabell, N., Geso, M., Mandarano, G. and Davidson, R.
10 (2012). A dose comparison survey in CT departments of dedicated paediatric hospitals in Australia
11 and Saudi Arabia. *World Journal of Radiology*, 4(10), 431–8. doi:10.4329/wjr.v4.i10.431
12
13 Montgomery, A. and Martin C. J. A study of the application of paediatric reference levels. *BrJ*
14 *Radiol* (2000), 73:1083-90.
15
16 Naidich, D. P., Marshall, C. H., Gribbin, C., Arams, R. S. and McCauley, D. I. (1990). Low-dose
17 CT of the lungs: preliminary observations. *Radiology*, 175(3), 729–31.
18 doi:10.1148/radiology.175.3.2343122
19
20 Natarajan, M. K., Paul, N., Mercuri, M., Waller, E. J., Leipsic, J., Traboulsi, M., Banijamali, H. S.,
21 Benson, L., Sheth, T.N.; Secondary Panel: Simpson, C.S., Brydie, A., Love, M.P., Gallo, R. (2013).
22 Canadian Cardiovascular Society position statement on radiation exposure from cardiac imaging
23 and interventional procedures. *The Canadian Journal of Cardiology*, 29(11), 1361–8. Retrieved
24 from <http://www.ncbi.nlm.nih.gov/pubmed/24035289>
25
26 HSE Medical Exposures Radiation Unit (2013). *Radiation Protection Manual. Section 7: Diagnostic*
27 *Reference Levels*.
28
29 NCRP 172: Reference levels and achievable doses in medical and dental imaging:
30 recommendations for the United States. Recommendations of the National Council on Radiation
31 Protection and Measurements, September 30, 2012.
32
33 Noffke, C. E. E., Farman, A. G., Nel, S. and Nzima, N. (2011). Guidelines for the safe use of dental
34 and maxillofacial CBCT: a review with recommendations for South Africa. *SADJ : Journal of the*
35 *South African Dental Association = Tydskrif van Die Suid-Afrikaanse Tandheelkundige*
36 *Vereniging*, 66(6), 262, 264–6. Retrieved from <http://www.ncbi.nlm.nih.gov/pubmed/23198473>
37
38 Onnasch, D. G. W., Schröder, F. K., Fischer, G. and Kramer, H.-H. (2007). Diagnostic reference
39 levels and effective dose in paediatric cardiac catheterization. *The British Journal of Radiology*,
40 80(951), 177–185. doi:10.1259/bjr/19929794
41
42 Papadopoulou, D., Yakoumakis, E., Sandilos, P., Thanopoulos, V., Makri, T., Gialousis, G.,
43 Houndas, D., Yakoumakis, N. and Georgiou, E. (2005). Entrance radiation doses during paediatric
44 cardiac catheterisations performed for diagnosis or the treatment of congenital heart disease.
45 *Radiation Protection Dosimetry*, 117(1-3), 236–240. doi:10.1093/rpd/nci755
46
47 Pearce MS, Salotti JA, Little MP, McHugh K, Lee C, Kim KP, Howe NL, Ronckers CM,
48 Rajaraman P, Sir Craft AW, Parker L, Berrington de Gonzalez A. *Lancet* 2012 4;380:499-505
49

- 1 Prins, R., Dauer, L. T., Colosi, D. C., Quinn, B., Kleiman, N. J., Bohle, G. C., Holohan, B., Al-
2 Najjar, A., Fernandez, T., Bonvento, M., Faber, R.D., Ching, H. and Goren, A. D. (2011).
3 Significant reduction in dental cone beam computed tomography (CBCT) eye dose through the use
4 of leaded glasses. *Oral Surgery, Oral Medicine, Oral Pathology, Oral Radiology, and Endodontics*,
5 112(4), 502–7. doi:10.1016/j.tripleo.2011.04.041
6
- 7 Radiation and Nuclear Safety Authority (STUK) (2013), Helasvuo T (Ed.). Number of radiological
8 examinations in Finland in 2011, Report STUK-B 161 (In Finnish; abstract in English).
9
- 10 Roch P. and Aubert B. French diagnostic reference levels in diagnostic radiology, computed
11 tomography and nuclear medicine: 2004-2008 review. *Radiat Prot Dosimetry*. 2013;154(1):52-75.
12 doi:10.1093/rpd/ncs152.
13
- 14 Ruiz-Cruces, R. (2015). Estimación de las dosis poblaciones en España (DOPOES project).
15 Memorandum of specific agreement between Spanish Nuclear Safety Council and the University of
16 Malaga).
17
- 18 Santos J., Foley S., Paulo G., McEntee M.F. and Rainford L. The establishment of computed
19 tomography diagnostic reference levels in Portugal. *Radiat Prot Dosimetry*. 2013;nct226-
20 doi:10.1093/rpd/nct226.
21
- 22 Schneider K., Kohn, M. M. and Ernst, G. The derivation of reference dose values to chest X-rays in
23 paediatric radiography. *Radiation Protection Dosimetry* (1998), 80: 199-202.
24
- 25 Schulze, R. (2013). Radiation protection vs research interests. *Dento Maxillo Facial Radiology*,
26 42(2), 20120348. doi:10.1259/dmfr.20120348
27
- 28 Segall, G., Delbeke, D., Stabin, M. G., Even-Sapir, E., Fair, J., Sajdak, R. and Smith, G. T. (2010).
29 SNM practice guideline for sodium 18F-fluoride PET/CT bone scans 1.0. *Journal of Nuclear*
30 *Medicine: Official Publication, Society of Nuclear Medicine*, 51(11), 1813–20.
31 doi:10.2967/jnumed.110.082263.
32
- 33 Seidenbusch, M. C. and Schneider, K. (2008). Radiation exposure of children in paediatric
34 radiology. *RöFo: Fortschritte Auf Dem Gebiete Der Röntgenstrahlen Und Der Nuklearmedizin*,
35 180(5), 410–22. Retrieved from <http://www.ncbi.nlm.nih.gov/pubmed/18438743>.
36
- 37 Seidenbusch, M. C. and Schneider, K. Radiation exposure of the mammarian glands in paediatric
38 high resolution computed tomographic (HRCT) examinations, *Pediatr Radiol* (2013) 43 (Suppl
39 3):S459–S656).
40
- 41 Shrimpton, P. C. and Wall, B. F. (2000). Reference doses for paediatric computed tomography.
42 *Radiat Prot Dosimetry*, 90(1), 249–252.
43
- 44 Shrimpton, P. C., Hillier, M. C., Lewis, M. A. and Dunn, M. (2006). National survey of doses from
45 CT in the UK: 2003. *British Journal of Radiology*, 79(948), 968–980. doi:10.1259/bjr/93277434
46
- 47 Shrimpton, P. C., Hillier, M. C., Meeson, S. and Golding, S. (2014). Doses from Computed
48 Tomography (CT) Examinations in the UK – 2011 Review. Chilton, England.
49

- 1 Smans, K., Vano, E., Sanchez, R. M., Schultz, F. W., Zoetelief, J. and Kiljunen T. Results of a
2 European survey on patient doses in paediatric radiology. *Radiat Prot Dosimetry* (2008), 129: 204-
3 10.
4
- 5 Sonawane, A. U., Sunil Kumar, J. V. K., Singh, M. and Pradhan, A. S. (2011). Suggested diagnostic
6 reference levels for paediatric X-ray examinations in India. *Radiation Protection Dosimetry*, 147(3),
7 423–8. doi:10.1093/rpd/ncq458
8
- 9 Stauss, J., Hahn, K., Mann, M. and De Palma, D. (2010). Guidelines for paediatric bone scanning
10 with ^{99m}Tc-labelled radiopharmaceuticals and ¹⁸F-fluoride. *European Journal of Nuclear*
11 *Medicine and Molecular Imaging*, 37(8), 1621–8. doi:10.1007/s00259-010-1492-3
12
- 13 Stecker M.S., Balter, S., Towbin, R. B., Miller, D. L., Vañó, E., Bartal, G., Angle, J.F., Chao, C. P.,
14 Cohen, A. M., Dixon, R.G., Gross, K., Hartnell, G.G., Schueler, B., Statler, J. D., de Baère, T., and
15 Cardella, J.F., for the SIR Safety and Health Committee and the CIRSE (2009). Guidelines for
16 Patient Radiation Dose Management. *J Vasc Interv Radiol* 20:S263-273.
17
- 18 Tapiovaara M. and Siiskonen T. (2008). A Monte Carlo program for calculating patient doses in
19 medical X-ray examinations, STUK-A231, 2nd ed. STUK, Finland.
20
- 21 Treier, R., Aroua, A., Verdun, F. R., Samara, E., Stuessi, A. and Trueb, P. R. (2010). Patient doses
22 in CT examinations in Switzerland: implementation of national diagnostic reference levels.
23 *Radiation Protection Dosimetry*, 142(2-4), 244–254. doi:10.1093/rpd/ncq279
24
- 25 Tsapaki, V., Aldrich, J. E., Sharma, R., Staniszewska, M. A., Krisanachinda, A., Rehani, M.,
26 Hufton, A., Triantopoulou, C., Maniatis, P. N., Papailiou, J. and Prokop, M. (2006). Dose reduction
27 in CT while maintaining diagnostic confidence: diagnostic reference levels at routine head, chest,
28 and abdominal CT--IAEA-coordinated research project. *Radiology*, 240(3), 828–834.
29 doi:10.1148/radiol.2403050993
30
- 31 Tsapaki, V., Kottou, S., Korniotis, S., Nikolaki, N., Rammos, S. and Apostolopoulou, S.C.
32 Radiation doses in paediatric interventional cardiology procedures. *Radiat Prot Dosimetry*.
33 2008;132(4):390-394.
34
- 35 Ubeda, C., Vano, E., Miranda, P., Leyton, F., Martinez, L. C. and Oyarzun, C. Radiation dose and
36 image quality for paediatric interventional cardiology systems. A national survey in Chile. *Radiat*
37 *Prot Dosimetry* 147:429-438, 2011
38
- 39 Ubeda, C., Vano, E., Miranda, P. and Leyton F. Pilot program on patient dosimetry in pediatric
40 interventional cardiology in Chile, *Med. Phys.* 39 (5), 2012: 2424-2430.
41
- 42 Ubeda, C, Miranda, P. and Vano E. Local patient dose diagnostic reference levels in paediatric
43 interventional cardiology in Chile using age bands and patient weight values. *Med Phys.* 2015
44 Feb;42(2): 615-22
45
- 46 United Nations Scientific Committee on the Effects of Atomic Radiation (UNSCEAR). UNSCEAR
47 2013 Report, Volume II, Scientific Annex B: Effects of radiation exposure of children. United
48 Nations 2013.
49

1 Vano, E., Ubeda, C., Leyton, F., & Miranda, P. (2008). Radiation dose and image quality for
2 paediatric interventional cardiology. *Physics in Medicine and Biology*, 53(15), 4049–4062.
3 doi:10.1088/0031-9155/53/15/003
4

5 Vano, E., Järvinen, H., Kosunen, A., Bly, R., Malone, J., Dowling, A., Larkin, A., Padovani, R.,
6 Bosmans, H., Dragusin, O., Jaschke, W., Torbica, P., Back, C., Schreiner, A., Bokou, C., Kottou,
7 S., Tsapaki, V., Jankowski, J., Papierz, S., Domienik, J., Werduch, A., Nikodemova, D., Salat, D.,
8 Kepler, K., Bor, M.D., Vassileva, J., Borisova, R., Pellet, S. and Corbett, R.H. Patient dose in
9 interventional radiology: A European survey. *Radiation Protection Dosimetry* 2008; 129 (1-3): 39-
10 45.
11

12 Vano, E., Ubeda, C., Miranda, P., Leyton F., Duran, A. and Nader A. Radiation protection in
13 paediatric interventional cardiology: an IAEA pilot program in Latin America. *Health Phys*
14 101:233-237, 2011
15

16 Vassileva J., Rehani M., Kostova-Lefterova D., Al-Naemi H. M., Al Suwaidi J. S., Arandjic D.,
17 Bashier, E. H., Kodlulovich, R. S., El-Nachef, L., Aguilar, J. G., Gershan, V., Gershkevitch, E.,
18 Gruppetta, E., Hustuc, A., Jauhari, A., Kharita, M. H., Khelassi-Toutaoui, N., Khosravi, H. R.,
19 Khoury, H., Kralik, I., Mahere, S., Mazuoliene, J., Mora, P., Muhogora, W., Muthuvelu, P.,
20 Nikodemova, D., Novak, L., Pallewatte, A., Pekarovič, D., Shaaban, M., Shelly, E., Stepanyan, K.,
21 Thelsy, N., Visrutaratna, P. and Zaman A., A study to establish international diagnostic reference
22 levels for paediatric computed tomography. *Radiation Protection Dosimetry* 2015 Jul;165(1-4):70-
23 80.
24

25 Vassileva J. and Rehani M. Patient grouping for dose surveys and establishment of diagnostic
26 reference levels in paediatric computed tomography. *Radiation Protection Dosimetry* 2015
27 Jul;165(1-4):81-85.
28

29 Vassileva, J., Rehani, M. M., Applegate, K., Ahmed, N. a, Al-Dhuhli, H., Al-Naemi, H. M. and
30 Zontar, D. (2012). IAEA Survey of Pediatric CT Practice in 40 Countries in Asia, Europe, Latin
31 America, and Africa: Part 1, Frequency and Appropriateness. *AJR* 2012; 198:1021–1031.
32

33 Vassileva, J., and Stoyanov, D. (2010). Quality control and patient dosimetry in dental cone beam
34 CT. *Radiation Protection Dosimetry*, 139(1-3), 310–312. doi:10.1093/rpd/ncq011
35

36 Veit, R., Guggenberger, R., Noßke, D., Brix, G., "Diagnostische Referenzwerte fuer
37 Röntgenuntersuchungen", *Radiologe* 2010, 50, 907-912.
38

39 Verdun F.R., Gutierrez D., Vader J.P., Aroua A., Alamo-Maestre, L.T., Bochud F. and Gudinchet
40 F. CT radiation dose in children: a survey to establish age-based diagnostic reference levels in
41 Switzerland, *Eur. Radiol.* (2008) 18: 1980-1986. doi:10.1007/s00330-008-0963-4.
42

43 Wambani, J. S., Korir, G. K., Korir, I. K., Kilaha, S. Establishment of local diagnostic reference
44 levels in paediatric screen-film radiography at a children's hospital. *Radiat Prot Dosimetry* (2013),
45 154:465-76.
46

47 Watson, D. J. and Coakley, K. S. (2010). Paediatric CT reference doses based on weight and CT
48 dosimetry phantom size: local experience using a 64-slice CT scanner. *Paediatric Radiology*, 40(5),
49 693–703. doi:10.1007/s00247-009-1469-1
50

- 1 Yakoumakis, E., Karlatira, M., Gialousis, G., Dimitriadis, a, Makri, T. and Georgiou, E. (2009).
2 Effective dose variation in paediatric computed tomography: dose reference levels in Greece.
3 Health Physics, 97(6), 595–603. doi:10.1097/01.HP.0000363840.78169.1b
4
- 5 Yakoumakis, E., Kostopoulou, H., Makri, T., Dimitriadis, A., Georgiou, E. and Tsalafoutas, I.
6 (2013). Estimation of radiation dose and risk to children undergoing cardiac catheterization for the
7 treatment of a congenital heart disease using Monte Carlo simulations. Paediatric Radiology, 43(3),
8 339–346. doi:10.1007/s00247-012-2510-3
9
- 10 Yakoumakis, E., Dimitriadis, A., Gialousis, G., Makri, T., Karavasilis, E. and Giakoumakis, N.
11 Evaluation of organ and effective doses during paediatric barium meal examinations using PCXMC
12 2.0 Monte Carlo Code. Rad Prot Dos 2014 doi:10.1093/rpd/ncul74.

1 **ANNEX A. NATIONAL DRL VALUES FOR PAEDIATRIC EXAMINATIONS AND**
2 **PROCEDURES IN EUROPEAN COUNTRIES**

3 The NDRL data in this Annex is based on DDM2 database, an update by PIDRL questionnaire
4 (Annex C, Section C.2.1), and a literature review (Annex C, Section C.2.2). Only NDRLs accepted
5 by an authoritative body have been presented.

6
7 Table A.1. DRLs for paediatric x-ray procedures: head, skull and sinuses.

Country	Procedure & quantity					
	Head, skull AP/PA		Head, skull LAT		Waters projection	
	K _{a,e} or K _{a,i} , mGy	P _{KA} , mGy*cm ²	K _{a,e} or K _{a,i} , mGy	P _{KA} , mGy*cm ²	K _{a,e} , mGy	P _{KA} , mGy*cm ²
AT	K _{a,i} , Ref ² 0.35 (0y) 0.60 (1y) 0.75 (5y) 0.90 (10y) 1.00 (15y)	Ref ^{1,2} 150(0y) 250 (1y) 350 (5y) 450(10y) 500(15y)	K _{a,i} , Ref ² 0.30 (0y) 0.40 (1y) 0.50 (5y) 0.55 (10y) 0.60 (15y)	Ref ^{1,2} 100(0y) 200 (1y) 250 (5y) 300(10y) 350(15y))		
CY	K _{a,e} , Ref ^{1,3} 1.5 (5y)		K _{a,e} , Ref ^{1,3} 1.0 (5y)			
DE		AP, Ref ^{1,4} 200(10±2mo) 300 (5±2y)		Ref ^{1,4} 200 (10±2mo) 250 (5±2y)		
ES		AP, Ref ⁵ 130 (0y) 230 (1y-5y) 350 (6y-10y) 430 (11y-15y)				
FI					Ref ^{1,6} 2 (7-15 y)	Ref ^{1,6} 250 (7-15 y)
IE	K _{a,e} , Ref ^{7,8} 1.37 (5y)		K _{a,e} , Ref ^{7,8} 0.82 (5y)			
IT	K _{a,e} , Ref ^{1,3} 1.5 (5y)		K _{a,e} , Ref ^{1,3} 1.0 (5y)			
LT	K _{a,e} , Ref ¹ 0.8 (1y) 1.0 (5y) 1.3 (10y) 1.5 (15y)	Ref ¹ 200 (1y) 290 (5y) 350 (10y) 410 (15y)	K _{a,e} , Ref ¹ 0.4 (1y) 0.5 (5y) 0.6 (10y) 0.65 (15y)	Ref ¹ 160 (1y) 260 (5y) 270 (10y) 380 (15y)		
LU	K _{a,e} , Ref ^{1,3} 1.5 (5y)		K _{a,e} , Ref ^{1,3} 1.0 (5y)			
PL	K _{a,e} , Ref ^{1,3} 1.5 (5y)		K _{a,e} , Ref ^{1,3} 1.0 (5y)			
RO	K _{a,e} , Ref ^{1,3} 1.5 (5y)		K _{a,e} , Ref ^{1,3} 1.0 (5y)			

8 ¹Questionnaire, ²Billiger et al., 2010, ³EC 1999 (Radiation Protection 109), ⁴Veit et al., 2010, ⁵Ruiz-Cruces, 2015,
9 ⁶STUK resolution 1 Jan 2006 (www.stuk.fi), ⁷Ireland Medical Council, 2004, ⁸HSE Medical Exposures Radiation Unit,
10 2013.

11

12

1 Table A.2. DRLs for paediatric x-ray procedures: thorax. (AP/PA: the same DRL for both AP and
 2 PA projections)

Country	Procedure & quantity				
	Thorax AP/PA		Thorax LAT		Thorax PA+LAT
	K _{a,e} or K _{a,i} , mGy	P _{KA} , mGy*cm ²	K _{a,e} , mGy	P _{KA} , mGy*cm ²	P _{KA} , mGy*cm ²
AT	K _{a,i} , Ref ² 0.05 (0y) 0.06 (1y) 0.07 (5y) 0.09 (10y) 0.11 (15y)	PA, Ref ¹ ; AP/PA, Ref ² 17 (0y) 23 (1y) 26 (5y) 37 (10y) 73 (15y)			
BE		PA, Ref ³ 20 (<1y) 35 (1-<5y) 50 (5-<10y) 120 (10-<15y)			Ref ³ 60 (<1y) 105 (1-<5y) 150 (5-<10y) 350 (10-<15y)
CY	K _{a,e} , Ref ^{1,4} 0,08 (newborn)(AP) 0.1(5y)		Ref ^{1,4} 0.2 (5y)		
DE		AP/PA, Ref ⁵ 3 (about 1000 g) 5 (about 3000 g) 15 (10±2mo) 25 (5±2y) 35 (10±2y)		Ref ⁵ 40 (5±2y) 60 (10±2y)	
DK	K _{a,e} , Ref ¹ 0.080 (5y; exp scaling with equiv.diam. for other ages)		Ref ¹ 0.095 (5y; exp scaling with eq.diam. for other ages)		
ES		PA, Ref ⁶ 40 (0y) 50 (1y-5y) 85 (6y-10y) 100 (11y-15y)			
FI	K _{a,e} , Ref ^{1,7,8} DRL-curve as a function of patient width	Ref ^{1,7,8} DRL-curve as a function of patient width	Ref ^{1,7,8} DRL-curve as a function of patient width	Ref ^{1,7,8} DRL-curve as a function of patient width	
FR	K _{a,e} , Ref ^{1,9} 0.08 (3,5 kg/ newborn) (AP) 0.08 (10 kg/1y) (AP) 0.1 (20 kg/5y) (PA) 0.2 (30 kg/10y) (PA)	Ref ^{1,9} 10 (3.5 kg/ newborn) (AP) 20 (10 kg/1 y) (AP) 50 (20 kg/5y) (PA) 70 (30kg/10y) (PA)	Ref ^{1,9} 0.2 (20 kg/5y) 0.3 (30kg/10y)	Ref ^{1,9} 60 (20 kg/5y) 80 (30 kg/10y)	

Country	Procedure & quantity				
	Thorax AP/PA		Thorax LAT		Thorax PA+LAT
	K _{a,e} or K _{a,i} , mGy	P _{KA} , mGy*cm ²	K _{a,e} , mGy	P _{KA} , mGy*cm ²	P _{KA} , mGy*cm ²
IE	K _{a,e} , Ref ^{10, 11} 0.057 (1y) 0.053 (5y) 0,066 (10y) 0.088 (15y)				
IT	K _{a,e} , Ref ^{1,4} 0.08 (newborn)(AP) 0.1 (5y)		Ref ^{1,4} 0.2 (5y)		
LT	K _{a,e} , PA, Ref ¹ 0.06 (1y) 0.07 (5y) 0,08 (10y) 0.09 (15y)	PA, Ref ¹ 50 (1y) 60 (5y) 80 (10y) 100 (15y)			
LU	K _{a,e} , Ref ^{1,4} 0.08 (newborn)(AP) 0.1 (5y)		Ref ^{1,4} 0.2 (5y)		
NL		Ref ¹ 15 (4 kg/0y), 20 (11 kg/1y) 50 (21 kg/5y)			
PL	K _{a,e} , Ref ^{1,4} 0.08 (newborn)(AP) 0.1 (5y)		Ref ^{1,4} 0.2 (5y)		
RO	K _{a,e} , Ref ^{1,4} 0.08 (newborn)(AP) 0.1 (5y)		Ref ^{1,4} 0.2 (5y)		

- 1 ¹Questionnaire, ²Billiger et al., 2010, ³www.fanc.fgov.be, ⁴EC 1999 (Radiation Protection 109), ⁵Veit et al., 2010, ⁶Ruiz-Cruces, 2015, ⁷STUK resolution 1 Jan 2006 (www.stuk.fi), ⁸Kiljunen et al. 2007, ⁹Roch and Aubert, 2012, ¹⁰Ireland Medical Council, 2004, ¹¹HSE Medical Exposures Radiation Unit, 2013.

1 Table A.3. DRLs for paediatric x-ray procedures: abdomen, pelvis, micturating cystourethrography,
 2 barium meal and barium swallow.

Country	Procedure & quantity						
	Abdomen, common technique		Pelvis		Micturating cystourethrography (MCU)	Barium meal	Barium swallow
	K _{a,e} or K _{a,i} , mGy	P _{KA} , mGy*cm ²	K _{a,e} , mGy	P _{KA} , mGy*cm ²	P _{KA} , Gy*cm ²	P _{KA} , Gy*cm ²	P _{KA} , Gy*cm ²
AT	K _{a,i} , AP/PA, Ref ² 0.20 (0y) 0.30 (1y) 0.40 (5y) 0.75 (10y) 1.00(15y)	AP, Ref ¹ ; AP/PA, Ref ² 60 (0y) 90 (1y) 200 (5y) 500 (10y) 700 (15y)			Ref ¹ 0.5 (0y) 0.7 (1y) 1.2 (5y) 2.0 (10y)		
BE		Ref ³ 30 (<1y) 100 (1-<5y) 250 (5-<10y) 450 (10-<15y)					
CY	K _{a,e} , AP/PA, Ref ^{1,4} 1.0 (5y)		AP, Ref ^{1,4} 0.2 (infants) 0.9 (5y)				
DE		AP/PA, Ref ⁵ 200 (10±2mo) 250 (5±2y) 350 (10±2y)		AP, Ref ⁵ 150 (5±2y) 250 (10±2y)	Ref ⁵ 0.1 (ab. 3000g) 0.2 (10±2mo) 0.3 (5±2y) 0.6 (10±2y)		
DK	K _{a,e} , Ref ¹ 0.075 (< 1y)		AP, Ref ¹ 0.375 (5y)		Ref ¹ 0.3 (<1y) 0.9 (1-5y)		
ES		AP, Ref ⁶ 150 (0y) 200 (1y-5y) 225 (6y-10y) 300 (11y-15y)		PA, Ref ⁶ 60 (0y) 180 (1y-5y) 310 (6y-10y) 400 (11y-15y)	Ref ⁶ 0,50 (0y) 0,75 (1y-5y) 0,90 (6y-10y) 1,45 (11y-15y)		
FI					Ref ^{1,7} 0.3 (<1y) 0.9 (1-5y)		
FR	K _{a,e} , Ref ^{1,8} 1.0 (20 kg/5y) 1.5 (30 kg/10y)	Ref ^{1,8} 300 (20 kg/5y) ¹ 700 (30 kg/10y) ^{1,8}	Ref ^{1,8} 0.2 (10 kg/1y) 0.9 (20 kg/5y) 1.5 (30 kg/10y)	Ref ^{1,8} 30 (10 kg/1y) ¹ 200 (20 kg/5y) ^{1,8} 400 (30 kg/10y) ^{1,8}			

Country	Procedure & quantity						
	Abdomen, common technique		Pelvis		Micturating cystourethrography (MCU)	Barium meal	Barium swallow
	K _{a,e} or K _{a,i} , mGy	P _{KA} , mGy*cm ²	K _{a,e} , mGy	P _{KA} , mGy*cm ²	P _{KA} , Gy*cm ²	P _{KA} , Gy*cm ²	P _{KA} , Gy*cm ²
IE	K _{a,e} , AP, Ref ^{9,10} 0.330 (1y) 0.752 (5y)		AP, Ref ^{9, 10} 0.265 (1y) 0.475 (5y) 0.807 (10y) 0.892 (15y)		Ref ^{9,10, 11} 0.4 (0y) 0.9 (1y) 1.1(5y) 2.1 (10y) 4.7(15y)	Ref ^{9,10,11} 0.7 (0y) 2 (1y) 2 (5y) 4.5 (10y) 7.2 (15y)	Ref ^{9,10,11} 0.8 (0y) 1.6 (1y) 1.3(5y) 2.7 (10y) 4.6(15y)
IT	K _{a,e} , AP/PA, Ref ^{1,4} 1.0 (5y)		AP, Ref ^{1,4} 0.2 (infants) 0.9 (5y)				
LT	K _{a,e} , Ref ¹ 0.3 (1y) 0.4 (5y) 0,6 (10y) 0.7 (15y)	Ref ¹ 300 (1y) 800 (5y) 1000 (10y) 1200 (15y)					
LU	K _{a,e} , AP/PA, Ref ^{1,4} 1.0 (5y)		AP, Ref ^{1,4} 0.2 (infants) 0.9 (5y)				
NL		Ref ¹ 15 (4 kg/0y) 100 (11 kg/1y) 250 (21 kg/5y)			Ref ¹ 0.3 (4 kg/0y) 0.7 (11 kg/1y) 0.8 (21 kg/5y)		
PL	K _{a,e} , AP/PA, Ref ^{1,4} 1.0 (5y)		AP, Ref ^{1,4} 0.2 (infants) 0.9 (5y)				
RO	K _{a,e} , AP/PA, Ref ^{1,4} 1.0 (5y)		AP, Ref ^{1,4} 0.2 (infants) 0.9 (5y)				
UK					Ref ¹² 0.1 (0y) 0.3 (1y) 0.3 (5y) 0.4 (10y) 0.9 (15y)	Ref ¹² 0.1 (0y) 0.2 (1y) 0.2 (5y) 0.7 (10y) 2.0 (15y)	Ref ¹² 0.2 (0y) 0.4 (1y) 0.5 (5y) 1.8 (10y) 3.0 (15y)

1 ¹Questionnaire, ²Billiger et al., 2010, ³www.fanc.fgov.be, ⁴EC 1999 (Radiation Protection 109), ⁵Veit et al., 2010,
2 ⁶Ruiz-Cruces, 2015, ⁷STUK resolution 1 Jan 2006 (www.stuk.fi), ⁸Roch and Aubert, 2012, ⁹Ireland Medical Council,
3 2004, ¹⁰HSE Medical Exposures Radiation Unit, 2013, ¹¹Hart et al., 2002, ¹²Hart et al., 2012.

4

1 Table A.4. DRLs for paediatric CT procedures: head. DRLs refer to a complete routine CT
 2 examination (one scan series) and the use of 16 cm phantom, except for (1) BE, where DLP is an
 3 average of plain scans and contrast enhanced scans, and (2) IE, where DLP is the average of routine
 4 CT examination which include both single phase and multi phase scans.

Country	Procedure & quantity						
	CT Head, brain, cranial, skull		CT Face and sinuses, nasal cavity	CT Facial bones		CT Petrous bone	
	DLP, mGy*cm	CTDI _{VOL} , mGy	DLP, mGy*cm	DLP, mGy*cm	CTDI _{VOL} , mGy	DLP, mGy*cm	CTDI _{VOL} , mGy
AT	Ref ¹ 300 (0y) 400 (1y) 600 (5y) 750 (10y) 900 (15y)						
BE	Ref ² 420 (<1y) 540 (1-<5y) 660 (5-<10y) 780 (10-<15y)	Ref ² 22 (<1y) 30 (1-<5y) 40 (5-<10y) 45 (10-<15y)	DLP (mGy cm), sinus ² 50 (1-<5y) 65 (5-<10y) 80 (10-<15y) CTDI _{vol} (mGy), sinus ² 4 (5-<10y) 6 (10-<15y)				
CH	Ref ^{1,3} 290 (newborn) 390 (0-1y) 520 (1-5y) 710 (6-10y) 920 (11-15y)	Ref ^{1,3} 27 (newborn) 33 (0-1y) 40 (1-5y) 50 (6-10y) 50 (11-15y)	Face, nasal cavity, Ref ^{1,3} 70 (newborn) 95 (0-1 y) 125 (1-5 y) 180 (6-10 y) 230 (11-15y)				
DE	Ref ^{1,4} 300 (newborn) 400 (< 1y) 500 (2-5y) 650 (6-10y) 850 (11-15y) 950 (>15y)	Ref ^{1,4} 27 (newborn) 33 (< 1y) 40 (2-5y) 50 (6-10y) 60 (11-15y) 65 (>15y)		Facial bones, Ref ^{1,4} 70 (newborn) 95 (< 1y) 125 (2-5y) 180 (6-10y) 230 (11-15y) 250 (>15y)	Facial bones, Ref ^{1,4} 9 (newborn) 11 (< 1y) 13 (2-5y) 17 (6-10y) 20 (11-15y) 22 (>15y)		
ES	Ref ⁵ 250 (0y) 340 (1y-5y) 450 (6y-10y) 650 (11y-15y)						

Country	Procedure & quantity						
	CT Head, brain, cranial, skull		CT Face and sinuses, nasal cavity	CT Facial bones		CT Petrous bone	
	DLP, mGy*cm	CTDI _{VOL} , mGy	DLP, mGy*cm	DLP, mGy*cm	CTDI _{VOL} , mGy	DLP, mGy*cm	CTDI _{VOL} , mGy
FI	Routine head, Ref ⁶ 330 (<1y) 370 (1-<5y) 460 (5-<10y) 560 (10-15y) Ventricular size, Ref ⁶ 35 (<1-15y)	Routine head, Ref ⁶ 23 (<1y) 25 (1-<5y) 29 (5-<10y) 35 (10-15y) Ventricular size, Ref ⁶ 4 (<1-15y)					
FR	Ref ^{1,7} 420 (10 kg/1y) 600 (20 kg/5y) 900 (30 kg/10y)	Ref ^{1,7} 30 (10 kg/1y) 40 (20 kg/5y) 50 (30 kg/10y)		Ref ^{1,7} 200 (10 kg/1y) 275 (20 kg/5y) 300 (30 kg/10y)	Ref ^{1,7} 25 (10 kg/1y) 25 (20 kg/5y) 25 (30 kg/10y)	Ref ^{1,7} 160 (10 kg/1y) 280 (20 kg/5y) 340 (30 kg/10y)	Ref ^{1,7} 45 (10 kg/1y) 70 (20 kg/5y) 85 (30 kg/10y)
IE	Ref ⁸ 340 (newborn) 470 (1-4y) 620 (5-9y) 850 (10-15y)						
LT	Ref ¹ 570 (1y) 630 (5y) 650 (10y) 830 (15y)						
NL	Ref ¹ 240 (4 kg/0 y) 300 (11kg/1y) 420 (21 kg/5y) 600 (36 kg/10y)	Ref ¹ 20 (4 kg/0 y) 25 (11kg/1y) 35 (21 kg/5y) 50 (36 kg/10y)					
UK	Head (trauma), Ref ⁹ 350 (0-1y) 650 (>1-5y) 860 (>5y)	Head (trauma), Ref ⁹ 25 (0-1y) 40 (>1-5y) 60 (>5y)					

1 ¹Questionnaire, ²www.fanc.fgov.be, ³Galanski and Nagel, 2006, ⁴Veit et al., 2010, ⁵Ruiz-Cruces, 2015, ⁶Järvinen et al.,
2 2015, ⁷Roch and Aubert, 2012, ⁸HSE Medical Exposures Radiation Unit, 2013, ⁹Shrimpton et. al., 2014.

1 Table A.5. DRLs for paediatric CT procedures: chest, abdomen. DRLs refer to a complete routine
 2 CT examination (one scan series) and the use of 32 cm phantom, except for (1) BE, where DLP is
 3 an average of plain scans and contrast enhanced scans, and (2) IE, where DLP is the average of
 4 routine CT examination which include both single phase and multi phase scans.

5

Country	Procedure & quantity			
	CT chest, thorax		CT abdomen	
	DLP, mGy*cm	CTDI _{VOL} , mGy	DLP, mGy*cm	CTDI _{VOL} , mGy
AT	Ref. ¹ 80 (0y) 100 (1y) 150 (5y) 180 (10y) 200 (15y)			
BE	Ref ² 35 (1-<5y) 55 (5-<10y) 130 (10-<15y)	Ref ² 1,5 (1-<5y) 2,0 (5-<10y) 3,5 (10-<15y)	Ref ² 110 (1-<5y) 220 (5-<10y) 330 (10-<15y)	Ref ² 5,0 (5-<10y) 7,5 (10-<15y)
CH	Ref ^{1,9} 12 (newborn) 28 (0-1y) 55 (1-5y) 105 (6-10y) 205 (11-15y)		Ref ^{1,9} 27 (newborn) 70 (0-1y) 125 (1-5y) 240 (6-10y) 500 (11-15y)	
DE	Ref ³ 20 (newborn) 30 (< 1y) 65 (2-5y) 115 (6-10y) 230 (11-15y) 400 (>15y)	Ref ³ 1,5 (newborn) 2 (< 1y) 3,5 (2-5y) 5 (6-10y) 8 (11-15y) 12 (>15y)	Ref ³ 45 (newborn) 85 (< 1y) 165 (2-5y) 250 (6-10y) 500 (11-15y) 900 (>15y)	Ref ³ 2,5 (newborn) 3,5 (< 1y) 6 (2-5y) 8 (6-10y) 13 (11-15y) 20 (>15y)
ES	Ref ⁴ 46 (0y) 82 (1y-5y) 125 (6y-10y) 200 (11y-15y)		Ref ⁴ 95 (0y) 150 (1y-5y) 190 (6y-10y) 340 (11y-15y)	
FI	Ref ⁵ DRL curve as a function of patient weight	Ref ⁵ DRL curve as a function of patient weight	Ref ⁵ DRL curve as a function of patient weight	Ref ⁵ DRL curve as a function of patient weight
FR	Ref ^{1,6} 30 (10 kg/1y) 65 (20 kg/5y) 140 (30 kg/10y)	Ref ^{1,6} 3 (10 kg/1y) 4 (20 kg/5y) 5 (30 kg/10y)	Abdomen- pelvis, Ref ^{1,6} 80 (10 kg/1y) 120 (20 kg/5y) 245 (30 kg/10y)	Abdomen- pelvis, Ref ^{1,6} 4 (10 kg/1y) 5 (20 kg/5y) 7 (30 kg/10y)
IE			Abdomen/ Pelvis, Ref ⁷ 130 (newborn) 160 (1-4y) 230 (5-9y) 400 (10-15y)	

Country	Procedure & quantity			
	CT chest, thorax		CT abdomen	
	DLP, mGy*cm	CTDI _{VOL} , mGy	DLP, mGy*cm	CTDI _{VOL} , mGy
UK	Chest, detect. of malignancy, Ref ⁸ 100 (0-1y) 115 (5y) 185 (10y)	Chest, detect. of malignancy, Ref ⁸ 6 (0-1y) 6,5 (5y) 10 (10y)		

1 ¹Questionnaire, ²www.fanc.fgov.be, ³Veit et al., 2010, ⁴Ruiz-Cruces, 2015, ⁵Järvinen et al., 2015, ⁶Roch and Aubert,
2 2012, ⁷HSE Medical Exposures Radiation Unit, 2013, ⁸Shrimpton et al., 2006, ⁹Galanski and Nagel, 2006.

3

4 Table A.6. DRLs for paediatric CT procedures: lumbar spine, whole body
5 (thorax+abdomen+pelvis). DRLs refer to a complete routine CT examination (one scan series) and
6 the use of 16 cm phantom.

Country	Procedure & quantity	Procedure & quantity	Procedure & quantity
	CT lumbar spine	CT whole body	CT whole body
	DLP, mGy*cm	DLP, mGy*cm	CTDI _{VOL} , mGy
CH	Ref ^{1,2} 42 (newborn) 85 (0-1y) 135 (1-5y) 215 (6-10y) 380 (11-15)		
FI		Whole body (WB; thorax + abdomen), Ref ³ DRL curve as a function of patient weight	Whole body (WB; thorax + abdomen), Ref ³ DRL curve as a function of patient weight

7 ¹Questionnaire, ²Galanski and Nagel, 2006, ³Järvinen et al., 2015

8

9

1 Table A.7. DRL curves (FI). Data for CT corresponds to 32 cm phantom.
2

Examination	Quantity and unit	DRL curve	x-value and unit	Reference
Chest radiography AP/PA	$K_{a,e}$, mGy	$y=0.036e^{0.067x}$	patient thickness, cm	STUK resolution 1, January 2006 (www.stuk.fi) Kiljunen et al., 2007
	P_{KA} , mGy cm ²	$y=3.556e^{0.132x}$		
Chest radiography LAT	$K_{a,e}$, mGy	$y=0.040e^{0.080x}$		
	P_{KA} , mGy cm ²	$y=7.469e^{0.083x}$		
Chest CT	CTDI _{VOL} , mGy	$y=0.726 e^{0.026x}$	patient weight, kg	STUK resolution 1, June 2015 (www.stuk.fi) Järvinen et. al, 2015
	DLP, mGy cm	$y=10.871e^{0.0409x}$		
Abdomen CT	CTDI _{VOL} , mGy	$y=1.314 e^{0.0282x}$		
	DLP, mGy cm	$y=38.75e^{0.0358x}$		
WB (thorax + abdomen) CT	CTDI _{VOL} , mGy	$y=1.8486 e^{0.0234x}$		
	DLP, mGy cm	$y=62.129e^{0.0373x}$		

1 **ANNEX B. DRL VALUES FOR PAEDIATRIC EXAMINATIONS AND**
2 **PROCEDURES: SUMMARY OF SELECTED DRL DATA PUBLISHED IN**
3 **EUROPEAN COUNTRIES.**

4
5 Table B1. Summary of selected DRL data from published in European countries, for paediatric
6 radiography examinations.
7

Country or region	Examination	Patient grouping	K _{a,e} mGy	P _{KA} mGy cm ²	Reference
ES (existing NDRL)	Head AP	0y		130	Ruiz-Cruces (2015) (DOPOES project)
		1-5y		230	
		6-10y		350	
		11-15y		430	
	Thorax PA	0y		40	
		1-5y		50	
		6-10y		85	
		11-15y		100	
	Abdomen AP	0y		150	
		1-5y		200	
		6-10y		225	
		11-15y		300	
	Pelvis PA	0y		60	
		1-5y		180	
		6-10y		310	
		11-15y		400	
Europe	Chest	<1 y	0.131	88	Smans et al., 2008
		1-2 y	0.240	136	
		2-3 y	0.143	189	
		3-8 y	0.228	233	
		8-12 y	0.434	395	
		>12 y	0.455		

8
9
10 Table B2. Summary of selected DRL data from published in European countries, for paediatric
11 fluoroscopy examinations.
12

Country or region	Examination	Patient grouping	P _{KA} mGy cm ²	Reference
ES (Existing NDRL)	MCU (VCUG)	0 y	500	Ruiz-Cruces (2015) (DOPOES project)
		1-5 y	750	
		6-10 y	900	
		11-15 y	1450	
Europe	VCUG	<1 y	187	Smans et al. (2008)
		2-3 y	533	
		8-12 y	1322	
		>12 y	3165	

1 Table B3. Summary of selected DRL data from selected publication in European countries, for
 2 paediatric CT examinations.
 3

Country	CT Protocol	Category	CTDI _{VOL} (mGy)	DLP (mGy cm)	Dosimetry Phantom size	Reference	
LT	Head (epilepsy)	0-9kg / 1.1y		350	16 cm	Jarvinen et al (2011)	
		9-19kg / 2.4y		500			
		>19kg / 9.6y		650			
EE, LT, FI	Chest (cancer follow up)	0-10kg		52			
		11-25kg		146			
		26-40kg		216			
		41-60kg		282			
		61-75kg		341			
>75kg (75-100)		398					
ES (Existing NDRL)	Head	0y		250	16 cm	Ruiz-Cruces (2015) (DOPOES project)	
		1-5y		340			
		6-10y		450			
		11-15y		650			
	Chest	0y		46	32 cm		
		1-5y		82			
		6-10y		125			
		11-15y		200			
	Abdomen	0y		95	32 cm		
		1-5y		150			
		6-10y		190			
		11-15y		340			
FR (existing NDRL)	Brain	10kg / 1y	30	420	16cm	Roch et al (2013)	
		20kg / 5y	40	600			
		30kg / 10y	50	900			
	Facial bones	10kg / 1y	25	200			
		20kg / 5y	25	275			
		30kg / 10y	25	300			
	Petrosal bone	10kg / 1y	45	160			
		20kg / 5y	70	280			
		30kg / 10y	85	340			
	Chest	10kg / 1y	3	30	32cm		
		20kg / 5y	4	65			
		30kg / 10y	5	140			
	Abdomen / Pelvis	10kg / 1y	4	80			
		20kg / 5y	5	120			
		30kg / 10y	7	245			
IT	Head	1-5y	30.6	504		16 cm	Granata et al (2015)
		6-10y	56.4	852			
		11-15y	58.2	985			
	Chest	1-5y	2.5	49	32 cm		
		6-10y	3.8	108			
		11-15y	6.6	195			
	Abdomen	1-5y	5.7	151	32 cm		
		6-10y	7	227			
		11-15y	14	602			

Country	CT Protocol	Category	CTDI _{VOL} (mGy)	DLP (mGy cm)	Dosimetry Phantom size	Reference
PT	Head	<1y	48	630	16 cm	Santos et al (2013)
		5y	50	770		
		10y	70	1100		
		15y	72	1120		
	Chest	<1y	2.4	45	32 cm	
		5y	5.6	140		
		10y	5.7	185		
15y		7.1	195			
UK (existing NDRL)	Chest (malignancy)	0-1y	12	200	16cm	Shrimpton et al (2006)
		5y	13	230		
		10	20	370		
UK (existing NDRL)	Head (trauma)	0-1y	25	350	16cm	Shrimpton et al (2014)
		>1-5y	40	650		
		>5-10y	60	860		

1

1 ANNEX C. REVIEW OF EXISTING PAEDIATRIC DRLS

2 C.1 Introduction

3 A follow-up questionnaire (Section C.2.1) on paediatric DRLs has been issued to 36 European
4 countries and a comprehensive literature review has been made of all published information on
5 paediatric DRLs (Section C.2.2). The information gained has been reviewed to identify the existing
6 status of paediatric DRLs with an emphasis on their application in European countries. Data from
7 this review have been used to form the basis of recommendations in Sections 6-10. The DRLs in
8 European countries which have been set by authoritative national institutions are presented and
9 discussed separately (Section C.3) from DRLs which are either new proposals or published for local
10 use only (Section C.4). The DRLs proposed internationally or published in other countries (outside
11 Europe) are also briefly summarized (Section C.5).

12 C.2 Methods of review

13 C.2.1 Questionnaire on paediatric DRLs

14 National DRLs set by an authoritative body in European countries were reviewed in 2010-11 in the
15 Dose Datamed 2 (DDM2) project (EC, 2014), including DRLs for paediatric examinations. For the
16 present Guidelines, the data on paediatric DRLs stored in the DDM2 database was verified
17 (confirmed and supplemented) by use of a questionnaire, sent to the contact persons of 36 European
18 countries according to the list of contacts established in the DDM2 project and updated for the
19 present purpose.

20
21
22 Two different approaches were adopted in the questionnaire: countries with no reported paediatric
23 DRLs were asked to verify the situation, and countries with reported paediatric DRLs were asked to
24 check and confirm the reported values. In both cases, if new paediatric DRLs had been set or if the
25 DDM2 data was no longer up-to-date, values of the new or updated DRLs were requested.
26 Furthermore, for all reported DRLs, details on how the DRLs had been established (own patient
27 dose surveys or published other data, years of data collection, sample sizes etc.) were requested,
28 because such details had not been collected in the DDM2 project.

29 C.2.2 Literature review and database

30
31 A worldwide review of literature on patient doses and DRLs for children of different age groups, or
32 other distributions and for different examinations was carried out with an emphasis on European
33 literature. Several different search engines were used: PubMed, Google Scholar and Science Direct,
34 using various terms to locate pertinent articles.

35
36 For the output of this review, a database of literature was created, classified in suitable headings,
37 using the Mendeley (www.mendeley.com) platform. The articles selected included studies on DRLs
38 in general but also in dose optimisation. Subgroups were created to help facilitate the process of the
39 literature review. The resulting database contains 215 articles [*until 25 Feb 2015*].

40
41 To evaluate the data found in the literature, the information was further grouped to help identify the
42 advantages and/or limitations of each study and to more easily draw conclusions on the
43 methodology used in the DRL determinations.

44

1 For articles reporting on DRLs in the European countries, the correspondence of this data with the
2 results of the questionnaire (Section C.3) was checked and the information from the two sources
3 combined.
4

5 **C.3 National DRLs for paediatric exams set in the European countries**

6 The summary of the national DRLs for paediatric exams set by an authoritative body in the
7 European countries is shown in Table C.1 (the same as Table 5.1), and the detailed data of the
8 DRLs are given in Annex A. National paediatric DRLs are provided for some groups of
9 examinations (radiography, fluoroscopy or CT) in 17 countries, i.e. in 47 % of the European
10 countries. In Lithuania and Belgium, the DRLs had been set very recently and had not been
11 included in the DDM2 database.
12

13 In 9 countries (AT, BE, DE, DK, ES, FI, LT, NL and UK) all available national DRLs are based on
14 own patient dose surveys covering several radiology institutions. In 6 countries (CY, LU, PL, RO,
15 CH, IT), the available national DRLs are adopted from published values; in 5 countries (CY, LU,
16 PL, RO, IT) from the EC guidance (EC, 1999) and in Switzerland from published values in another
17 country (DE). In Ireland, DRLs are based on own survey only for some radiography and CT
18 examinations, other values are adopted from the UK. In France, the national DRLs are based on
19 collected data, protocol data or adopted from literature.
20

1 Table C.1. Summary of existing national DRLs in European countries, set or accepted by an
 2 authoritative body, based on the results of the questionnaire and the literature review. Coloured
 3 cells: data accepted for EDRL calculation.
 4

Country	Source of DRL values	Radiography		Fluoroscopy	CT		References
		K _{a,e} (ESD, ESAK), K _{a,i} (IAK)	P _{Ka} (KAP, DAP)	P _{Ka} (KAP, DAP)	DLP (P _{KL})	CTDI _{vol} (C _{vol})	
AT	Own survey		Skull (AP/ PA, LAT) Thorax (AP/PA) Abdomen (AP/PA)	MCU	Brain Chest		Questionnaire (all). Billiger et al. 2010 (radiography)
BE	Own survey		Thorax (PA, PA+LAT) Abdomen		Brain Sinus Thorax Abdomen	Brain Sinus Thorax Abdomen	www.fanc.fgov.be
DE	Own survey		Head (AP, PA, LAT) Thorax (AP, PA, LAT) Abdomen (AP) Pelvis	MCU	Head Facial bones Thorax Abdomen	Head Facial bones Thorax Abdomen	Questionnaire. Bundesamt fur Strahlenschutz, 2010.
DK	Own survey	Thorax (AP, PA, LAT) Pelvis (AP) Overview of abdomen		MCU			Questionnaire.
ES	Own survey		Head (AP) Thorax (PA) Abdomen (AP) Pelvis (PA)	MCU	Head Chest Abdomen		Ruiz-Cruces, 2015
FI	Own survey	Sinuses (Waters projection) (discrete values) Thorax (AP, PA, LAT) (DRL-curve)	Sinuses (Waters projection) (discrete values) Thorax (AP, PA, LAT) (DRL-curve)	MCU	Head (discrete values) Thorax, abdomen (abd. + pelvis), WB (chest+abd. +pelvis) (DRL-curve)	Head (discrete values) Thorax, abdomen (abd. + pelvis), WB (chest+abd. +pelvis) (DRL-curve)	Questionnaire. Kiljunen et al., 2007. Järvinen et al. 2015.
LT	Own survey	Chest (PA) Skull (AP/PA, LAT) Abdomen	Chest (PA) Skull (AP/PA, LAT) Abdomen		Head		Questionnaire.
NL	Own survey		Thorax (AP, PA) Abdomen (AP)	MCU	Head	Head	Questionnaire.
UK	Own survey			MCU Barium meal Barium swallow	Head Chest	Head Chest	Hart et al. 2012 (F). Shrimpton et al., 2006, 2014 (CT).
IE	Own survey for some radiography and CT examinations. Other values adopted from other countries.	Skull (AP, LAT) Chest (AP/PA) Abdomen (AP) Pelvis (AP)		MCU Barium meal Barium swallow	Brain Abdomen/Pelvis		Questionnaire. Medical council, 2004. HSE Medical Exposures Radiation Unit, 2013.
FR	Own survey for radiography, CT data based on protocol data or literature	Thorax (AP, LAT) Pelvis	Thorax (AP, PA, LAT) Abdomen (AP) Pelvis		Brain Facial Bone Petrous Bone Chest Abdomen+Pelvis	Brain Facial Bone Petrous Bone Chest Abdomen+Pelvis	Questionnaire. Roch et al., 2012.
CY	Adopted (EC)	Head (AP, PA, LAT) Thorax (AP, PA, LAT) Abdomen Pelvis (AP)					Questionnaire.
IT	Adopted (EC)	"					Questionnaire
LU	Adopted (EC)	"					Questionnaire.
PL	Adopted (EC)	"					Questionnaire.
RO	Adopted (EC)	"					Questionnaire.
CH	Adopted (DE)				Brain Face, nasal cavity Thorax Abdomen Lumbar spine	Brain Face, nasal cavity	Questionnaire.. Galanski and Nagel, 2005

5
6

1 C.3.1 Radiography

2 In 9 countries (AT, BE, DE, DK, ES, FI, FR, LT and NL; see Table C.1), the paediatric DRLs for
 3 radiography are based on own national patient dose survey covering several radiology institutions.
 4 In France, the DRLs for radiography are based on both collected data and literature data. In 5
 5 countries (CY, LU, PL, RO, IT) the paediatric DRLs for radiography had been adopted from the EC
 6 guidelines (EC, 1999). In Ireland national DRLs for radiography are based on own survey for some
 7 radiography examinations, other values are adopted from the UK.

8
 9 In Tables C.2 and C.3 details of DRLs, for both radiography and fluoroscopy (see Section C.3.2),
 10 are given for those countries, which have their DRLs based on own national patient dose surveys.
 11 All these DRLs correspond to complete routine CT examination (one scan series). When comparing
 12 NDRLs it is important to ensure that the DRLs correspond to one scan series and not to a complete
 13 procedure of all series (multi-phase examinations)-

14
 15 Table C.2. Patient dose survey and setting of the national paediatric DRLs in European countries for
 16 radiography (R) and fluoroscopy (F): organisational and practical details.
 17

Country	Years of data collection	Organizer of dose survey	Organization to set the DRL	Professional societies/ clinical experts consulted	Number of institutions/ installations/ patients; coverage of total (%)	Practical method, limitations, comments	User guidance given (recommended sample size, frequency of comparison with DRLs)	References
AT	2006-2007	Center for Biomedical Engineering and Physics, Medical			14 hospitals/ 25 installations/ 41-1187 patients	Standard forms for data collection, data sending by mail.		Billiger et al. 2010
BE		Federal Agency of Nuclear Control (FANC)	Federal Agency of Nuclear Control (FANC)					www.fanc.fgov.be
DE	2006-2009		Bundesamt für Strahlenschutz	Yes	All German institutions (100 %)			Questionnaire
DK	2004-2005		NIRP		4-5 (about 10 % (R))		Yes (10 patients, 2 years) (R) Yes (10 patients, 1 year) (F)	Questionnaire. Report in NIRP website.
ES	2011-2013	DOPOES project	Ministry of Health		5-10 % of paediatric institutions			Ruiz-Cruces, 2015
FI	2004-2005	STUK	STUK	Yes	8-20 (3-6 %) (R) 11 (about 50 %) (F)	Both grid and non-grid techniques (R)	Yes (10 patients, 3 years)	Questionnaire. Kijunen et al. 2007. STUK Resolution 1Jan 2006 (www.stuk.fi)
LT	2009-2012	Radiation Protection Centre of Lithuania	Ministry of Health of the Republic of Lithuania		5 institutions/ 260-1474 patients		(at least 10 patients, 5 years)	Questionnaire
NL		The Netherlands Commission on Radiation Dosimetry	The Netherlands Commission on Radiation Dosimetry	Yes (Commission members include representatives of professional societies)	Restricted survey			Questionnaire
UK	2010	Health Protection Agency	Health Protection Agency		12-61 rooms	DAP for children of known size adjusted to the values for the nearest standard size.		Hart et al. 2012 (F).
FR	2004-2008	Nuclear Safety and Radiation Protection French Institute (IRSN)	Ministry of Health and ASN					Roch and Aubert, 2012

1 Table C.3. Patient dose survey and setting of the national paediatric DRLs in European countries for
 2 radiography (R) and fluoroscopy (F): technical details.

Country	DRL quantities*	Source/verification of dosimetric value	Patient grouping	DRL method: Percentile of dose distribution	Reference
AT	$K_{a,e}$, $K_{a,i}$, P_{KA}	Local audits to ensure correct values: Dose output measurements and in situ calibration of P_{KA} meters. Conversion of $K_{a,i}$ to $K_{a,e}$ by mean of backscatter factor.	Age: 0, 1, 5, 10, 15 y (R) 0, 1, 5, 10 y (F)	75 %	Questionnaire. Billiger et al. 2010
BE	P_{KA}		Age: <1 y, 1-<5 y, 5-<10 y, 10-<15 y	75 %	www.fanc.fgov.be
DE	P_{KA}		Weight: 1000 g, 3000 g (R), 3000 g (F) (premature babies and newborns) Age: 10±2mo, 5±2y, 10±2y (R,F)		Questionnaire
DK	$K_{a,e}$, P_{KA}	Calculated based on exposure parameters, calibration 2005 (R) for P_{KA} meters, calibration unknown (F)	Age: 5 y (= thickness 14,7 cm) (thorax, pelvis) < 1 y (overview of abdomen) <1, 1-5 y (MCU)	75 %	Questionnaire
ES	P_{KA}		Age: 0, 1-5, 6-10, 11-15 y	75 %	Ruez-Cruices, 2015
FI	$K_{a,e}$, P_{KA}	$K_{a,e}$ calculated from both P_{KA} and x-ray tube output (R). Calibrated P_{KA} meters (R, F)	DRL-curve as a function of patient thickness (thorax) One age group 7-15 y (Sinuses tilted projection) Age groups < 1 y, 1-5 y (MCU)	75 %	Questionnaire. Kijunen et al. 2007. STUK Resolution 1Jan 2006 (www.stuk.fi)
LT	$K_{a,e}$, P_{KA}	$K_{a,e}$ calculated from x-ray tube output (R). Calibration of P_{KA} meters checked (R, F)	Age: 1, 5, 10, 15 y (R)	75 %	Questionnaire
NL	P_{KA}		Weight/age groups: 4 kg/ 0 y, 11 kg/ 1 y, 21 kg/ 5 y	Expert judgement guided by the results of a restricted dose survey	Questionnaire
UK	P_{KA}		Age: 0, 1, 5, 10, 15 y		Hart et al. 2012 (F).
FR	$K_{a,e}$, P_{KA}		Weight: 3.5, 10, 20, 30 kg, Age: 0, 1, 5, 10 y	75 %	Roch and Aubert, 2012

4
5
6 All the DRLs are specified on the basis of the anatomical region imaged. The most common
7 radiography examinations are:

- 8 • Skull (head) AP, PA and LAT (in 4 countries with own patient dose survey)
- 9 • Chest (thorax) AP, PA, LAT (in 9 countries with own patient dose survey)
- 10 • Abdomen AP/PA (in 7 countries with own patient dose survey)
- 11 • Pelvis AP (in 6 countries with own patient dose survey)

1 These are the same groups of examinations that had been earlier recommended by the European
2 Commission (EC, 1999). Consequently, DRLs for these groups have been set in the 5 countries
3 adopting the DRL values from the EC.
4

5 Most of the DRLs (in 8 of the 9 countries having their own patient dose surveys) are given in terms
6 of dose-area product (P_{KA}). Entrance-surface air kerma ($K_{a,e}$) has also been used in 4 of these
7 countries, and solely in one country (see Table C.3). $K_{a,e}$ has been calculated from the x-ray tube
8 output values and the examination parameters and in one case also from the P_{KA} values. P_{KA} values
9 have been obtained from P_{KA} meters; in four countries it has been reported that the P_{KA} meter
10 calibration has been checked in connection with the data collection. In the other countries (having
11 only adopted values) only the $K_{a,e}$ has been used, in accordance with the EC recommendations (EC,
12 1999).
13

14 In 7 out of 9 countries it was noted that DRLs were estimated using the traditional approach, i.e.
15 using the 3rd quartile or 75 % point of the dose distribution, In the Netherlands, the setting of DRLs
16 was based on expert judgement guided by the results of a restricted dose survey; a metric called
17 “achievable dose level” has been given together with the DRL. The earlier recommendation by the
18 EC (EC, 1999) was based on the 3rd quartile approach.
19

20 For patient groupings in the 9 countries with their own patient dose surveys, age alone has been
21 used in 6 countries, both age and weight in three countries and patient thickness in one country
22 (Table C.3). In Germany, for premature babies and newborns, two weight groups (1000 g and 3000
23 g) have been defined while age groups with limits have been defined for older children (10 ± 2
24 months, 5 ± 2 y and 10 ± 2 y). The most common age groups are 0, 1, 5, 10 and 15 years; the whole
25 set (0-15) in two countries and 1-15 years in one country. In the other countries, slightly different
26 sets of groups exist, but one or more of the ages 0, 1, 5 and 10 years appear in these groupings. In
27 the Netherlands, with both age and weight groups specified, the equivalence of weight and age are
28 defined as: 4 kg – 0 y, 11 kg – 1 y and 21 kg – 5 y. In the UK, P_{KA} values for children with known
29 sizes (ages) were adjusted for the values of the nearest standard size (age). In France, several age
30 and weight groups have been defined, with their equivalence being close to that used in the
31 Netherlands, i.e. 3,5 kg – newborn, 10 kg – 1y, 20 kg – 5 y and 30 kg – 10y.
32

33 One study deserves specific attention, especially when there is limited data for statistical analysis.
34 According to the study of Kiljunen et al (2007), a DRL curve produced using $K_{a,e}$ and P_{KA} as a
35 function of patient projection thickness could be a practical method for determining a DRL. The
36 study was limited to chest examinations but could be potentially applied to other types of
37 examinations as well.
38

39 The majority of patient dose surveys were carried out during 2004-2009, while the most recent ones
40 (three countries) are from 2010-2013. The organiser of the patient dose survey was reported to be
41 an authority in 5 countries, and in most countries the DRLs were set by an authority (radiation
42 protection or health authority). Professional societies or clinical experts were consulted in at least
43 two countries. In one case (NL), the DRLs have been set by a national committee, which consists of
44 members of several professional organisations.
45

46 The number of institutions surveyed in different countries ranged from a few to all of their imaging
47 institutions, 5% – 100 %, with the total number of patients ranging from less than 100 to more than
48 1000. No automatic data collection and management has been reported. User guidance for the
49 comparison of local patient doses with the national DRLs has been issued in three countries,

1 requesting a minimum of 10 patients for each age group, or 10 patients in total in the case of the
2 DRL curve approach, and the comparison frequency ranged from 2 to 5 years.

3
4 In one national study (Kiljunen et al., 2007), attention was paid to the use of anti-scatter grids and
5 additional filtration in paediatric examinations which should be taken into account for the
6 calculation of DRLs as they influence the patients' dose. The national DRLs in this study were
7 provided for common grid and non-grid techniques because the use of removable grid techniques in
8 paediatric examinations was not always possible.

9
10 In conclusion, there seems to be reasonable agreement on the radiography examinations for which
11 DRLs have been needed (skull, chest, abdomen, pelvis) and on the quantities used (P_{KA} and/or $K_{a,e}$).
12 All the current national DRLs seem to be based on the 3rd quartile method. For patient grouping, a
13 set of age groups up to 15y of age (0, 1, 5, 10, 15 y) seems to be the practice while in one country, a
14 DRL curve with patient thickness as the parameter has been proposed to overcome the problems of
15 poor statistics with discrete groups. All current DRLs have been set by authorities, based on patient
16 dose data collected about 5-10 years ago. There is a large variation between countries on the
17 number of institutions and patients included in the patient dose surveys. For user guidelines,
18 consistent systems exist (minimum of 10 patients in each group, data collection frequency 2-5
19 years). It is evident that a rough consensus on the examinations for the DRLs and the DRL
20 parameters (quantities, percentile of dose distribution, patient grouping) already exists or is close to
21 being achieved. However, better standardisation and guidelines are needed, in particular for the
22 patient dose surveys as the basis of setting the DRLs.

23 24 **C.3.2 Fluoroscopy**

25 In 7 countries, the paediatric DRLs for fluoroscopy examinations are based on own national patient
26 dose survey covering several radiology institutions (AT, DE, DK, ES, FI, NL and UK) (Table C.1).
27 In Ireland (IE), the DRL was adopted from UK data (Hart et al. 2002).

28
29 In Tables C.2 and C.3 details of DRLs are given for the countries, that have their DRLs based on
30 own national patient dose surveys.

31
32 The current national DRLs in European countries are given only for micturating cystourethrography
33 (MCU), except in the UK and Ireland, where DRLs have been set also for barium swallow and
34 barium meal.

35
36 All the DRLs for fluoroscopy are given in terms of P_{KA} . P_{KA} values have been obtained from P_{KA}
37 meters; in four countries it has been reported that the P_{KA} meter calibration had been checked in
38 connection with the data collection.

39
40 In 4 out of 6 countries the DRLs were estimated using the traditional approach, i.e. using the 3rd
41 quartile or 75 % point of the dose distribution. In the Netherlands, the setting of DRLs was based on
42 expert judgement guided by the results of a restricted dose survey; a metric called "achievable dose
43 level" has been given together with the DRL.

44
45 For patient grouping in the 7 countries with own patient dose surveys, age has been used in 6
46 countries, and both age and weight in one country (Table C.3). In Germany, a weight group (3000
47 g) has been defined for newborns, while age groups with limits have been defined for older children
48 (10 ± 2 months, 5 ± 2 y and 10 ± 2 y). Age groups 0, 1, 5, 10 years have been used in 2 countries, with
49 an additional 15 years used in one of these countries. In two countries, only two age groups have

1 been defined: < 1 y and 1-5 y. In one country (NL) both age and weight groups are used, the
2 equivalence of weight and age are defined as: 4 kg – 0 y, 11 kg – 1 y and 21 kg – 5 y (the same as
3 for radiography examinations). In the UK, P_{KA} values for children with known sizes (ages) were
4 adjusted for the values of the nearest standard size (age): the adjustment was based on the
5 relationship between the thickness of the body part being x-rayed in the patient and the
6 corresponding thickness in the nearest standard-sized child. This could either be measured directly
7 or if more convenient, could be calculated from the height and weight of the patient (Hart et al.,
8 2000).

9
10 The majority of patient dose surveys for fluoroscopy were carried out during 2004-2009, while the
11 most recent ones are from 2010 (in UK) and 2013 (ES). The organiser of the patient dose survey
12 was reported to be an authority (radiation protection or health) in 2 countries, and in most countries
13 the DRLs were set by an authority. Professional societies or clinical experts were consulted in at
14 least in two countries. In one case (NL), the DRLs have been set by a national committee, which
15 consists of members of several professional organisations. The institutions involved in the patient
16 dose surveys ranged from around half to all in the country. User guidance for the comparison of
17 local patient doses with the national DRLs has been issued in two countries, requesting a minimum
18 of 10 patients for each age group and the comparison frequency of 1 or 3 years.

19
20 In conclusion, there seems to be reasonable agreement on the fluoroscopy examinations for which
21 DRLs have been needed (mainly MCU) and on the quantities used (P_{KA}). All the current national
22 DRLs seem to be based on the 3rd quartile method. For patient grouping, a set of age groups up to
23 15y of age (0, 1, 5, 10, 15 y) have been identified although in some cases only children up to 5y of
24 age (< 1 y and 1-5 y) have been considered. All current DRLs have been set by authorities, based on
25 patient dose data for children of about 5-10 years old. For user guidelines, consistent systems exist
26 (minimum of 10 patients for comparison in each group, comparison frequency 1 or 3 years). It is
27 evident that a rough consensus on the examinations for the DRLs and the DRL parameters
28 (quantities, percentile of dose distribution, patient grouping) already exists or is closely achievable.
29 However, better standardisation and guidelines are needed, in particular for the patient dose surveys
30 as the basis of setting the DRLs.

31 32 **C.3.3 Computed tomography**

33 In 9 countries (AT, BE, DE, ES, FI, IE, LT, NL and UK), the paediatric DRLs for CT examinations
34 are based on own national patient dose survey covering several radiology institutions (see Table
35 C.1). In Ireland, the DRLs are based on a combination of local survey (HSE Medical Exposures
36 Radiation Unit, 2013) and on the initial European values (Shrimpton and Wall, 2000). In France,
37 the DRLs are not based on collection of individual patient doses but on typical dose values for
38 given imaging protocols, or on published other data. In Switzerland, the existing DRLs have been
39 adopted from old German DRLs (Galanski and Nagel, 2005), while a proposal on new national
40 DRLs has been published (Verdun et al. 2008). In Portugal and Italy, proposals on national DRLs
41 have been published (Santos et al. 2013, Granata et al. 2015) although this has not yet been
42 accepted by an authoritative body.

43
44 In Tables C.4 and C.5 details of DRLs are given for those countries that have their DRLs based on
45 own national patient dose surveys. When comparing NDRLs it is important to ensure that the DRLs
46 correspond to a complete routine CT examination (one scan series) and not to a complete procedure
47 of all series (multi-phase examinations)-
48

1 Table C.4. Patient dose survey and setting of the national paediatric DRLs in European countries for
 2 computed tomography: organisational and practical details
 3

Country	Years of data collection	Organizer of dose survey	Organization to set the DRL	Professional societies/ clinical experts consulted	Number of institutions/ installations/ patients; coverage of total (%)	Practical method, limitations, comments	User guidance given (recommended sample size, frequency of comparison with DRLs)	References
AT	No details reported							
BE	2012	Federal Agency of Nuclear Control (FANC)	Federal Agency of Nuclear Control (FANC)	No			Website	Questionnaire. www.fanc.fgov.be
DE	2005-2006	Medizinische Hochschule Hannover	Bundesamt für Strahlenschutz	Yes	656 institutions, incl. 72 devoted paediatric institutions, 6-1634 patients			Questionnaire
DK	No DRLs for CT							
ES	2011-2013	DOPOES project	Ministry of Health		5-10 % of paediatric institutions			Ruiz-Cruces, 2015
FI	2011-2013	STUK	STUK	Yes	4 institutions (about 30 %)/ 1049 patients	Indication based	Yes	Questionnaire Järvinen et al. 2015
IE	2009		HSE Medical Exposures Radiation Unit, 2013.	Yes	27 institutions (about 20 %), 3200 patients.			Medical council, 2004. HSE Medical Exposures Radiation Unit, 2013.
LT	2009-2012	Radiation Protection Centre of Lithuania	Ministry of Health of the Republic of Lithuania		3 institutions/ 51-234 patients		(at least 10 patients, 5 years)	Questionnaire
NL	No details reported	The Netherlands Commission on Radiation Dosimetry	The Netherlands Commission on Radiation Dosimetry	Yes (Commission members include representatives of professional societies)	Restricted survey			Questionnaire
UK	2003	Health Protection Agency (HPA)	Department of Health (Public Health England)	Yes	118 hospitals/ 126 scanners; about 25 % of total	Scan protocols + scan sequence data for min. 10 patients		Shrimpton et al., 2006, 2014

4
5

1 Table C.5. Patient dose survey and setting of the national paediatric DRLs in European countries for
 2 computed tomography: technical details

Country	DRL quantities	Source/verification of dosimetric value	Patient grouping	DRL method: Percentile of dose distribution	Reference
AT	DLP		Age: 0, 1, 5, 10, 15 y		Questionnaire
BE	DLP, CTDI _{VOL}	Federal Agency of Nuclear Control (FANC)	Age: <1 y, 1-<5 y, 5-<10 y, 10-<15 y	75 %	Questionnaire. www.fanc.fgov.be
DE	DLP, CTDI _{VOL}		Age: Newborn, < 1 y, 2-5 y, 6-10 y, 11-15 y, > 15 y		Questionnaire
DK					
ES	DLP		Age: 0, 1-5, 6-10, 11-15 y	75 %	Ruez-Cruices, 2015
FI	DLP, CTDI _{VOL}	Calibration of CT console values checked	DRL-curve as a function of patient weight (chest, abdomen, trunk) Ages: <1, 1-5, 5-10, 10-15 (head, routine); all ages (head, ventricular size)	75%, 50 %	Questionnaire Järvinen et al. 2015
IE	DLP		Age: Newborn, 1-4 y, 5-9 y, 10-15 y	75 %	Medical council, 2004. HSE Medical Exposures Radiation Unit, 2013.
LT	DLP	Calibration of CT console values checked	Age: 1, 5, 10, 15 y	75 %	Questionnaire
NL	DLP, CTDI _{VOL}		Weight/age groups: 4 kg/ 0 y, 11 kg/ 1 y, 21 kg/ 5 y, 36 kg/10y	Expert judgement guided by the results of a restricted dose survey	Questionnaire
UK	DLP, CTDI _{VOL}	Calculations based on protocol and sequence data	Age: 0-1 y, 5 y, 10 y	75 %	Shrimpton et al., 2006, 2014.

4
5
6 At present the DRLs are specified mainly on the basis of the anatomical region imaged. DRLs for
 7 CT head (brain) have been set in all 9 countries that have national DRLs for CT examinations, for
 8 both CT chest (thorax) and CT abdomen in 5 countries, and for either CT chest or CT
 9 abdomen/pelvis in 2 countries. In Germany, DRLs for CT facial bones have also been set. In UK,
 10 the DRLs for CT are based on anatomical region and clinical indication, e.g. paediatric head
 11 (trauma) (Shrimpton et al., 2014). The new DRLs for CT examinations in Finland (Järvinen et al.,
 12 2015) are based on clinical indications, while in the case of examinations of the thorax, abdomen
 13 and trunk (=thorax+abdomen) the DRLs are the same for all indications studied, and in case of
 14 head, the DRLs have been given for two indications (routine head and ventricular size).

15
16 In 4 of the 9 countries, DRLs are given in terms of both air kerma-length product (DLP) and
 17 volume computed tomography dose index (CTDI_{VOL}) (Table C.5). DRLs have been set in terms of
 18 DLP alone in four countries and in terms of CTDI_{VOL} alone in one country. In two countries it has
 19 been reported that the calibration of the CT scanner console values have been checked in
 20 connection with the data collection.

21
22 In 5 out of 8 countries the DRLs were estimated using the traditional approach, i.e. using the 3rd
 23 quartile or 75 % point of the dose distribution. In the Netherlands, the setting of DRLs was based on
 24 expert judgement guided by the results of a restricted dose survey; an “achievable dose level” has

1 been given together with the DRL. In Finland, in addition to the use of the 75 % DRL curve, a 50 %
2 level curve is provided as supplementary information to enable varying levels of technology to be
3 taken into account (Järvinen et al., 2014) (the 75 % DRL curve was obtained by making an
4 exponential fitting to the points above the 50 % level curve).

5
6 For patient groupings, in 6 of the 8 countries with own patient dose surveys (DE, ES, FI, IE, LT,
7 UK), age has been used, in one country both age and weight has been used (NL), and in one country
8 patient weight for body CT and age for head CT (Table C.5) has been used (FI). Similar sets of age
9 groups, 1, 5, 10 and 15 years have been used by 5 countries and additionally 0 years have been used
10 in one country (AT) and 0-1 years in one country (UK). In some countries (DE, ES, FI, IE) the age
11 groups are defined by ranges, e.g. newborn, < 1y, 2-5, 6-10 y, 11-15 y and >15y (DE). In one
12 country with both age and weight groups (NL), the equivalence of weight and age are defined as: 4
13 kg – 0 y, 11 kg – 1 y, 21 kg – 5 y and 36 kg – 10 y (similarly with radiography). In Finland, the
14 dosimetric quantities (DLP and CTDI_{VOL}) are presented as a function of patient weight (the DRL
15 curve approach) which has been considered to be a better parameter than age (Järvinen et al., 2014).

16
17 In four countries (ES, FI, IE, LT) the patient dose surveys for CT examinations is quite recent and
18 were carried out during 2009-2013, while in the other cases surveys were carried out during 2003-
19 2006. The organiser of the patient dose survey was reported to be an authority (radiation protection
20 or health) in 3 countries, and in most countries the DRLs were set by an authority. Professional
21 societies or clinical experts were consulted at least in two countries. In one case (NL), the DRLs
22 have been set by a national committee, which consists of members of several professional
23 organisations. The patient dose surveys ranged from a few to hundreds of institutions, with the
24 number of patients ranging from less than 100 to more than 1000. User guidance for comparison of
25 local patient doses with the national DRLs has been issued in two countries, requesting a minimum
26 of 10 patients for each age group, or 10 patients in total in case of the DRL curve approach, and the
27 comparison frequency of 3 or 5 years.

28
29 In conclusion, there seems to be reasonable agreement on the CT examinations for which DRLs
30 have been needed (head, chest, abdomen) and on the quantities used (DLP and CTDI_{VOL}). All the
31 current national DRLs seem to be based on the 3rd quartile method, while in one case a 50% level is
32 planned to be given as supplementary information. For patient grouping, a set of age groups (e.g. 0,
33 1, 5, 10, 15 y) seems to be the practice while in one country, a DRL curve with patient weight as the
34 parameter has been proposed to overcome the problems of poor statistics with discrete groups. All
35 current DRLs have been set by authorities, based in part on recent patient dose data, about 2-5 years
36 old, and partly on data that is more than 10 years old. For user guidelines, the reported systems are
37 similar to that of radiography (minimum of 10 patients for comparison in each group or per DRL
38 curve, comparison frequency 3 or 5 years). It is evident that a rough consensus on the examinations
39 for the DRLs and the DRL parameters (quantities, percentile of dose distribution, patient grouping)
40 already exist or is closely achievable. However, better standardisation and guidelines are needed, in
41 particular for the patient dose surveys as the basis of setting the DRLs. A consensus in the definition
42 of DLP (one series or all series) is also needed.

43 44 **C.3.4 Interventional radiology**

45 No national paediatric DRLs have been set for IR procedures in any European country.

46 47 **C.4 Studies on paediatric DRLs in European countries**

48 Besides the national DRLs set by authoritative bodies for paediatric examinations and procedures
49 (Section C.3.), several studies have been published in European countries, to propose national

1 DRLs or to develop practice or local DRLs for paediatric examinations, or to compare patient dose
2 distributions between several countries. These articles are summarized in the following sections,
3 with a note on those studies which have already led to the establishment of national DRLs by
4 authoritative bodies.

5 6 **C.4.1 Radiography**

7 The summary of the literature survey for DRLs in paediatric radiography in European countries is
8 compiled in Table C.6. The actual values of NDRLs are shown in Annex A and for *selected* other
9 DRLs in Annex B.

10
11 Nine European publications plus one personal communication (Ruiz-Cruces, 2015) were identified
12 which reported dose values for paediatric radiography examinations, six of which were based on
13 data collected from single countries/regions (Billiger et al., 2010; Kiljunen et al., 2007; Roch et al.
14 2012; Ireland Medical council, 2004; Montgomery et al., 2000, Ruiz-Cruces, 2015) and three
15 dealing with European wide establishment for DRLs (Schneider et al., 1998; Hart, 1996; Smans et
16 al., 2008). Five of these publications have already resulted in national DRLs (Billiger et al., 2010 -
17 AT; Kiljunen et al., 2007- FI; Roch et al. 2012- FR, Ireland Medical council, 2004-IE, Ruiz-Cruces,
18 2015-ES) and have been included in the discussion in Section 5.3.1. Dabin et al (Dabin et al. 2013)
19 published data on a national survey with proposal of NDRL for chest X-ray and combined chest-
20 abdomen X-ray in neonatology.

21
22 In one paper (Montgomery et al., 2000) the aim was to investigate if the use of a single value as a
23 DRL for all ages (DRL for 5-year old child) is appropriate or if age group classification is needed.
24 $K_{a,e}$ values, for only non-grid examinations, were collected for chest, abdomen and pelvis
25 examinations from three hospitals. The relationship between age, weight and calculated EPD
26 (equivalent patient diameter) was discussed and weight was found to be as reliable a factor as EPD,
27 and better than age. Adjustment factors have been defined for doses to be compared to a standard 5
28 years old child. The main limitation of the results is that examinations with a grid, which generally
29 leads to a higher patient dose, have not been considered.

30
31 From the three European wide studies, Schneider et al. (1998) re-analysed the data from four
32 European surveys for chest X-rays examinations, which had formed the basis for the DRLs
33 proposed by the European Guidelines (EC, 1996). They re-grouped the data according to the
34 patient's age and in addition sorted the data into the "optimised" and "un-optimised" techniques
35 proposing that the data from an optimised technique could be considered as a DRL. The study had
36 several limitations (differences in the use of grid, differences in focus-to-film distance/focus-to-
37 detector distance) and the results are dated. Hart (1996) also re-analysed the data from the survey
38 presented in the European guidelines (EC, 1996). The purpose of this study was to normalize the
39 doses to those of the nearest standard-sized patient and define new DRLs for each group. A new
40 method was suggested for the estimation of the patient thickness according to the patient height and
41 weight. The main limitation of this study was that there were not enough data for children older
42 than 5 years old, and the results are also dated. Smans et al. (2008) collected patient dose data for 6
43 age groups (<1, 1-2, 2-3, 3-8, 8-12, >12y) from 11 EU Member States: $K_{a,e}$ and/or P_{KA} for chest (12
44 centres), abdomen (4 centres) and pelvis (5 centres) radiography. The main limitation with the study
45 was the relative small number of centres included.

1 Table C.6. Published studies on paediatric DRLs for radiography in European countries.
2

Reference	Region	Data source	Exams	Patient groupin g	Dose value	No. patients	No. centres	NDRLs proposed
Billiger et al., 2010	AT	Patients	Skull, thorax, abdomen	0y, 1y, 5y, 10y, 15y	3 rd quartile $K_{a,e}$, $K_{a,i}$, P_{KA}	41-1187	14	YES (existing NDRL, see C.3.1)
Dabin et al, 2013	BE	Patients	Chest PA and combined chest-abdomen in neonatology	<1000 g,, 1000 g<. . .<2000 g, , >2000 g,	3 rd quartile $K_{a,e}$	721	17	YES
Rafael Ruiz-Cruces, 2015 (DOPOES-project)	ES	Patients	Head AP, thorax PA, abdomen AP, pelvis PA	0y, 1-5y, 6-10y, 11-15y	3 rd quartile P_{KA}	135-1025	5-10 % of total	YES (existing NDRL, see C.3.1)
Kiljunen et al., 2007	FI	Patients	Thorax, sinuses waters	7-15 y DRL – curve for thorax	3 rd quartile values $K_{a,e}$, P_{KA}	N/a	8-20	YES (existing NDRL, see C.3.1)
Roch et al., 2012	FR	A mixture of patient data, EC guidelines, literature and PCXMC calculations	Thorax, abdomen, pelvis	Newborn 1y, 5y, 10y / 3,5 kg, 10 kg, 20 kg, 30 kg	3 rd quartile $K_{a,e}$, P_{KA}			YES (existing NDRL, see C.3.1)
HSE Medical Exposures Radiation Unit, 2013	IE	Patients	Chest, abdomen, pelvis, skull	0y, 1y, 5y, 10y, 15y	3 rd quartile $K_{a,e}$		1	YES (existing NDRL, see C.3.1)
Montgomery et al., 2000	UK	Patients	Chest, abdomen, pelvis	5y	3 rd quartile $K_{a,e}$		3	No
Schneider et al., 1998	Europe	Patients	Chest	5 y, 10 y	3 rd quartile $K_{a,e}$		12	No
Hart, 1996	Europe	Patients	Chest, abdomen, pelvis, skull	1y, 5y, 10y, 15y	3 rd quartile $K_{a,e}$		12	No
Smans et al., 2008	Europe	Patients	Chest, abdomen, pelvis	<1, 1-2, 2-3, 3-8, 8-12, >12y	3 rd quartile $K_{a,e}$		12	No

3
4 As a conclusion, except for the few studies for national DRLs, the other published studies, including
5 the European wide studies, are either dated or limited to a few centres so that they do not provide
6 high quality input to the setting of European paediatric DRLs.
7

1 **C.4.2 Fluoroscopy**

2 The summary of the literature survey for DRLs in paediatric conventional fluoroscopy in European
 3 countries is compiled in Table C.7. The actual values of NDRLs are shown in Annex A and for
 4 *selected* other DRLs in Annex B.

5
 6 Four European publications plus one personal communication (Ruiz-Cruces, 2015) were identified
 7 which reported dose values for paediatric fluoroscopy examinations, four of which were based on
 8 data collected from single countries/regions (Hart et al., 2012; Hiorns et al. 2014; Yakoumakis et
 9 al., 2014, Ruiz-Cruces, 2015) and one considers a European wide establishment for DRLs (Smans
 10 et al., 2008). Two of these publications has resulted in a national DRL (Hart et al., 2012 –UK, Ruiz-
 11 Cruces, 2015 - ES) and has been included in the discussion in Section C.3.2.

12
 13 Table C.7. Published studies on paediatric DRLs for fluoroscopy in European countries.

14

Reference	Region	Data source	Exams	Patient groupin g	Dose value	No. patients	No. centres	NDRLs proposed
Rafael Ruiz-Cruces, 2015 (DOPOES-project)	ES	Patients	MCU	0y, 1-5y, 6-10y, 11-15y	3rd quartile P _{KA}	200-1050	5-10 % of total	YES (existing NDRL, see C.3.2)
Hart et al., 2012	UK	Patients	MCU (MCUG), barium meal, barium swallow	0y, 1y, 5y, 10y, 15y	3 rd quartile P _{KA}	335-2020		YES (existing NDRL, see C.3.2)
Hiorns et al., 2014	UK	Patients	MCU (MCUG) + 7 other exams	0y, 1y, 5y, 10y, 15y	3 rd quartile P _{KA}		1	No
Smans et al., 2008	Europe	Patients	Lower GI tract, upper GI tract, voiding cystourethro-gram (VCUG)	<1y, 1-2y, 2-3y, 3-8y, 8-12y, <12y	3 rd quartile P _{KA}		12	No
Yakoumakis et al, 2014	EL?	Patients	Barium meal	Newborn 1y, 5y	Mean P _{KA}	51	1	No

15
 16 Hiorns et al. (2014) reported LDRLs for paediatric fluoroscopy at a tertiary referral centre (GOSH,
 17 London, UK) and compared them with the current national DRLs. The authors' conclusions are that
 18 only strict attention to technique and critical review of LDRLs can ensure best practice. They also
 19 underscore that, if the DRLs are used as a sole guide, many institutions can be falsely reassured and
 20 may be using greater doses than necessary.

21
 22 In conclusion, data concerning paediatric DRLs in fluoroscopy procedures are extremely scarce.
 23 Just a single study reports national DRLs (Hart e al., 2012).

24 **C.4.3 Computed tomography**

25
 26 The summary of the literature survey for DRLs in paediatric computed tomography in European
 27 countries is compiled in Table C.8. The actual values of NDRLs are shown in Annex A and for
 28 *selected* other DRLs are given in tables in Annex B.

29

1 Thirteen European publications plus one personal communication (Ruiz-Cruces, 2015) were
 2 identified which reported dose values for paediatric CT examinations, eleven of which were based
 3 on data collected from single countries, while three collected data from multiple jurisdictions
 4 (Brisse & Aubert, 2009; Järvinen et al., 2011; Shrimpton & Wall, 2000). Many of these
 5 publications (N=7) proposed national DRL values based on their data; three of them (Roch and
 6 Aubert, 2013; Shrimpton et al., 2006, Ruiz-Cruces, 2015) have resulted in currently existing NDRLs
 7 (see also Table 4.1), one (Galanski et al., 2005) has resulted in NDRLs which are already obsolete,
 8 two (Santos et al., 2013; Shrimpton et al., 2014) proposed NDRLs, and one (Verdun et al., 2008)
 9 proposed DRLs to be used only provisionally until more robust data became available. Two studies
 10 (Buls et al., 2010, Granata et al. 2015) are national multi-centre studies but do not propose national
 11 DRLs, and one (Yakoumakis et al., 2009) presents local DRLs and derives from these a suggestion
 12 for national DRLs.

13
 14 In terms of the examinations for which DRLs were calculated, the most common were for
 15 brain/head (N=14), chest (N=13) and abdomen (/pelvis) (N=10), although others were included by
 16 some, facial bones / sinuses (N=4), temporal bones / inner ear (N=2), HRCT (N=1), low dose chest
 17 (N=1) and lumbar spine (N=1)). Most studies, where the patient data was not collected from the
 18 displayed CT dose metrics for each patient, do not report the scan length per examination which can
 19 have a large effect on the study DLP. Regarding the abdomen (/pelvis) examination, six studies
 20 reported the extent of the scan range used, as being the full abdomen (from the diaphragm to the
 21 symphysis pubis), but one study (Verdun et al., 2008) did not provide this detail, making
 22 comparison between studies difficult. Similarly only half of publications (Brisse & Aubert, 2009;
 23 Buls et al., 2010; Järvinen et al., 2011,2014; Shrimpton et al., 2006, 2014; Verdun et al., 2008)
 24 incorporated clinical indications (e.g. trauma) in the setting of DRLs. To allow comparison between
 25 published values, it is essential that clinical indications for CT protocols (e.g. Head CT: trauma) are
 26 reported, as protocols and doses for specific clinical indications within a single CT examination
 27 category (e.g. Head) can differ significantly.

28
 29 Table C.8. Published studies on paediatric DRLs for CT in European countries.
 30

Reference	Region	Data source	Exams	Patient group	Dose value	No. patients	No. centres	NDRLs proposed
Brisse et al, 2009	FR data + 1 Belgian hosp. and 1 Dutch hosp.	Sample protocols	Head, Facial bones, Sinus, Temporal bones, Chest, Low dose chest, Abdomen-Pelvis Bone	1y, 5y, 10y	3 rd quartile CTDI _{VOL}	N/a	20	Yes
Buls et al, 2010	BE	Phantoms	Head, Sinus, Inner Ear, Chest, Abdomen	<1y 1-5y 5-10 y 10-15y	3 rd quartile values from standard protocols	N/a	18	No
Verdun et al, 2008	CH	Sample protocols	Brain, Chest, Abdomen	<1y, 1-5y, 5-10y, 10-15y	Mean CTDI _{VOL} , DLP	N/a	8	Yes

Reference	Region	Data source	Exams	Patient groupin g	Dose value	No. patients	No. centres	NDRLs proposed
Galanski et al, 2005	DE	Sample protocols	Brain, Facial bones/Sinus Chest, Abdomen/ Pelvis, L-spine	Newborn <1y 1-5y 6-10y 11-15y >15y	3 rd quartile CTDI _{VOL} , DLP	N/a	63	Yes
Yakoumakis et al, 2009	EL	Phantoms	Brain, Chest, Abdomen	5y, 10y	3 rd quartile CTDI _{VOL} , DLP	N/a	12	No. PDRL for 12 sites
Rafael Ruiz-Cruces, 2015 (DOPOES-project)	ES	Patients	Head, Chest, Abdomen	0y, 1-5y, 6-10y, 11-15y	3 rd quartile DLP	80-750	5-10 % of total	YES
Jarvinen et al., 2011	FI (EE, LI)	Patients	Brain, Chest	0-9kg, 9-19kg, >19kg, 0-10kg, 11-25kg, 26-40kg, 41-60kg, 61-75kg, >75kg	3 rd quartile DLP	286	9	No
Jarvinen et al., 2015	FI	Patients	Head Chest, Abdomen, Chest + Abdomen	< 1y, 1-<5y, 5-<10y, 10-15y DRL curve with weight	3 rd quartile CTDI _{VOL} , DLP	1049	4	Yes (Existing NDRL, see C.3.3)
Roch & Aubert, 2013	FR	Sample protocols	Brain, Facial bones, Chest, Abdomen/ Pelvis	1y /10kg 5y /20kg 10y/30kg	3 rd quartile CTDI _{VOL} , DLP	Not given	Not given	Yes (Existing NDRL, see C.3.3)
Granata et al. , 2015	IT	Patients	Head, Chest, Abdomen	1-5y, 6-10y, 11-15y	3 rd quartile CTDI _{VOL} , DLP	993	25	No but reports 3 rd quartile values
Santos et al, 2013	PT	Patients	Head, Chest	0y, 5y, 10y, 15y	3 rd quartile CTDI _{VOL} , DLP	330	3	Yes
Shrimpton & Wall, 2000	7 countries	Phantoms	Brain, Chest, HRCT, Upper Abdomen, Lower abdomen	<1y, 5y, 10y	3 rd quartile CTDI _{VOL} , DLP	N/a	40	No. Regional Europe
Shrimpton et al, 2006	UK	Sample protocols	Head, Chest	0-1y, 5y, 10y	3 rd quartile CTDI _{VOL} , DLP	Not given	126	Yes (Existing NDRL, see C.3.3)
Shrimpton et al, 2014	UK	Patients	Head	0-1y, >1-5y, >5-10y	3 rd quartile CTDI _{VOL} , DLP	838	19	Yes (Existing NDRL, see C.3.3)

1 All methodologies used the standard CT dose metrics of either CTDI_{vol} and/or DLP, with the majority
2 (N=12) basing their calculations on the 3rd quartile of dose distribution recorded. Just one study
3 used the adjusted mean value as a DRL (Verdun et al., 2008), as no dose distribution was available
4 here, while Galanski et al (2005) used a modified 3rd quartile value.

5
6 Three distinct methods of data collection were noted across all publications, with six collecting the
7 displayed CT dose metrics from patient studies (Järvinen et al., 2011, 2014; Santos et al., 2013;
8 Shrimpton et al. 2014; Ruiz-Cruces, 2015; Granata et al., 2015), while another three (Shrimpton &
9 Wall, 2000; Yakoumakis et al., 2009; Buls et al., 2010) used phantom data and the remaining five
10 collected CT dose metrics from standard protocols (Galanski et al., 2005; Shrimpton et al., 2006,
11 Verdun et al., 2008; Brisse & Aubert, 2009; Roch & Aubert, 2013). The number of CT scanners
12 from which data was collected varied from as little as three scanners (Santos et al., 2013) to as
13 many as 126 (Shrimpton & Wall, 2000), while the reported patient numbers ranged from 51 to
14 1049, divided amongst all the various examination and patient categories.

15
16 Regarding patient groupings, the majority of publications used patient age (N=11) with just two
17 using patient weight (Järvinen et al., 2011, 2014), and one quoting both patient age and weight
18 (Roch & Aubert, 2013). Of note a variety of patient age categories were used, although the most
19 common appears to be derivations of the following <1, 1-5, 5-10, 10-15 years of age.

20
21 Most studies (N=11) detailed the calibration phantom size (16 cm or 32cm) used for reporting
22 paediatric CT dose metrics, or else reported values based on both phantom sizes (e.g., Galanski et
23 al., 2005). This involved applying a correction factor for some examinations, in particular trunk
24 examinations to adjust for this difference, which exists with some manufacturer's settings. However
25 two studies (Santos et al., 2013; Verdun et al., 2008) did not specify or detail such adjustment, so it
26 is unclear which values are reported. Only one study (Santos et al., 2013) reported calibrating /
27 checking the displayed dose metrics to ensure accuracy prior to reporting patient values, although
28 two others did refer to routine quality assurance being performed (Shrimpton et al., 2014; Verdun et
29 al., 2008).

30
31 In conclusion, a small number of European publications have collected paediatric CT data with
32 most of these doing so to propose national DRL values, although a range of methodologies were
33 used. In particular, studies varied according to whether patient or phantom/protocol data was
34 collected and also in how patients were categorized into specific age ranges.

35 **C.4.4 Interventional radiology**

36 *C.4.4.1 Paediatric interventional cardiology*

37
38 Data concerning dose exposures in paediatric interventional cardiology are very scarce. All of the 8
39 European articles located (Barnaoui et al., 2014; Dragusin et al., 2008; Martinez et al., 2007;
40 McFadden et al., 2013; Onnasch et al., 2007; Tsapaki et al., 2008; Papadopoulou et al., 2005,
41 Corredoira et al., 2015) considered data from a single institution. The main aim of all studies was to
42 determine Local Diagnostic Reference Levels (LDRL). In a recent article (Corredoira et al., 2015)
43 the impact of 3D rotational angiography, or Cone beam CT, on the patient dose level was studied.
44 Of 7 Institutions from 6 countries (BE, DE, EL, ES, FR, IE), 7 were specialized paediatric
45 cardiology interventional units and 1 general cardiology unit (EL; Tsapaki et al, 2008).

46
47
48 The number of interventional procedures undertaken in a single institution ranged from 137 to
49 2140, performed mostly from 1998 to 2011. Examples of the procedures studied are: PDA closure,

1 atrial septal defect closure, balloon angioplasty, balloon valvuloplasty, and electrophysiology for
2 different body weight ranges.

3
4 Patient grouping was done according to age in 4 studies (Dragusin et al., 2008; Martinez et al.,
5 2007; McFadden et al., 2013; Tsapaki et al., 2008) and to weight in 2 studies (Barnaoui et al., 2014,
6 Corredoira et al., 2015). In 1 study (Onnasch et al., 2007) grouping was not done but P_{KA} was
7 normalized to body weight, whereas grouping was not done at all in 1 study (Papadopoulou et al.,
8 2005).

9
10 In all studies dose exposures were differentiated between diagnostic and interventional procedures.
11 In 2 studies (Barnaoui et al., 2014; Onnasch et al., 2007) exposure data were provided concerning
12 respectively 5 and 7 different common interventional procedures.

13
14 In all studies the source of dosimetric values was the patient. LDRLs were reported as the mean
15 (Barnaoui et al., 2014; Dragusin et al., 2008; Martinez et al., 2007; McFadden et al., 2013; Onnasch
16 et al., 2007, Corredoira et al., 2015) or median (Tsapaki et al., 2008; Papadopoulou et al., 200530-
17 32) value of the distribution of the dose observed. Corredoira et al., 2015 reported also 75th
18 percentile values. Dosimetric values were expressed in terms of P_{KA} in 7 studies, whereas in 1 study
19 these were reported as P_{KA} per body weight (Onnasch et al., 2007). Effective dose was also reported
20 in 1 study (Onnasch et al., 2007) and calculated in detail by Dragusin et al., 2008. Mean fluoroscopy
21 time and number of images was reported in 4 studies (Barnaoui et al., 2014; Dragusin et al., 2008;
22 McFadden et al., 2013; Tsapaki et al., 2008). Dose data were quite dispersed among institutions.

23
24 More details from some of these studies are compiled in Annex G.

25
26 In conclusion, dose data concerning exposures from paediatric interventional cardiology procedures
27 are still very scarce. Neither national nor regional DRLs are available, only LDRLs are provided by
28 each study. The studies greatly differ in their methodology and information provided, making the
29 comparison very difficult. Furthermore, sometimes the conclusions are contradictory. Better
30 standardisation and guidelines are needed, in particular for the patient dose surveys as the basis of
31 setting the DRLs (see also the conclusions in Annex G).

32 33 *C.4.4.2 Paediatric non-cardiologic interventional procedures*

34
35 There are no studies available from European countries on DRLs for paediatric non-cardiologic
36 interventional procedures.

37 38 **C.5 Other studies on paediatric DRLs**

39 In this section, DRLs published or studied outside Europe are briefly reviewed.

40 41 **C.5.1 Radiography**

42 A total of 5 publications were identified from outside Europe which reported DRL values for
43 paediatric radiography, with 2 from America (Freitas, 2009; ACR, 1998; 2013), 2 from Asia
44 (Sonawane, 2011; Kim, 2012) and 1 from Africa (Wambani, 2013). All studies but one (Wambani,
45 2013) determined national DRLs.

46
47 The most common examination for which DRL values were calculated was for the Chest (N=5).
48 Other examinations were: skull (N=3) (Wambani, Sonawane, Freitas), abdomen (N=2) (Wambani,
49 Sonawane), pelvis (N=2) (Wambani and Sonawane) and spine (N=2) (Wambani, Sonawane).

1
2 All studies but one (Wambani, 2013) based their DRL calculations on the 3rd quartile value.
3 Wambani (2013) calculated the mean value of measurements for setting local DRLs.
4

5 The dose quantity applied was $K_{a,e}$ (N=5) (ESD with Wambani, Kim, and Freitas and ESAK with
6 Wambani and Sonawane). One study used air-kerma without backscatter (ACR). Two out of 5
7 studies based their calculations on patient data (Wambani, Freitas) and the rest on air-kerma or
8 phantom measurements. Patients in these 2 studies were grouped according to age.
9

10 All 5 studies have major limitations and could not be considered for DRL determination. These
11 limitations are listed below:

- 12 • The Wambani study is limited to only one hospital.
- 13 • The Sonawane study defines DRLs for only one age group 5-9 yrs old.
- 14 • The Freitas study considers all children under 15 years old as one group and there is no
15 division of the sample into groups.
- 16 • The Kim study found the 3rd quartile value was too high and it was finally concluded that it
17 could not be used as a DRL
- 18 • The ACR study is based on data from 1998.

19
20 In conclusion, none of the above studies could be considered when trying to set up DRLs in
21 radiography.
22

23 **C.5.2 Fluoroscopy**

24 Only three articles on DRLs have been found from countries outside Europe (NCRP, 2012; Emigh
25 et al., 2013; Lee et al., 2009). The NCRP report (NCRP, 2012) does not recommend DRLs in terms
26 of P_{KA} but in terms of $K_{a,i}$ at a specified location. The measurements were made using a geometry
27 representative of clinical conditions which includes some backscatter due to the phantom-dosimeter
28 geometry. The other two articles (Emigh et al., 2013; Lee et al., 2009) report P_{KA} and effective dose
29 estimations for patients in single institutions, for upper GI examinations and MCU, respectively;
30 these studies can be considered to yield data for local DRLs only.
31

32 **C.5.3 Computed tomography**

33 A total of thirteen publications were identified from outside Europe which reported DRL values for
34 paediatric CT, with four from USA (NCRP, 2012; CRCPD, 2012; Goske et al., 2013; McCollough
35 et al., 2011) and three from Australia (Brady, Ramanaukas, Cain, & Johnston, 2012; Hayton et al.,
36 2013; Watson & Coakley, 2010), one from Syria (Kharita & Khazzam, 2010), Thailand
37 (Kritsaneepaiboon, Trinavarat, & Visrutaratna, 2012) and Japan (Fukushima et al., 2012), one with
38 data from both Saudi Arabia and Australia (Mohiy et al., 2012) and finally two international studies
39 performed by the IAEA across 40 countries (Vassileva et al., 2015; Vassileva and Rehani 2015).
40

41 Most publications did not report national DRL values. Two of the Australian studies reported local
42 DRLs for single institutions, each with a single CT scanner (Brady et al., 2012; Watson & Coakley,
43 2010), while the other (Hayton et al., 2013) was unable to collect sufficient data from a nationwide
44 study to propose DRLs. Fukushima et al (2011) calculated regional DRL values, while
45 Kristaneepaiboon et al (2010) and Goske et al (2013) calculated local DRLs for just three and six
46 selected centres respectively. The Nationwide Evaluation of X-ray Trends survey in the US
47 (CRCPD, 2012) did not set DRLs, but rather reported 75th percentile values for the data collected to
48 allow comparison with other published DRL figures. McCollough et al (2011) did report national

1 DRL values, based on phantom measurements using standard protocols, although this used data
2 from 2002. The recent IAEA study (Vassileva et al., 2015) proposes international DRLs for
3 paediatric CT examinations in 4 age groups, based on data from 32 countries worldwide.
4

5 The most common examinations for which DRL values were calculated was for the abdomen (or
6 abdomen/pelvis) (N=10), Head (N=9), and Chest (N=6), although one single centre study also
7 reported values for temporal bones, sinuses and HRCT examinations (Watson & Coakley, 2010).
8 Eleven of the twelve studies based their DRL calculations on the 3rd quartile value, using either or
9 both CTDI_{VOL} and DLP, with only one reporting the mean value (Brady et al., 2012) and another
10 also reported the SSDE (Goske et al., 2013).
11

12 Six of the twelve studies based their calculations on patient data (Brady et al., 2012; Fukushima et
13 al., 2012; Goske et al., 2013; Hayton et al., 2013; Kritsaneepaiboon et al., 2012; Watson & Coakley,
14 2010) using relatively small numbers (range 220-1382), with the other studies using either phantom
15 data or standard protocols. Patients were mainly grouped according to age (N=8), although the age
16 categories varied significantly between studies. One study categorized according to weight (Watson
17 & Coakley, 2010), while another according to body width (Goske et al., 2013).
18

19 Of interest, one study proposed a range of dose values for CT, termed a diagnostic reference range
20 (Goske et al., 2013), which included a lower 25th percentile value, below which it advised that
21 image quality may not be diagnostic and was based on a subjective image quality analysis, while
22 the upper 75th percentile value gave an indication of when doses may be excessive. This study also
23 reported the SSDE based on body size as a better indicator of patient dose.
24

25 Regarding limitations, only seven studies reported the phantom size used, with just two reporting
26 performing any calibration / checking of the displayed dose metrics to ensure accuracy prior to
27 reporting patient values. Of the ten studies reporting values for the abdomen examination again in
28 four it was unclear whether this referred to the entire abdomen/pelvis or just to the upper abdomen.
29

30 In conclusion, the majority of international publications reported local DRLs for a small number of
31 centres and not national values. Although age was the most commonly used method to categorise
32 patients there was no consistency in terms of the categories used between studies.
33

34 **C.5.4 Interventional radiology**

35 *C.5.4.1 Paediatric interventional cardiology*

36

37 Only four articles on paediatric DRL studies outside European countries have been found (Chida et
38 al, 2010; Ubeda et al., 2011; Ubeda et al. 2015; Vano et al., 2011). Three of these articles
39 considered data just from a single institution, and one (Vano et al., 2011) dealt with 10 centres in 9
40 different South American countries. The main aim of the first three studies was to determine local
41 DRLs, while Vano et al. (2011) aimed at determining the quality of radiation protection in
42 paediatric cardiologic IR procedures in Latin America; patient radiation doses were collected from
43 only 70 procedures. Of 12 institutions from 11 countries (Japan, Chile and nine South American
44 countries) 1 (Ubeda et al., 2011; 2015) was a specialized paediatric cardiology interventional unit
45 and 11 others general cardiology units. The number of interventional procedures executed in the
46 two single institutions (Chida et al, 2010; Ubeda et al., 2011; 2015) was 239 and 517 and
47 respectively.
48

1 Patient grouping was according to age except in the study by Chida et al. (2010), where grouping
2 was not done at all. Patient doses were differentiated between diagnostic and interventional
3 procedures except in the study by Vano et al. (2011).
4

5 In all studies the source of dosimetric values was the patient. Local DRLs were reported as the
6 mean (Chida et al, 2010) or median (Ubeda et al., 2011; 2015) value of the distribution of the doses
7 observed. The dosimetric data reported in the multicentre study by Vano et al. (2011) cannot be
8 considered as DRL data, as the sample was too small. Dosimetric values were expressed in terms of
9 P_{KA} in all studies. Mean fluoroscopy time was reported only by Chida et al. (2010), while none of
10 these publications reported the number of images. Dose data were quite dispersed among
11 institutions.
12

13 More details of the first three publications are compiled in Annex G.
14

15 In conclusion, data published outside European countries, concerning patient doses and DRLs from
16 paediatric interventional cardiology procedures, is even scarcer than in Europe. Only local DRLs
17 are provided by the existing few studies. Similarly to European studies, these studies greatly differ
18 in their methodology and information provided, making comparisons very difficult.
19

20 *C.5.4.2 Paediatric non-cardiologic interventional procedures* 21

22 Data concerning dose exposures in paediatric non-cardiologic interventional procedures are
23 extremely scarce and limited to common vascular and enteric procedures. Just one non-European
24 article concerning paediatric non-cardiologic interventional procedures from a single paediatric
25 institution was found (Govia et al., 2012). The aim of this study was to determine the effective dose
26 in children for enteric (insertion of gastrostomy tube, gastro-jejunal tube, cecostomy tube and their
27 maintenance) and venous access procedures (central venous catheter, PICC, Port). Patient grouping
28 was according to age. The number of procedures performed from 2004 to 2008 was 7074.
29

30 No data are available about embolization or sclerotherapy of vascular malformations,
31 neuroradiology procedures, arteriography, CT guided biopsies, and biliary IR. Although relatively
32 rare, these procedures can cause very high individual dose exposures. Therefore, further studies and
33 guidelines are needed, as the basis to setting DRLs.

1 **ANNEX D. NEED FOR PAEDIATRIC DRLs**

2 For the basis of the recommendations given in Section 6, on the paediatric examinations and
3 procedures with highest need for DRLs, statistical information on the frequency of paediatric
4 examinations was collected. Further, the relative importance of the examinations in Tables 6.1 and
5 6.2, on point of view of their contribution to the overall collective effective dose to population
6 (population dose) was analysed by rough estimation of the population doses.
7

8 **D.1 Frequencies of paediatric examinations**

9 Information about the distributions of different types of procedures in paediatric imaging is sparse;
10 the paper by Seidenbusch depicts such data over 30 years but gives no information on the
11 proportion of paediatric examinations compared to adult examinations (Seidenbusch & Schneider,
12 2008). The UNSCEAR 2013 Report, Volume II, Scientific Annex B (UNSCEAR, 2013)
13 summarizes the percentages of various types of medical examinations on infants and children (0-15
14 years old) in well-developed countries. This indicated that approximately 3-10 % of all x-ray
15 procedures are performed on children. The UNSCEAR report also gives some data on the age and
16 sex distributions of various radiographic examinations, and summarizes methods to estimate
17 effective doses from the measurable patient dose metrics for various examinations. In an IAEA
18 survey of paediatric CT practice in 40 countries in Asia, Europe, Latin America, and Africa
19 (Vassileva et al., 2012, 2013), the average frequency of paediatric CT examinations for all
20 departments was 7.5% in 2007 and 9.0%, in 2009. The lowest mean frequency was in European
21 facilities (4.6% in 2007 and 4.3% in 2009). In Finland, complete statistics of all paediatric
22 examinations has been published every three years (STUK, 2013).
23

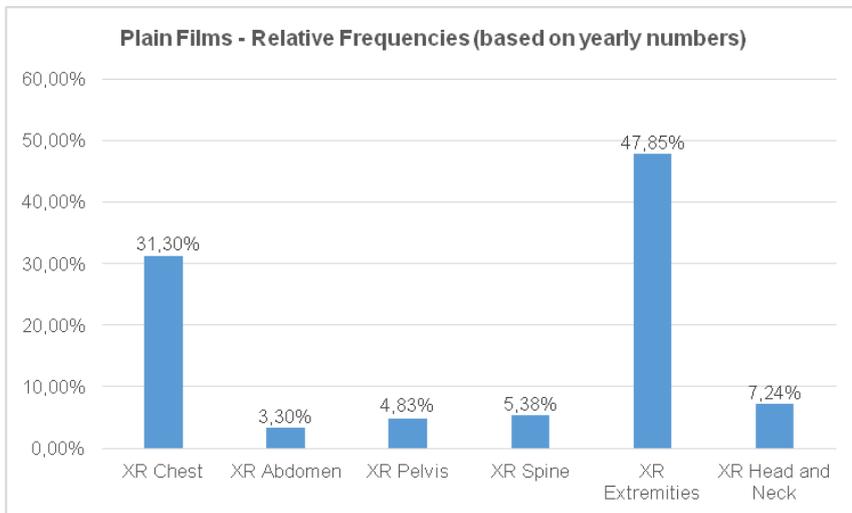
24 Because of the general sparseness of data, the specific questionnaire on the most common paediatric
25 examinations was conducted to support the information available from the other sources. The
26 questionnaire was sent to key persons of the European Society of Paediatric Radiology (ESPR –
27 www.espr.org) and to medical partners of Central European Exchange Program for University
28 Studies (CEEPUS; www.ceepus.info). Altogether 33 centres were contacted and responses were
29 received from 18 centres (54.5%; Table D.1); from one centre information was received only for
30 frequencies for Interventional Radiology.
31
32

1 Table D.1. Responses per country (without Interventional Radiology and Cardiac Catherization).
 2

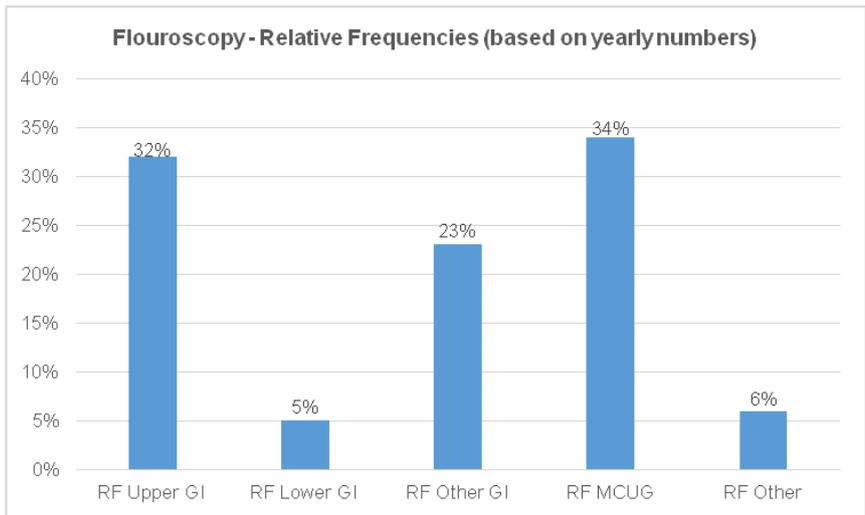
Country	Responses
AT	3
CH	1
CZ	1
DE	1
IE	1
IT	2
PT	2
RO	2
SI	1
RS	2
UK	1
Total	17

3
 4
 5
 6
 7
 8
 9

The detailed results of the questionnaire are presented in Tables D.2 to D.4. The calculated relative frequencies of examinations, for radiography, fluoroscopy and CT, based on the total annual frequencies obtained from the 16 centres that replied to the questionnaire, are shown in Fig. D.1 to Fig. D.3, respectively.

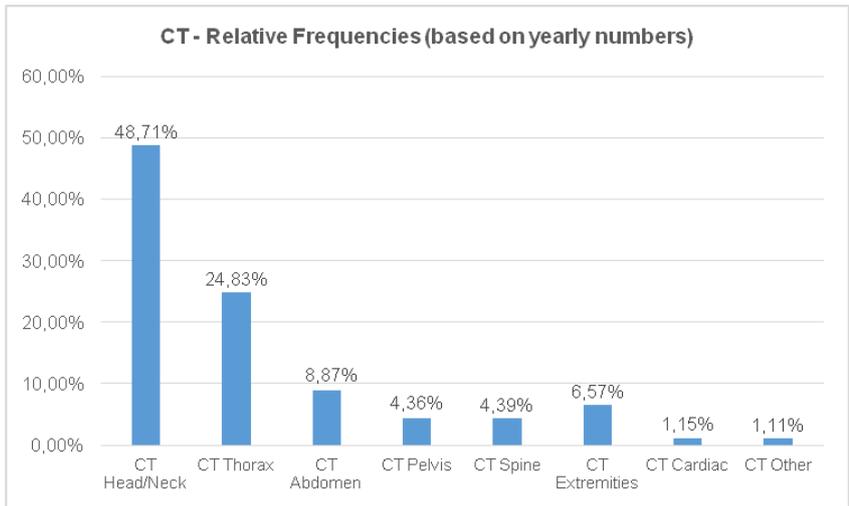


10
 11
 12 Fig. D.1. Relative frequencies of plain radiography examinations.
 13



1
2
3
4
5

Fig. D.2. Relative frequencies of fluoroscopy examinations



6
7
8
9

Fig. D.3. Relative frequencies of computed tomography examinations.

10 These result for radiography, fluoroscopy and CT are reasonably consistent with the data obtained
11 from the others sources of information, i.e. the literature survey and information collected through
12 the PiDRL contacts.

13
14

1 Table D.2. Radiography examinations.
2

Country	XR Chest	XR Abdomen	XR Pelvis	XR Spine	XR Extremities	XR Head & Neck
Austria	12800	2398	2069	3211	43799	5751
Czech	9903	664	0	0	13658	2478
Germany	1989	0	943	547	2205	0
Ireland	6581	1187	4714	863	2348	0
Italy	34589	5303	3523	4897	42947	1408
Portugal	1447	0	540	662	279	318
Romania	7933	250	827	1881	20377	4056
Serbia	12260	1998	1490	3100	33687	6350
Slovenia	2194	61	60	136	1307	51
Swiss	3452	356	710	0	3692	0
UK	13897	1859	1324	2472	857	0
Total	107045	14076	16200	17769	165156	20411
Mean	9731,32	1279,64	1472,68	1615,40	15014,17	1855,58
Stand. Dev.	9429,09	1592,17	1462,95	1623,23	17453,45	2453,47
%	31,42	4,13	4,76	5,22	48,48	5,99

3
4
5 Table D.3. Fluoroscopy (Upper GI: upper gastro-intestinal tract, lower GI: lower gastro-intestinal
6 tract, MCU: micturating-cysto-urethrography)
7

Country	RF Upper GI	RF lower GI	RF Other GI	RF MCU	RF Other
Austria	82	50	371	509	2
Czech	283	149		296	
Germany	62	54		114	15
Ireland	456		131	119	
Italy	868			1149	
NL	90	82	9	37	48
Portugal	266			276	156
Romania	451		164	35	157
Serbia			104	377	
Slovenia	70	7	59	50	45
Swiss	47	35	23	146	8
UK	333		866	179	
Total	3007	377	1727	3287	431
Mean	273,39	62,75	215,91	273,92	61,60
Stand. Dev.	251,00	48,90	286,26	311,96	67,14
%	34,06	4,26	19,56	37,23	4,88

8
9
10

1 Table D.4. Computed tomography.
2

Country	CT Head/Neck	CT Thorax	CT Abdomen	CT Pelvis	CT Extremities	CT Cardiac
Austria	1370	568	395	154	429	18
Czech						
Germany	79	30			20	
Ireland	83	90				
Italy	2617	2632	1420	88	300	182
NL	334	199	21	7	173	5
Portugal	1018	851	603	423	192	
Romania						
Serbia	2068	281	203	18	105	
Slovenia						
Swiss	370	141	45	21	19	32
UK	1244	656				109
Total	9183	5448	2687	711	1238	346
Mean	1020,36	605,31	447,82	118,45	176,81	69,14
Stand. Dev.	899,87	810,42	524,74	159,41	149,40	74,92
%	46,82	27,78	13,70	3,62	6,31	1,76

3

4

5 D.2 Population dose from paediatric examinations

6 As discussed in Section 6, the need for a DRL is judged mainly on the basis of collective effective
7 dose to population: all examinations resulting in high collective effective doses should have DRLs.

8

9 For the estimation of population dose, the frequencies of paediatric examinations for several age (or
10 weight) groups should be known as well as the typical effective doses for each examination and
11 each age (weight) group. Such information is not comprehensively and conveniently available, and
12 can have high differences from country to country. Therefore, it has neither been possible nor
13 considered feasible to provide an exact analysis on the population dose caused by the paediatric
14 examinations recommended for DRLs in Section 6.

15

16 However, a very rough estimate of the population dose was done for some of the radiography and
17 CT examinations, making use of (1) relative distributions of frequencies for various age groups
18 based on comprehensive frequency data available from one country, (2) the total frequency data
19 from the DDM2 project (EC, 2014), and (3) published values of typical effective doses of paediatric
20 examinations (mean values were calculated from several published values). Due to the roughness of
21 the results or associated high uncertainties, only relative values of this estimation are shown in
22 Table D.5.

23

24

1 Table D.5. Relative collective effective doses to population, for a few paediatric radiography and
 2 CT examinations where setting DRLs has been recommended
 3

Anatomical region	Description (PiDRL)	Relative collective effective dose to population, normalized to thorax radiography.
Radiography		
Head (skull)	AP/PA and LAT	0,01
Thorax	Thorax AP/PA	1,0
Abdomen	Abdomen-pelvis AP	0,1
Pelvis	Pelvis/hip AP	na
Spine	Cervical spine AP/PA and LAT	na
	Thoracic spine AP/PA and LAT	na
	Lumbar spine AP/PA and LAT	na
	Whole spine/Scoliosis AP/PA and LAT	na
Computed Tomography (CT)		
Head	Routine	2,6
	Paranasal sinuses	na
	Inner ear/ Internal auditory means	na
	Ventricular size (shunt)	na
Neck	Neck	na
Chest	Chest	10,2
	Cardiovascular CT angiography	na
Abdomen	Abdomen (upper abdomen)	4,5
	Abdomen+pelvis	na
Trunk	Whole body CT in trauma	na
Spine	Cervical+thoracic+lumbar	na

4 na: not available (sufficient data for calculations have not been available)
 5

6 It can be seen that, despite of being a very low dose examination, conventional thorax radiography
 7 is of top importance among radiography because of its commonness. On the other hand, all CT
 8 examinations result in higher population dose than any of the radiography examinations, thus
 9 highlighting the importance of establishing DRLs also for paediatric CT examinations.

10 The proportion of the collective effective dose of the paediatric examinations shown in Table D.5
 11 from the total population dose (adults + children) varied from less than 1 % to more than 3 %. For
 12 spine CT, this proportion seemed to be much higher and also the collective effective dose seemed to
 13 be very high; no value has been recorded in Table D.5., because of the very poor statistics of this
 14 case. This observation however supports paediatric spine CT to be in the list of examinations where
 15 DRL should be established.
 16

1 ANNEX E. DEVELOPMENT OF DOSE MANAGEMENT SYSTEMS

2 E.1 General development

3 Dose management systems are an extremely helpful tool for radiation protection, dose monitoring,
4 quality control, detection and reporting of unintended overexposures (EU-BSS, Art. 63; EC, 2013)
5 and collection of data for national authorities for update of NDRLs.

6
7 The first step towards automatic dose management systems was the DICOM standard which has
8 specified that the radiation dose to the patient (or more specifically, the doses reported by the x-ray
9 unit) may be stored in the DICOM header of each image. However, at that time, the data was only
10 stored in the Picture Archiving and Communication System (PACS). In many cases it is therefore
11 impossible to deduce the dose from the procedure. Moreover, the DICOM standard does not give
12 requirements on necessary fields to be filled, e.g., which field (place of information) should be used
13 for a given parameter. The dose reporting was completed independently by various vendors and the
14 comparison of different dose reports is not straightforward. In CT examinations, an advantage of
15 dosimetric data in the DICOM header of each CT slice is, that it allows monitoring the dose
16 distribution along the z-axis of a patient, if dose modulation is used.

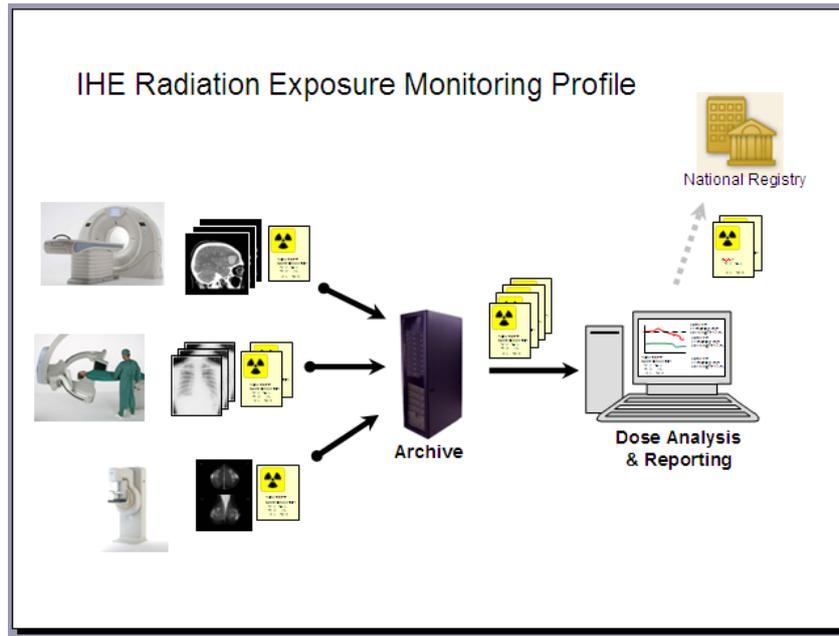
17
18 The above shortcomings were identified and a DICOM supplement 94 was published in 2005
19 (DICOM, 2005). In this supplement a new type of dose report was described (Radiation Dose
20 Structure Report, RDSR) that was intended to be used independently of the image data and be
21 stored in “an appropriate Radiation Safety Reporting System”. An advantage of RDSR is that
22 dosimetric data stored at the end of a procedure include exposures of non stored images like
23 rejected exposures. Furthermore RDSR in fluoroscopy also include the dose contribution of
24 fluoroscopy times without taking images. In 2007, the RDSR was promoted when the IEC
25 published a Publicly Available Specification (PAS) (IEC, 2007) that applies to medical electrical
26 equipment and medical electrical systems including fluoroscopy systems. It gives the means for
27 measuring or calculating dose-related quantities and for producing DICOM compatible images
28 and/or reports, i.e. RDSR’s. The implementation of the RDSRs was requested in the update of IEC
29 60601-2-43, published in 2010 (IEC, 2010). Currently, work is underway to publish IEC/PAS (IEC,
30 2007) as an IEC standard. Today nearly all modalities on the market allow generating and storing
31 DICOM images but a significant number of modalities are still not able to generate a RDSR report.

32
33 To overcome technical problems in inter-system communication, healthcare professionals and
34 industry have established a community (Integrating the Healthcare Enterprise, IHE) that aims to
35 improve the way computer systems in health care share information (IHE, 2014a). IHE publishes
36 Integration Profiles that describe solutions to particular problems by introducing case examples and
37 the use of standards. One profile is devoted to radiation exposure monitoring (IHE, 2014b). In this
38 profile the data flow (see Fig. E.1) and the functions of the different actors are described. The
39 interest of national authorities to collect the patient exposure data is clearly identified.

40
41 The software used to upload the data from the x-ray equipment or workstation can be made vendor-
42 independent, due to the use of the DICOM standard. In the central database, it is easy to implement
43 analysis functions. Special attention should be paid to data security and integrity of the data
44 especially if data are read remotely. The IHE profiles can be used as a basis for such solutions.

45
46 At the present time, several vendors offer commercial solutions for dose management solutions. A
47 typical system consists of a central data storage (database or cloud service) and an access to the
48 collected data using charting features and dashboard like visualisations (often internet browser
49 based).

1



2
3

4 Fig.E.1. Flow of data from the modality to the PACS and the local dose management system. The
5 local dose management systems can then report to national registries. Graphic from the IHE WIKI
6 (http://wiki.ihe.net/index.php?title=Radiation_Exposure_Monitoring).

7

8

9 **E.2 Existing dose management systems**

10

11 The information on existing dose management systems is based on a questionnaire to the
12 software manufacturers, direct contacts to these companies and Internet research. The summary
13 of the products is shown in Table E.1.

14

15 Table E.1 Commercial products for automatic patient dose management.

Product	Company	Website/contact
DoseMonitor = NEXO Dose	PHS Technologies Group LLC Bracco	www.dosemonitor.com Enrico.Seccamani@bracco.com ,
Dose Track	Sectra	https://www.sectra.com/medical/dose_monitoring/
DoseWatch	GE	http://www3.gehealthcare.com/en/products/dose_ma nagement/dosewatch
EasyDoseQM	BMS Informationstechno logie GmbH	http://www.bms-austria.com/
Imalogix	Imalogix	www.imalogix.com ,
OpenREM.org		http://openrem.org
Physico	MS Emme Esse	www.emme-esse.com

Product	Company	Website/contact
Radimetrics	Bayer HealthCare	http://www.medrad.com/en-us/info/products/Pages/Radimetrics-Enterprise-Platform.aspx
RDM (Radiation Dose Monitor)	Medsquare	www.medsquare.com
RightDose	Siemens	http://www.healthcare.siemens.com/medical-imaging/low-dose/
S1	RaySafe (Fluke Biomedical)	http://www.raysafe.com/Products/Patient/RaySafe%20S1
TQM /Dose (Total Quality Monitoring)	Qaelum N.V.	http://www.qaelum.com/products/total-quality-monitoring.html

1

1 **ANNEX F. DETAILS OF EDRL CALCULATION**

2 In Tables F.1 and F.2, more details of the calculation of the EDRLs (as shown in Tables 10.2 a, b)
 3 have been given. The list of countries are the countries, from where the DRL data (official NDRL,
 4 proposed NDRL or the 75th percentile determined from a nationwide patient dose distribution) is
 5 accepted for the calculation; the actual DRL data can be found in Annexes A or B. Both the mean
 6 and median (EDRL) values of the DRL distribution and their difference have been indicated, and
 7 also the interquartile value (ratio: 3rd quartile/ 1st quartile).

8
 9 The interquartile value gives some indication of how feasible the EDRL values are for adoption as a
 10 NDRL: high interquartile value means a higher risk that the true NDRL (based on country's own
 11 patient dose survey) could deviate significantly from the given EDRL, while for low interquartile
 12 value there is higher probability that the true NDRL could be closer to the given EDRL. As can be
 13 seen from the interquartile values, for example, the EDRLs for chest CT examinations (interquartile
 14 values 1.0-3.5) have a little higher uncertainties than the EDRLs for head CT examinations
 15 (interquartile values 1.2-1.4) and for most radiography examinations (interquartile values mostly 1.0
 16 – 2.0).

17
 18
 19 Table F.1. Calculation of the EDRL for radiography and fluoroscopy.
 20

Radiography and fluoroscopy										
Exam	Age group or weight group	Age group, y	Mean of DRL distribution		EDRL, median of DRL distribution		Diff. Median & mean, %	Countries	No of countries	Interquartile value
			K _{a,e1} , mGy	P _{KA1} , mGy cm ²	K _{a,e1} , mGy	P _{KA1} , mGy cm ²				
Head AP/PA	3 months-<1 y	1		220		215	-2	AT, DE, ES	3	1,18
	1-<6 y	5		293		295	1	AT, DE, ES	3	1,14
	>6 y	10		383		350	-9	AT, DE, ES, LT	4	1,14
Head LAT	3 months-<1 y	1		187		200	7	AT, DE, LT	3	1,11
	1-<6 y	5		253		250	-1	AT, DE, LT	3	1,02
Thorax AP/PA	5-<15 kg	1	0,07			0,06	-10	At, FI, LT	3	1,17
	15-<30 kg	5	0,08			0,08	-5	AT, DK, FI, FR, LT	5	1,43
	30-<50 kg	10	0,12			0,11	-14	AT, FI, FR, LT	4	1,60
	<5 kg	0		17		15	-13	AT, BE, DE, ES, FI, FR, NL	7	1,61
	5-<15 kg	1		29		22	-26	AT, BE, DE, ES, FR, LT, NL	8	1,96
	15-<30 kg	5		42		50	18	AT, BE, DE, ES, FI, FR, LT, NL	8	1,87
	30-<50 kg	10		66		70	5	AT, BE, DE, ES, FI, FR, LT	7	2,20
Abdomen AP	50-<80 kg	15		83		87	4	AT, ES, FI, LT	4	1,43
	15-<30 kg	5	0,60			0,40	-33	AT, FR, LT	3	1,75
	30-<50 kg	10	0,95			0,75	-21	AT, FR, LT	3	1,67
	<5 kg	0		64		45	-29	AT, BE, ES, NL	4	3,14
	5-<15 kg	1		165		150	-9	AT, BE, DE, ES, LT, NL	6	2,00
	15-<30 kg	5		321		250	-22	AT, BE, DE, ES, FR, LT, NL	7	1,22
Pelvis AP	30-<50 kg	10		538		475	-12	AT, BE, DE, ES, FR, LT	6	1,73
	50-<80 kg	15		733		700	-5	AT, ES, LT	3	1,90
	15-<30 kg	5		177		180	2	DE, FR, ES	3	1,15
	30-<50 kg	10		320		310	-3	DE, FR, ES	3	1,27
MCU	<5 kg	0		300		300	0	AT, DE, DK, ES, FI, NL, UK	7	2,00
	5-<15 kg	1		636		700	10	AT, DE, DK, ES, FI, NL, UK	7	1,65
	15-<30 kg	5		736		800	9	AT, DE, DK, ES, FI, NL, UK	7	1,71
	30-<50 kg	10		975		750	-23	AT, DE, ES, UK	4	2,14

21
 22

1 Table F.2. Calculation of the EDRL for computed tomography.

2

Computed tomography										
Exam	Age group or weight group	Age group, y	Mean of DRL distribution		EDRL, median of DRL distribution		Diff. Median & mean, %	Countries	No of countries	Interquartile value
			CTDI _{VOL} , mGy	DLP, mGy cm	CTDI _{VOL} , mGy	DLP, mGy cm				
Head	0-<3 months	0	28		24		-13	BE, DE, FI, NL, PT, UK,	6	1,19
	3 months-<1 y	1	28		28		-2	BE, DE, FI, IT, NL, UK	6	1,22
	1-<6 y	5	38		40		6	BE, DE, FI, IT, NL, PT, UK	7	1,22
	>6 y	10	52		50		-4	BE, DE, FI, IT, NL, PT, UK	7	1,23
	0-<3 months	0		343		300	-13	AT, DE, ES, FI, NL, PT, UK	7	1,24
	3 months-<1 y	1		404		385	-5	AT, DE, ES, FI, IT, LT, NL, UK	8	1,23
	1-<6 y	5		541		504	-7	AT, DE, ES, FI, IT, LT, NL, PT, UK	9	1,37
	>6 y	10		719		650	-10	AT, DE, ES, FI, IT, LT, NL, PT, UK	9	1,42
Thorax	<5 kg	0	2,4		1,4		-43	DE, FI, PT, UK	4	2,40
	5-<15 kg	1	1,7		1,8		1	BE, DE, FI, IT, UK	5	1,56
	15-<30 kg	5	3,1		2,7		-15	BE, DE, FI, IT, PT, UK	6	1,56
	30-<50 kg	10	4,5		3,7		-20	BE, DE, FI, IT, PT, UK	6	1,56
	50-<80 kg	15	5,6		5,4		-3	DE, FI, IT, PT	4	1,71
	<5 kg	0		47		34	-27	AT, DE, ES, FI, PT, UK	6	3,47
	5-<15 kg	1		56		49	-12	AT, DE, ES, FI, IT, UK	6	2,73
	15-<30 kg	5		80		70	-12	AT, DE, ES, FI, IT, PT, UK	7	1,73
	30-<50 kg	10		124		115	-7	AT, DE, ES, FI, IT, PT, UK	7	1,52
	50-<80 kg	15		185		198	7	AT, DE, ES, FI, IT, PT	6	1,07
Abdomen	5-<15 kg	1	3,7		3,5		-4	DE, FI, IT	3	1,75
	15-<30 kg	5	4,8		5,35		11	BE, DE, FI, IT	4	1,32
	30-<50 kg	10	6,7		7,3		9	BE, DE, FI, IT	4	1,21
	50-<80 kg	15	12,0		13,0		8	DE, FI, IT	3	1,23
	<5 kg	0		61		45	-26	DE, ES, FI	3	1,60
	5-<15 kg	1		111		118	6	DE, ES, FI, IT	4	1,93
	15-<30 kg	5		139		151	8	DE, ES, FI, IT	4	1,14
	30-<50 kg	10		210		209	-1	DE, ES, FI, IT	4	1,25
	50-<80 kg	15		474		478	1	DE, ES, FI, IT	4	1,23

3
4

1 ANNEX G. PATIENT DOSES AND DRLS IN PAEDIATRIC CARDIAC AND NON 2 CARDIAC PROCEDURES

3 G.1 Paediatric diagnostic or therapeutic interventional cardiac procedures

4 G.1.1 Introduction

5 Interventional cardiology (IC) is a subspeciality of cardiology/radiology, whereby procedures that
6 traditionally used a surgical approach are performed during a heart catheterization. These minimally
7 invasive procedures involve inserting catheters and other devices through superficial arterial and
8 venous access sites. IC can be used to carry out both diagnostic and therapeutic examinations
9 depending on the procedure being carried out.

10

11 The number, types and complexity of interventional cardiac (IC) procedures have increased
12 dramatically in recent years due to increased reliability and advancing technology (McFadden et al.,
13 2013, Corredoira et al., 2013, Hijazi and Award, 2008). According to UNSCEAR (UNSCEAR
14 2013), 4 % of all cardiac angiography is carried out in paediatric patients. Also the use of CBCT in
15 paediatric cardiology has been increasing, because of its potential usefulness by acquiring high
16 resolution 3D images of vascular volumes (Corredoira et al., 2015).

17

18 Fluoroscopically guided cardiac catheterizations are an essential technique for the diagnosis and
19 treatment of congenital and acquired heart conditions. Paediatric IC procedures are very different
20 from adult IC procedures not only because of the age of the patients but also because of the
21 diversity of structural anomalies in congenital heart diseases. Pediatric IC procedures are in general
22 longer and more complex than adult procedures (Ubeda et al., 2012; Lock, 2000).

23

24 The IC procedures can result in high patient doses, sometimes including also high skin exposure.
25 Patients with complex congenital heart disease are now living longer and may need several IC
26 procedures throughout their lifetime, thus the cumulative dose can become very high. The increased
27 risk of developing a malignancy (Rassow et al., 2000) highlights the importance of establishing
28 DRLs in paediatric IC; the risk for small children is higher because of the higher organ specific risk
29 factor and because the collimation is centred around the heart and more critical radiosensitive
30 organs are being irradiated simultaneously due to their close proximity to one another.

31

32 No NDRLs for paediatric IC have been set, but a few papers have been published in recent years,
33 reporting the patient doses in paediatric IC procedures and the development of local DRLs.

34

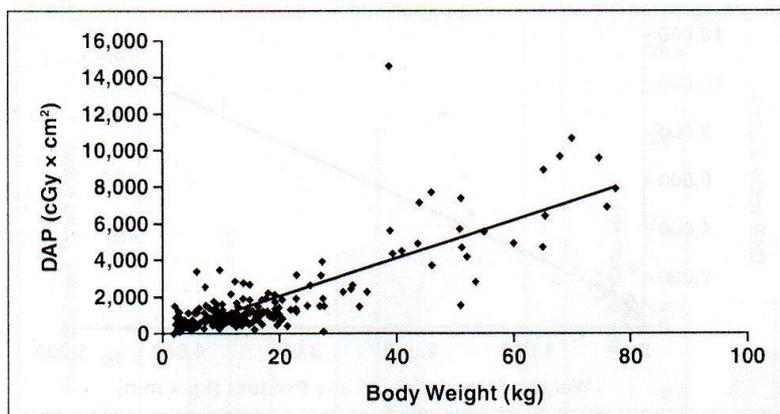
35 G.1.2 Recent publications on patient doses and LDRLs

36 Onnasch et al. (2007) evaluated P_{KA} values for three different types of angiography systems over a
37 time span of 8 years, for a total of 2859 patients. They observed linear correlation between P_{KA}
38 values and patient weight (body weight) and suggested P_{KA} per patient weight as the appropriate
39 DRL concept. They also observed that this constant of proportionality decreased during the years,
40 mainly due to technological advances rather than the experience of the operators. They observed
41 significant differences of patient dose levels between different types of IC procedures, the mean
42 value of P_{KA} per patient weight being between 0,35 and 1,3 Gy cm² kg⁻¹.

43

44 Chida et al. (2010) evaluated 239 consecutive paediatric patients who underwent cardiac
45 catheterizations or other IR procedures. They also found good correlation between P_{KA} and patient
46 weight; an example is shown in Fig. G.1. They concluded that patient doses in other IR procedures
47 were higher than in the IC procedures.

1
 2 Ubeda et al. (2012; 2015) evaluated patient doses in paediatric cardiology at first in a pilot program
 3 and more comprehensively for a three years period (2011-2013), in the largest paediatric hospital in
 4 Chile, which manages approximately 60 % of all paediatric cardiac procedures in the country. In
 5 total, they evaluated 517 consecutive procedures (200 diagnostic and 317 therapeutic). Their results
 6 also indicate a reasonable linear correlation between P_{KA} and body weight (R^2 coefficient ranged
 7 from 0,247 to 0,698) so that they could suggest P_{KA} per body weight ratios as a basis of the local
 8 DRLs. Using this ratio, they calculated the DRLs for different weight groups (10-60 kg), for both
 9 diagnostic and therapeutic procedures. They concluded that there was no significant difference
 10 between the diagnostic and therapeutic procedures: the 75th percentile value was 0,163 Gy cm² kg⁻¹
 11 for diagnostic procedures and 0,170 Gy cm² kg⁻¹ for therapeutic procedures. They noted that DRLs
 12 for IR procedures are linked to the complexity of the procedures: if the local values are higher than
 13 the DRL, the complexity of the local procedures should be analyzed together with the other factors.
 14



15
 16 Fig. G.1. P_{KA} as a function of body weight in paediatric patient who underwent cardiac
 17 catheterization ($r=0.819$, $p<0.01$; regression line $y=106.67 x - 130.0$) (Chida et al., 2010)
 18

19 McFadden et al. (2013) gathered data for a total 354 paediatric patients (159 diagnostic and 195
 20 therapeutic procedures) in a dedicated cardiac catheterization laboratory over a 17 month period;
 21 the mean patient age was 2.6 years (range newborn – 16 years) and the mean patient weight 14,9 kg
 22 (range 2,4 – 112,0 kg). Maximum P_{KA} readings were slightly higher for therapeutic interventions
 23 but the difference between diagnostic and therapeutic procedures was not statistically significant (p
 24 = 0.59). Patient weight and age had a moderate correlation with P_{KA} ($r = 0.557$ and $r = 0.472$,
 25 respectively), thus suggesting that either patient weight or age could be used to stratify LDRLs.
 26 LDRL values for several age groups were suggested based on the mean of the dose distribution
 27 according to the UK practice (IPEM, 2000) (not the 75th percentile as recommended in these EC
 28 guidelines). Maximum and minimum P_{KA} readings varied greatly between examinations and there
 29 was a high number of extreme outlier points recorded. It was found that the 4 main technical factors
 30 that had the most significant impact on the patient dose were: use of antiscatter grid, higher frame
 31 rates, complexity of procedure and the duration of fluoroscopy. Three levels of complexity were
 32 suggested: standard/uncomplicated, medium and very complex.
 33

34 Barnaoui et al. (2014) assessed patient exposure levels (P_{KA} , fluoroscopy time and the number of
 35 cine frames) in a French reference centre for paediatric IC. In the final analysis, they included all
 36 procedures performed more than 20 times for a given weight group, resulting in 801 procedures
 37 (288 diagnostic and 513 therapeutic). LDRLs were proposed for all three quantities as the mean
 38 values of the distribution; patient weight was used as the DRL parameter, because the technical
 39 parameters that influence the dose (tube voltage, mA and filtration) vary with patient weight and

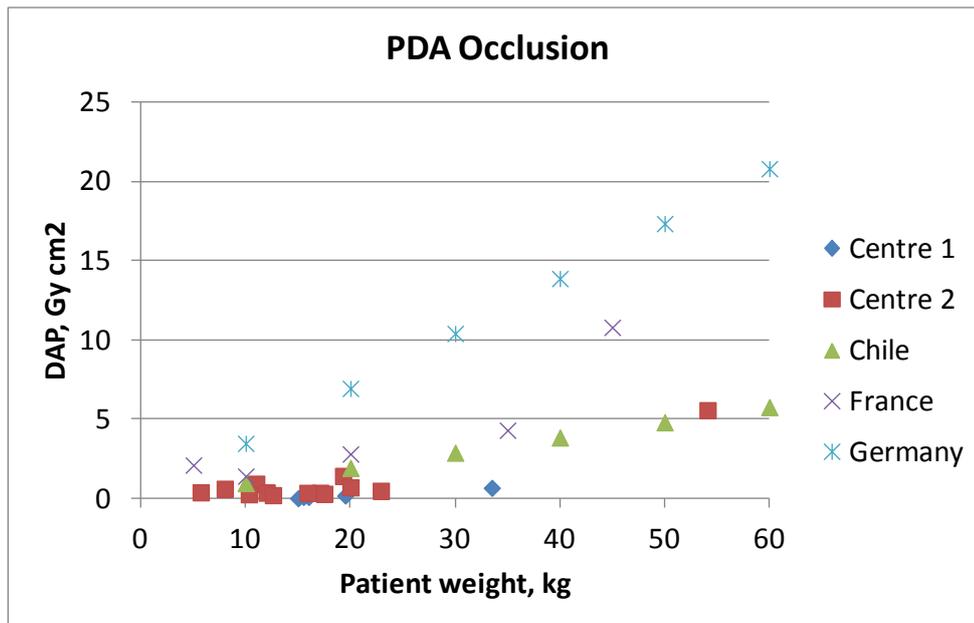
1 volume. They also calculated the effective doses using the PCXMC program (Tapiovaara and
2 Siiskonen, 2008). The mean P_{KA} for diagnostic procedures was 4.9 Gy cm^2 , while for therapeutic
3 procedures the mean P_{KA} values varied from 2.0 Gy cm^2 for atrial septal defect (ASD) to 11.9 Gy
4 cm^2 for angioplasty. For diagnostic procedures, the results were in agreement with some previously
5 reported values, thus suggesting that in diagnostic catheterization, the procedures are roughly
6 standardised. For therapeutic procedures, the agreement with some previous studies was less good.
7 These results also suggest that, compared with DRLs for diagnostic procedures, either lower or
8 higher DRLs should be used for therapeutic procedures, depending on the type of procedure. A
9 wide variation was shown in the results, even though all procedures were performed in the same
10 catheterization room and the vast majority of them by the same radiologist.

11
12 Harbron et al. (2015) report from a large multicentre study including 10257 procedures carried out
13 on 7726 patients at 3 UK hospitals from 1994 to 2013. They noticed that P_{KA} was positively
14 correlated with patient mass, and report median P_{KA} (with interquartile range) and median P_{KA} per
15 kilogram for different patient mass ranges, for all 3 hospitals and different eras of data collection.
16 They observed a decrease of dose levels during the years (different eras) and conclude that the
17 impact of technological factor is greater than increased operator experience or gradual refinement of
18 techniques. The usage patterns of antiscatter grids appear to have had the greatest influence on dose.
19 Due to the considerable variation observed in median doses between procedure types, they warn
20 against the classification of procedures as simply diagnostic or therapeutic, in particular when DRLs
21 are being set.

22
23 Corredoira et al. (2015) has studied the contribution of 3D rotational angiography, also referred to
24 as cone beam CT (CBCT), to patient doses in a cardiac catheterization laboratory. In four years
25 period (2009-2013), they collected data from 756 procedures (77 % therapeutic) involving 592
26 patients. CBCT were acquired for 109 patients (18,4 % of the sample). The results were presented
27 separately for five age groups and ten weight groups. The maximum P_{KA} was higher for diagnostic
28 procedures than for therapeutic procedures due to differences in difficulty and complexity and the
29 greater proportion of cine series acquisitions (this observations is contradictory to the experience in
30 the other studies above). The percentage increase of the median P_{KA} due to CBCT was 33 % and 16
31 % for diagnostic and therapeutic procedures, respectively. The correlation between P_{KA} and weight
32 was poor ($r^2 = 0.22 \dots 0.28$) because in the biplane system the dose from PA-projection may be
33 related to weight but in lateral projection it is related to thorax size and to the complexity of the
34 procedure.

35 36 **G.1.3 PiDRL survey from two cardiac centres**

37 In the context of the PiDRL project, patient dose data for a few paediatric cardiac procedures were
38 requested from a few centres. Due to practical difficulties, data were received only from two
39 centres, and from this very scarce data (total of 26 and 23 patients), only data for one procedure,
40 patent ductus arteriosus (PDA) occlusion, could be used for comparison with some other published
41 data (Fig. G.2). While the data is too scarce to make any firm conclusions, it seems from Fig. G.2
42 that there are clear differences of patient dose levels between centres: the data from the most recent
43 studies seem to be lower, which is in agreement with the general trend of decreasing dose levels
44 seen in some of the published studies above (Onnasch et al, 2007; McFadden et al., 2013).



1
2
3
4
5
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33

Fig. G.2. Comparison of P_{KA} (DAP) values for paediatric PDA occlusion as a function of patient weight: a few results from two centres in the PiDRL survey (2015), data from Chile (Ubeda et al., 2015; using median value of P_{KA} /weight 0,096 Gy cm² kg⁻¹), France (Barnaoui et al., 2014; using median values of P_{KA} per weight group) and Germany (Onnasch et al., 2007; using mean value of P_{KA} /weight 0,347 Gy cm² kg⁻¹).

G.1.4 Summary

The observations from the above papers can be summarized as follows:

- The implementation of DRLs for paediatric IC procedures is not as straightforward as for simple radiographic examinations. This is because of the typically broad patient dose distributions. The sources of dose variations in paediatric IC procedures are many-fold: they include the X-ray system specifications and performance, the examination protocol and the quality of preceding echocardiographic examination, patient pathology, in particular the complexity of the cardiac disease, operator skill and the size of the patient and the angle of projection. In particular, the complexity of the local procedures should be analyzed whenever the local values exceed a DRL.
- The size of the patient is the cause of increasing patient dose, not the age. The differentiation of boys and girls is not required. The rationale for relating P_{KA} to patient weight is that the mass of the heart and the volumes of its chambers are growing in proportion to the patient's body weight (not to the body surface area).
- There seems to be a linear increase of P_{KA} with patient weight over two orders of magnitude. Therefore, P_{KA} per patient weight could be used as a DRL, instead of using different P_{KA} values for different age groups; i.e. a single value (constant of proportionality) to cover all patients could be applied.
- There seems to be contradictory results for the difference in patient dose levels between diagnostic and therapeutic procedures; therapeutic procedures have been reported to yield higher dose than diagnostic procedures, on the average, or vice versa, or no significant difference have been reported. On the other hand, therapeutic procedures seem to be less standardised than diagnostic procedures, and also the complexity level of therapeutic

procedures seems to have more variation; therefore, the difference in dose levels between diagnostic and therapeutic procedures can be associated with the type of therapeutic procedures involved. For best accuracy, therefore, DRLs should be defined separately for specified diagnostic or therapeutic procedures.

- There seems to be high variations between the patient dose levels in different centres and also within a centre. In general, the dose levels seem to have decreased over the years due to technological advances.

The comparison of published P_{KA} values or DRLs for IC procedures is difficult mainly due to inconsistent grouping of patients in weight groups. However, data from the most recent publications have been compiled in Tables G.1- G.4. The data has been derived from the published values by taking as the actual comparison parameter the mean value of the weight group in the first column (i.e., 5, 15, 25 kg etc), then using the published P_{KA} per weight ratio, or calculating the mean weight for each published weight band, then fitting a curve through the points (P_{KA} versus mean weight) and finally calculating the P_{KA} from the fitted curve for each weight parameter value.

Table G.1. Summary of published median or mean P_{KA} values ($Gy\ cm^2$) for diagnostic IC procedures.

Weight group, kg	Corredoira et al., 2015	Ubeda et al., 2015	McFadden et al., 2013	Harbron et al., 2015	Barnaoui et al., 2014	Chida et al., 2010
	mean values			median values		
<10	3,27	0,66	1,9	1,4	1,8	4,03
10 - <20	7,7	1,98	4,2	2,2	2,6	14,7
20 - <30	14,3	3,30	5,8	3,3	3,7	25,4
30 - <40	52,3	4,62	12,9	5,1	5,2	36,0
40 - <50	32,4	5,94	12,9	7,7	7,3	46,7
50 - <60	22,7	7,26	17,8	11,6	10,3	57,4
60 - < 70	38,0	8,6	17,8	17,7	14,5	68,0
70 - < 80	17,0	9,9	17,8	26,8	20,5	78,7

Table G.1. Summary of published median or mean P_{KA} values ($Gy\ cm^2$) for therapeutic IC procedures.

Weight group, kg	Corredoira et al., 2015	Ubeda et al., 2015	McFadden et al., 2013	Harbron et al., 2015	Barnaoui et al., 2014
	mean values			median values	
<10	3,25	0,70	1,9	1,4	3,5
10 - <20	6,35	2,10	4,2	2,2	5,6
20 - <30	19,6	3,50	5,8	3,3	9,0
30 - <40	22,3	4,90	12,9	5,1	14,5
40 - <50	34,2	6,30	12,9	7,7	23,4
50 - <60	42,3	7,70	17,8	11,6	37,8
60 - < 70	28,4	9,1	17,8	17,7	61,0
70 - < 80	18,9	10,5	17,8	26,8	98,3

1 Table G.3. Summary of published 75th percentile P_{KA} values (Gy cm²) for diagnostic IC procedures.
2

Weight group, kg	Corredoira et al., 2015	Ubeda et al., 2015	Onnasch et al., 2007
<10	4,72	0,82	2,5
10 - <20	13,0	2,45	7,5
20 - <30	30,1	4,08	12,5
30 - <40	23,0	5,71	17,5
40 - <50	81,9	7,34	22,5
50 - <60	51,9	8,97	27,5
60 - < 70	37,1	10,6	32,5
70 - < 80	68,8	12,2	37,5

3
4
5 Table G.4. Summary of published 75th quartile P_{KA} values (Gy cm²) for therapeutic IC procedures.
6

Weight group, kg	Corredoira et al., 2015	Ubeda et al., 2015	Onnasch et al., 2007
<10	3,30	0,85	3,3
10 - <20	9,41	2,55	9,8
20 - <30	11,3	4,25	16,4
30 - <40	24,6	5,95	23,0
40 - <50	27,7	7,65	29,5
50 - <60	44,5	9,35	36,1
60 - < 70	60,0	11,1	42,6
70 - < 80	48,4	12,8	49,2

7
8
9
10 **G.2 Paediatric interventional non-cardiac procedures**

11 As noted in Section 6.3 and C.5.4, there are no published studies related to the establishment of
12 DRLs for paediatric interventional non-cardiac procedures. Therefore, to obtain some understanding
13 of the frequencies and patient doses in these procedures, a limited survey of patient dose data in six
14 dedicated IR centres of the partner countries was carried out in the PiDRL project.

15
16 The most common of the 1700 procedures performed in 2011 or later and included in the survey are
17 shown in Table G.5. Inclusion criteria were interventions on patients up to the age of 18 years
18 where P_{KA} and clinical data were available and performed not earlier than in 2011. All centres
19 provided data for age groups whereas weight information was available only from three centres.
20 When the number of procedures was lower than 15 for any age or weight group, the results were
21 excluded from the further analysis.

22
23 As an example of the results, Table G.6 presents the 75th percentile data for peripheral insertion of
24 central venous catheters (PICC). This was the most frequent intervention of the survey, with low
25 DRLs compared to other interventions. While the number of patients in many groups of other
26 interventions was not sufficient for evaluation, local DRLs could be derived for most groups of
27 PICC. As for other interventions, the interquartile range was typically high (Q3/Q1 ratio up to 9).
28 Beyond this high variation within one centre, an even more important variation between centres was
29 typical for the majority of the interventions surveyed. PICC is special in that it is often performed

1 by combined fluoroscopic and ultrasonographic guidance and that the relative contribution of the
 2 two imaging methods is highly variable at different places.

3
 4 In Fig. G.2, the P_{KA} (DAP) values from two centres (centres 3 and 4) are shown as a function of
 5 patient weight, for arteriography of abdomen, rotational techniques. A reasonable linear correlation
 6 ($R^2 = 0,76$) can be seen despite the scarceness of data; it could be expected that for the interventions
 7 in the trunk region, the P_{KA} per patient weight could be roughly constant, analogous to the several
 8 observations in paediatric cardiac procedures (Section G.1). In Fig. G.3, another example of the
 9 data, P_{KA} values plotted as a function of patient weight, indicates a reasonable linear correlation
 10 with weight.

11
 12 Table G.5. Numbers of paediatric body interventions per centre (total number = 1700), contributed
 13 by the six centres.

14

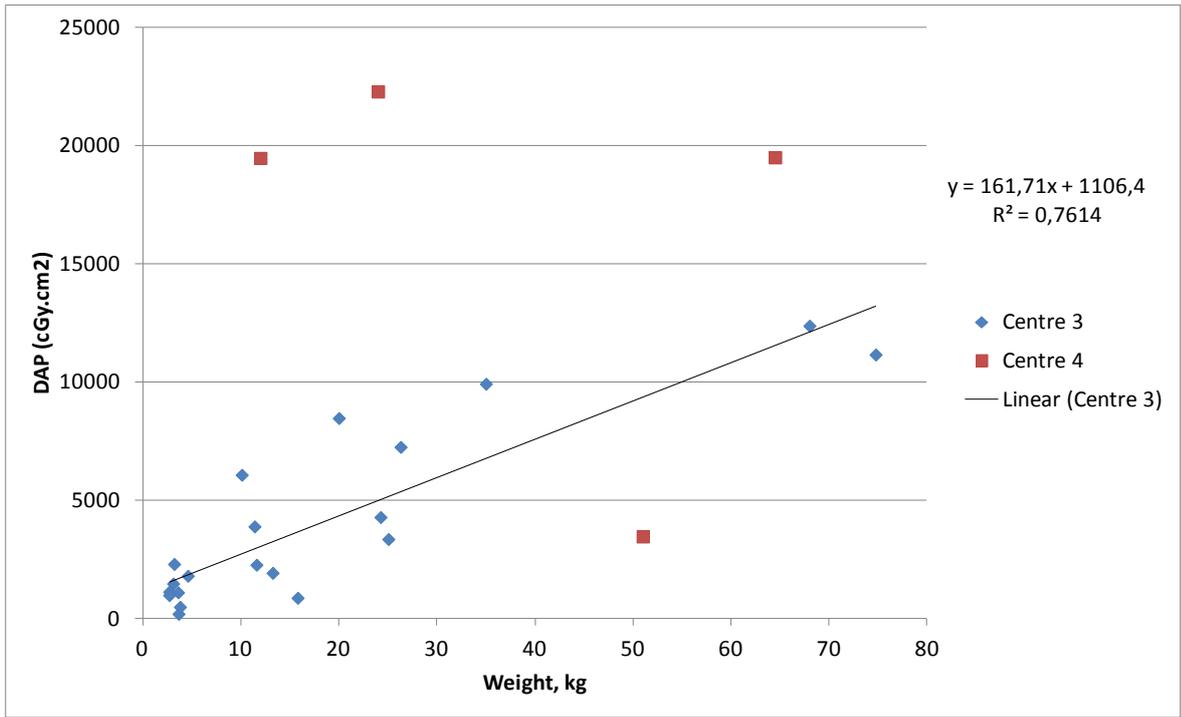
Type of intervention (*embolization includes chemoembol.)	Centre 1	Centre 2	Centre 3	Centre 4	Centre 5	Centre 6
Embolization* (all justifications) Whole body excl. head + neck + spine	11	28	32	9		
Embolization* (all justifications) Head/brain + neck + spine	1	61	102	33		
Sclerotherapy (venous malformations, lymphangiomas, cysts)	71	60	145	22		
Arteriography	53	47	159	30		
PICC (peripheral insertion of central ven. catheter) + Port/Positioning/“Broviac”	21	35	201	353		43
(GI intervention)	63					
Biliary/hepatic intervention	32			8	80	
Interventions contributed per centre	252	231	639	455	80	43

15
 16

1 Table G.6. The 75th percentiles (Q3) of the P_{KA} (DAP)–values (cGy cm²) for paediatric IR
 2 procedures “peripheral insertion of central venous catheters (PICC)” (number of patients in
 3 parenthesis). Also shown are the 25th percentile (Q1) and the interquartile range (ratio Q3/Q1), a
 4 measure of the spread of values within the age/weight group.
 5

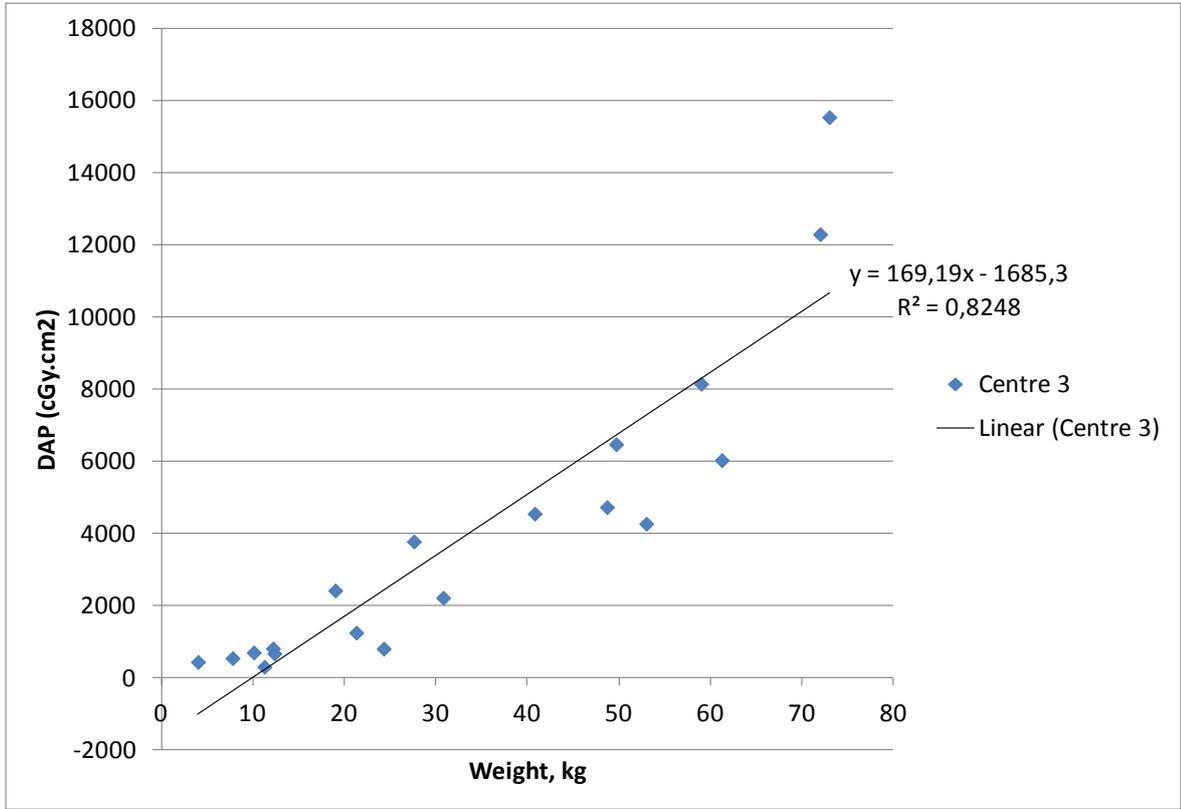
PICC – Port	C 3		C 4		C 6	
	Q3 DRL (n)	Q1, Q3/Q1	Q3 DRL (n)	Q1, Q3/Q1	Q3 DRL (n)	Q1, Q3/Q1
AGE						
<1y	1.9 (27)	0.34, 6	79.5 (54)	26.3, 3		
1y - <5y	1.9 (68)	0.49, 4	114.3 (116)	37, 3	16.9 (16)	9.6, 2
5y - <10y	3.4 (45)	0.82, 4	112 (85)	26, 4	32.3 (19)	6.3, 5
10y -<15y	9.7 (43)	1.77, 6	161.6 (72)	27.5, 6	46.9 (15)	9.2, 5
15y - 18y	18.1 (18)	5.6, 3	259.8 (26)	30, 9		
WEIGHT						
<5kg	1.8 (15)	0.44, 4				
5 - <15kg	1.8 (58)	0.38, 5	114 (65)	29, 4	16.7 (19)	7.5, 2
15 -<30kg	2.2 (66)	0.64, 3	106 (91)	38, 3	33.2 (17)	6.1, 5
30 -<50kg	12.0 (31)	1.99, 6	129.9 (67)	22, 6	32.8 (16)	12.0, 3
50 -<80kg	10.3 (28)	3.26, 3	126.7 (44)	34, 4		

6
7



1
2
3
4
5
6

Fig. G.2. P_{KA} (DAP) values as a function of patient weight for “embolization, general” in trunk region, for two centres of the PiDRL survey.



7
8
9
10
11

Fig. G.3. P_{KA} (DAP) values as a function of patient weight for “all abdomen, rotational techniques”, or one centre in the PiDRL survey.

1 The comparison of different interventions (Table G.7) clearly identified embolizations (of the head-
 2 neck-spine as well as of other body areas) and arteriographies as high DRL interventions. In
 3 contrast, PICC, gastrointestinal interventions, biliary interventions and sclerotherapy usually
 4 required lower P_{KA} (DAP) values and, thus, showed lower DRLs. Exposure, and consecutively
 5 DRLs often – but not consistently - increased parallel to the weight and the age. Table G.7 also
 6 demonstrates the high variation of DRLs of the same weight/age group between different centres.
 7 Note that the difference between two centres may reach a factor of more than 50.

8
 9 Table G.7. The 75th percentiles of the P_{KA} (DAP) values ($cGy\ cm^2$) compared as local DRLs of
 10 different centres for the most important age and weight groups. The different values for one single
 11 age/weight group represent the different local DRLs of those centres with at least 15 interventions
 12 of this type.

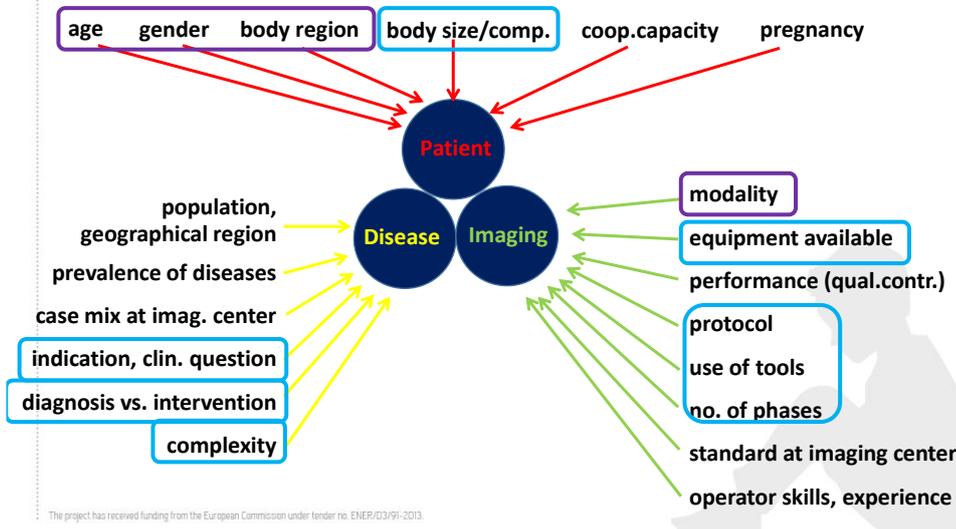
Intervention	1 - <5y	5 - <10y	10 - <15y	5 - <15kg	15- <30kg	30 - <50kg
Embolization Head n-s	9928, 13325		7768, 9195	9105	16470	10889
Embolization body	6550					
Arteriography	2177	4029	4077, 6250, 6797	1690	4223	4541, 27781
Sclerotherapy	26	32, 67, 365	88, 51, 225	39	41	49
PICC (insertion of central ven. cath.)	2, 17, 114	3, 32, 112	18, 260	2, 17, 114	2, 33, 106	12, 33,130
(Gastrointest.)	7		31			
Biliary	55	74	114			

14
 15

conventional

new approaches

FACTORS INFLUENCING DRLs



2
3

4 Fig. G.4. Factors affecting patient dose and setting of the DRLs.

5

6 There is a large number of factors affecting patient doses (Fig. G.4), and this makes the
7 establishment and use of DRLs very challenging, in particular for paediatric non-cardiac IR
8 procedures. The results of the PiDRL limited study support the conclusion that more studies,
9 collection and comparison of patient dose data from several European centres have to be conducted
10 to obtain sufficient basis to judge the feasibility of the DRLs for paediatric non-cardiac
11 interventions. In view of the wider inter-centre than intra-centre variation, the PiDRL project
12 suggests local and national DRLs are first produced. The evaluation and comparison of a large
13 number of LDRLs may allow the future establishment of European DRLs.

1 ANNEX H. LIST OF ABBREVIATIONS AND SYMBOLS

2	AAPM	American Association of Physicists in Medicine
3	ACR	American College of Radiology
4	ALARA	As low as reasonably achievable
5	AP	Anterio-posterio
6	ASD	Atrial septal defect
7	BSS	Basic safety standards
8	CBCT	Cone beam computed tomography
9	CR	Computed radiography
10	CT	Computed tomography
11	CTDI	Computed tomography dose index
12	CTDI _{vol}	Volume computed tomography dose index
13	DAP	Dose-area product
14	DDM2	Dose Datamed II
15	DICOM	Digital imaging and communications in medicine
16	DLP	Dose-length product
17	DR	Digital radiography
18	DRL	Diagnostic reference level
19	EC	European Commission
20	ESAK	Entrance-surface air kerma (the same as $K_{a,e}$)
21	ESD	Entrance-surface dose
22	EU	European Union
23	EDRL	European diagnostic reference level
24	GI	Gastro-intestinal
25	HRCT	High-resolution computed tomography
26	IAEA	International Atomic Energy Agency
27	IAK	Incident air kerma (the same as $K_{a,i}$)
28	IC	Interventional cardiology
29	ICRP	International Commission on Radiological Protection
30	ICRU	International Commission on Radiation Units and Measurements
31	IEC	International Electrotechnical Commission
32	IHE	Integrating the Healthcare Enterprise
33	IR	Interventional radiology
34	$K_{a,i}$	Incident air kerma (the same as IAK)
35	$K_{a,e}$	Entrance-surface air kerma (the same as ESAK)
36	$K_{a,r}$	Air kerma at patient entrance reference point (the same as CAK)
37	KAP	Air kerma-area product (the same as P_{KA})
38	LAT	Lateral
39	LDRL	Local diagnostic reference level
40	MCU	Micturating cysto-urethrography (the same as VCU)
41	NDRL	National diagnostic reference level
42	P_{KA}	Air kerma-area product (the same as KAP)
43	PA	Posterior-anterior
44	PACS	Picture archiving and communication system
45	PDA	Patent ductus arteriosus
46	PET-CT	Positron emission tomography – computed tomography
47	PICC	Peripheral insertion of central catheters
48	PiDRL	Paediatric imaging diagnostic reference level
49	RDSR	Radiation dose structured report

- 1 SPECT-CT Single-photon emission tomography – computed tomography
2 SSDE Size-specific dose estimate
3 TCM Tube current modulation
4 UNSCEAR United Nations Scientific Committee on Effects of Atomic Radiations
5 VCU Voiding cysto-urethrography (the same as MCU)

6
7 Country codes (EUROSTAT):
8 (http://ec.europa.eu/eurostat/statistics-explained/index.php/Glossary:Country_codes)
9

AT	Austria
BE	Belgium
BG	Bulgaria
CH	Switzerland
CY	Cyprus
CZ	Czech Republic
DE	Germany
DK	Denmark
EE	Estonia
EL	Greece
ES	Spain
FI	Finland
FR	France
HR	Croatia
HU	Hungary
IE	Ireland
IS	Iceland
IT	Italy
LT	Lithuania
LU	Luxembourg
LV	Latvia
MT	Malta
NL	The Netherlands
NO	Norway
PL	Poland
PT	Portugal
RO	Romania
SE	Sweden
SI	Slovenia
SK	Slovakia
UK	United Kingdom

10